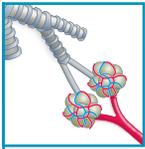


# DEFINING PHYSIOLOGICAL NORMOXIA FOR IMPROVED TRANSLATION OF CELL PHYSIOLOGY TO ANIMAL MODELS AND HUMANS

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**Keeley TP, Mann GE.** Defining Physiological Normoxia for Improved Translation of Cell Physiology to Animal Models and Humans. *Physiol Rev* 99: 161–234, 2019. Published October 25, 2018; doi:10.1152/physrev.00041.2017.—The extensive oxygen gradient between the air we breathe ( $P_{O_2} \sim 21$  kPa) and its ultimate distribution within mitochondria (as low as  $\sim 0.5$ – $1$  kPa) is testament to the efforts expended in limiting its inherent toxicity. It has long been recognized that cell culture undertaken under room air conditions falls short of replicating this protection *in vitro*. Despite this, difficulty in accurately determining the appropriate  $O_2$  levels in which to culture cells, coupled with a lack of the technology to replicate and maintain a physiological  $O_2$  environment *in vitro*, has hindered addressing this issue thus far. In this review, we aim to address the current understanding of tissue  $P_{O_2}$  distribution *in vivo* and summarize the attempts made to replicate these conditions *in vitro*. The state-of-the-art techniques employed to accurately determine  $O_2$  levels, as well as the issues associated with reproducing physiological  $O_2$  levels *in vitro*, are also critically reviewed. We aim to provide the framework for researchers to undertake cell culture under  $O_2$  levels relevant to specific tissues and organs. We envisage that this review will facilitate a paradigm shift, enabling translation of findings under physiological conditions *in vitro* to disease pathology and the design of novel therapeutics.

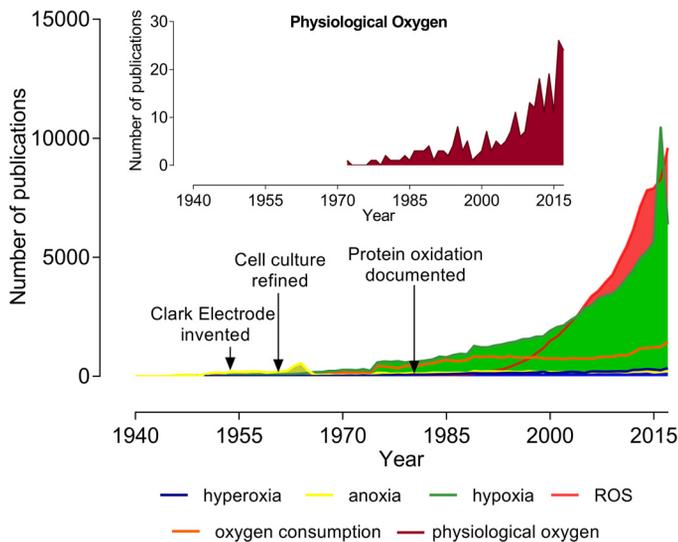
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## I. INTRODUCTION

Although most organisms on Earth possess a carbon-based skeleton, oxygen fuels life. The conversion of a  $CO_2$ -rich atmosphere to one containing precious  $O_2$ , initially by photosynthesizing cyanobacteria, and later by plants, was the pivotal step in the evolution of multicellular life on Earth (324). However,  $O_2$  is an inherently dangerous molecule, and hence, its utilization as a metabolic substrate is closely associated with the development of highly efficient detection [e.g., hypoxia-inducible factors (516, 630)], defense [glutathione (GSH) (195, 387) and antioxidant enzymes (261)] systems. Despite this, the damage caused by a lifetime breathing  $O_2$  may ultimately affect lifespan (222, 324). Several excellent and comprehensive reviews have discussed the various roles played by  $O_2$  in mammalian physiology (59, 119, 333, 565, 594, 679, 699), and thus, these will not form the primary focus of this review article. Nevertheless, a brief overview is important to inform the themes addressed herein.

The principle role of  $O_2$  in mammalian physiology is as the terminal electron acceptor in the electron transport chain (ETC). In this capacity, a single oxygen atom is reduced to  $H_2O$  in the presence of two protons and two electrons. Such reductive/oxidative (redox) reactions are fundamental in  $O_2$  physiology and are utilized by cytosolic enzymatic systems in addition to mitochondria. Aside from molecular  $O_2$ , oxygen strongly influences cellular physiology through the formation of reactive oxygen species (ROS). First considered merely as unwanted by-products of oxidative phosphorylation and dysfunctional enzymatic reactions (222), ROS are now considered to play functional and nonredundant roles in cell signaling in physiology as reviewed previously (119).

Our increased understanding of oxygen's role in human physiology is paralleled by the growing number of primary research publications (see **FIGURE 1**). To date, over half a million research articles reference oxygen as a keyword, and the number per year has steadily increased over the last century. Attention has shifted from initial interests in the mechanisms of cellular  $O_2$  utilization to consequences associated with dysfunction in these processes, leading ultimately to the production of ROS (**FIGURE 1**). Another key theme to have emerged is the concept of hypoxia, a pathological reduction in  $O_2$  availability now accepted as a hallmark of disease conditions (522). Indeed, a significant proportion of  $O_2$ -related research still focuses on the conse-



**FIGURE 1.** Timeline of  $O_2$ -related research publications. *Main graph:* Number of PubMed entries in which the keyword oxygen is mentioned within the title or abstract over the past 76 yr. Arrows indicate important events relevant to the scientific study of oxygen in the context of medical science. *Inset:* Distribution of PubMed entries in which “oxygen” is mentioned in either the title or abstract between January 1, 2010 and December 31, 2017. ROS, reactive oxygen species.

quences of  $O_2$  deprivation (FIGURE 1). In view of the importance of maintaining  $O_2$  levels within a finite range at the whole organism level, we here readdress the role of  $O_2$  in mammalian cell culture.

The invention of  $O_2$ -sensitive electrodes (87), and in recent years, phosphorescent dyes (116, 610), has enabled researchers to resolve tissue  $O_2$  distribution in vivo. Although incredibly heterogeneous, at no point beyond the mouth is  $PO_2$  equivalent to room air (20.9 kPa). Despite this, the culture of mammalian cells is routinely conducted under atmospheric  $O_2$ , conditions hyperoxic with respect to the tissue of origin. Although this discrepancy has been widely acknowledged (215, 455, 633), only in recent years have primary research publications addressed this issue directly (FIGURE 1, inset). A consensus approach to tackling this concept is still lacking, largely plagued by incorrect nomenclature and widely differing experimental conditions. This review aims to provide an insight into the current knowledge regarding tissue  $O_2$  distribution in vivo and in doing so, to redefine the term normoxia for more appropriate use in in vitro experiments. Techniques used to monitor  $O_2$  levels both in vivo and in vitro will be described initially, followed by an overview of experimental issues associated with varying  $O_2$  levels in vitro. Physiological  $O_2$  levels in numerous tissues and the existing literature concerning replication of these conditions in vitro are summarized and critically discussed. The development of cell culture techniques revolutionized medical science in the 1950s, yet maintenance of cultured cells or tissues under nonphysiological  $O_2$  levels limits translation from bench to bedside. In many fields, cell culture under atmospheric, room air  $O_2$

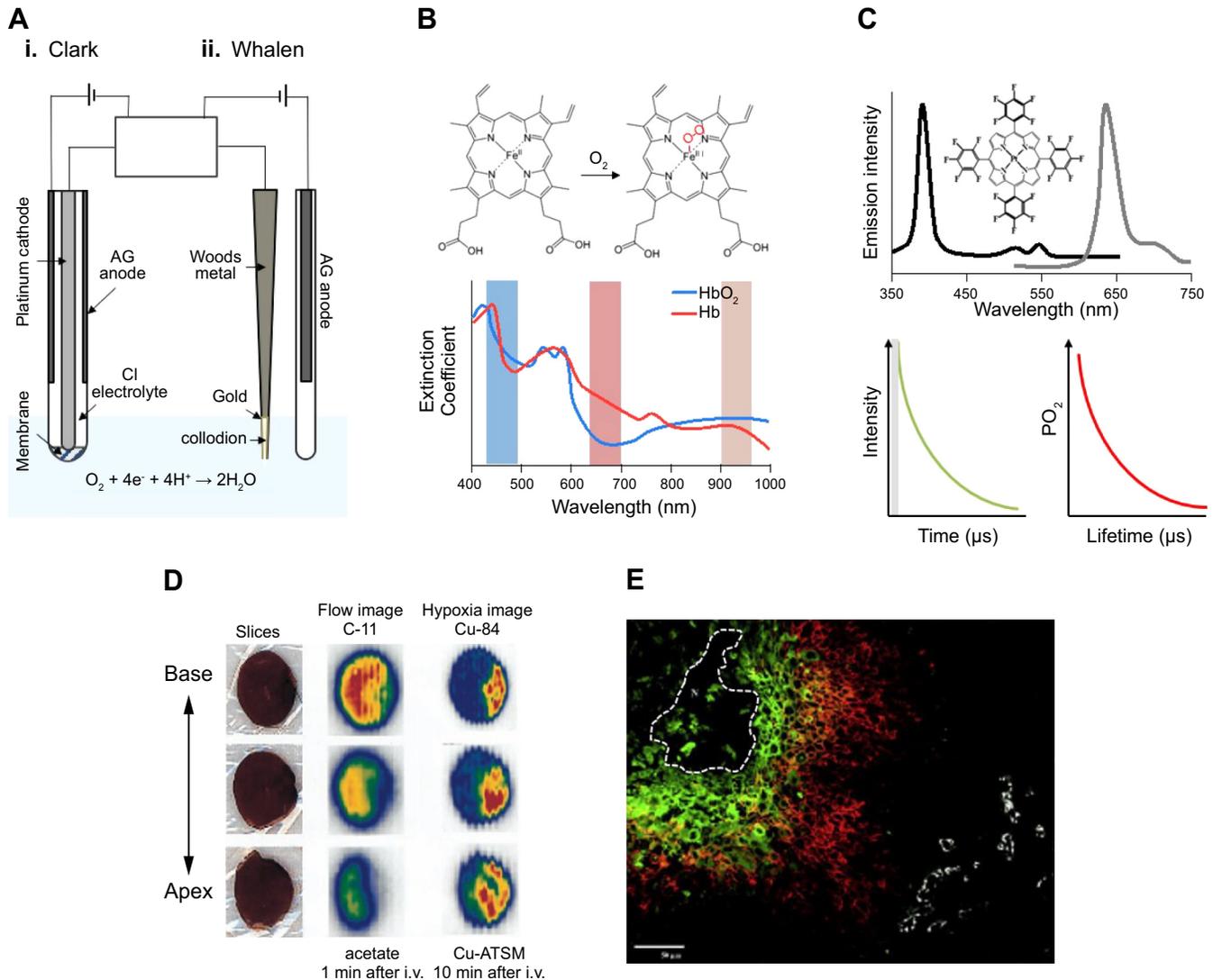
levels has been assumed to reflect normoxia largely because of the complexity of conducting experiments in an oxygen-regulated workstation. This review aims to readdress the conditions in which all mammalian cells should be cultured, with the aim of more effective translation of in vitro science into potentially life-saving therapies.

## II. TECHNIQUES TO MEASURE OXYGEN IN CELLS AND TISSUES

Necessity often dictates that improvements in experimental techniques frequently precede advances in scientific knowledge, and such is the case with oxygen-related physiology (FIGURE 1). The study of the physiology and biochemistry of molecular  $O_2$  was aided immensely in the 1950s by the development of  $O_2$ -sensitive electrodes, which allowed the direct quantification of  $O_2$  levels in biological fluids (87). A number of innovative techniques have since been developed, facilitating more advanced experimental measurements with greater spatial and temporal resolution. Wire electrodes can offer excellent spatial definition over a very small sample area, whereas phosphorescence imaging techniques can offer greater stability over time and over a greater sampling size. Notably, these techniques rarely monitor  $O_2$  concentration directly but rather  $PO_2$ , which is directly proportional to concentration, or hemoglobin (Hb) saturation. The following section outlines the basic principles of the most well-established techniques currently used to monitor cellular and tissue  $PO_2$ , providing a basis for discussion of data obtained using such equipment in later sections.

### A. Oxygen-Sensitive Electrodes

The chemical reduction of molecular  $O_2$  on a polarized (usually 0.6–7 V) platinum cathode generates a current proportional to the concentration of  $O_2$  present. This concept led to the development of  $O_2$ -sensitive electrodes in the early 1950s consisting of a polarized platinum cathode and nonpolarizable silver anode (see FIGURE 2A). Although effective in determining dissolved  $O_2$ , these early electrodes were not suitable for measuring tissue or blood  $O_2$  because of the accumulation of cells/proteins on the cathode-limiting reactivity. This problem was solved by Leland Clark and colleagues who, in 1953, described the fabrication of a platinum electrode with an  $O_2$ -permeable cellophane coating (87) (FIGURE 2A). The addition of a selectively permeable membrane permitted the measurement of  $PO_2$ , as  $O_2$  must now diffuse across its partial pressure gradient to react on the cathode. These electrodes, commonly referred to now as “Clark Electrodes,” were greatly utilized for the measurement of liquid  $PO_2$  for blood gas analysis and early mitochondrial respiration experiments (73), yet their relatively large size (<1 mm) prevented accurate measurements of tissue  $PO_2$ . Efforts during the 1960s culminated in the in-



**FIGURE 2.** Techniques to determine tissue and cellular  $PO_2$ . **A:** Diagram of the two common types of  $O_2$ -sensitive electrodes, the Clark and Whalen types. Both are connected to an external power supply and galvanometer to record changes in current due to reduction of  $O_2$  at the cathode. **B:** The basis for hemoglobin saturation measurements. The binding of  $O_2$  to hemoglobin is associated with a change in its spectral properties, which are measured at various wavelengths to determine the ratio of oxyhemoglobin to total hemoglobin. **C, Top:** the excitation (solid)/emission spectra, (dashed) spectra for Pt<sup>II</sup>/porphyrin-based phosphorescent probes, with a structural schematic provided in the inset. Adapted from Fercher et al. (151). **Bottom:** schematics illustrating the basis for  $O_2$  measurements by time-resolved fluorescence; *left*, after the initial excitation flash, phosphorescent emission decays at an exponential rate, with most  $O_2$ -sensitive complexes exhibiting lifetimes in the 10–1000- $\mu$ s range; *right*, the relationship between calculated probe lifetime and  $PO_2$ . **D:** Representative images of  $^{11}C$ /acetate and  $^{64}Cu$ /ATSM loaded isolated hearts subjected to left-anterior-descending artery occlusion, generating a region of ischemia identified by the absence of flow ( $^{11}C$  negative and  $^{64}Cu$  positive). Taken with permission from Fujibayashi et al. (169). **E:** Immunohistochemical section of a squamous cell carcinoma stained to show pimonidazole (green) and carbonic anhydrase 9 (red), with blood vessels (white) and necrotic regions (enclosed in dashed white) identified. Taken with permission from Hoogsteen et al. (253).

roduction of the “Whalen”-type electrode; a recessed-tip gold alloy cathode with a diameter of 1–3  $\mu$ m (644) (FIGURE 2Aii). By attaching an  $O_2$  electrode to a micromanipulator, tissue  $PO_2$  histograms were easily obtainable and rapidly became the preferred method for reporting  $PO_2$  (see sect. VI). In recent decades, the use of electrodes has decreased in favor of newer techniques (discussed below) because of the following disadvantages: 1) by virtue of their chemistry,

electrodes consume  $O_2$  (proportional to their diameter) and therefore, may be considered less reliable, especially when attempting to measure very low levels of  $O_2$ , 2) the small sampling area means measuring large areas of tissue is tedious, and 3) many have shown that tissue penetration by electrodes produces artifactual changes in tissue  $PO_2$  resulting from blood vessel rupture or cell disruption (266). The second point has been partially addressed through the de-

velopment of the multiwire platinum electrode (296), in which eight independent Clark-type electrodes are housed within a hemispherical structure of roughly  $\sim 50\text{-}\mu\text{m}$  diameter. Although greatly increasing the sampling area, these electrodes are confined to surface  $\text{PO}_2$  measurements, and hence, their use is limited.

## B. Hb/myoglobin Spectroscopy

Prior to the invention of  $\text{O}_2$ -sensitive electrodes, the only readout of blood oxygenation available was the spectrophotometric analysis of Hb, although this was only employed clinically in the late 1970s following the development of the pulse oximeter by Aoyagi and colleagues (13). This technique relies on the change in absorbance spectrum of Hb upon binding to  $\text{O}_2$  (see **FIGURE 2B**) characterized by a reduction in absorbance in the red region (650–700 nm) and an increase in the near-infrared (900–1000 nm) region. Isolation of the Hb-derived signal from intrinsic signals of the surrounding tissues and venous blood is achieved by only measuring the pulsatile changes in absorbance. So-called pulse oximeters are extensively used clinically to monitor peripheral arterial blood  $\text{O}_2$  saturation, which is 95%–99% in normoxic patients. In the laboratory, a technique to measure Hb saturation in the microvasculature was developed by Pittman and Duling in 1975 (460, 461), in which the effects of light scattering by red blood cells was accounted for. A similar technique has also been used to measure myoglobin saturation in cardiac and skeletal muscle (89, 252). In the context of defining tissue  $\text{PO}_2$ , Hb saturation can be converted into approximate  $\text{PO}_2$  based on the known Hb saturation curves for the appropriate species (594), although this conversion is subject to changes in local pH/ $\text{PCO}_2$  and temperature and hence should be used with caution.

## C. Fluorescent and Phosphorescent Probes

Optical techniques to monitor cellular and tissue  $\text{PO}_2$  were developed by David Wilson and colleagues in the late 1980s, who introduced platinum ( $\text{Pt}^{\text{II}}$ ) and palladium ( $\text{Pd}^{\text{II}}$ ) porphyrin-based probes, which exhibit quenched phosphorescence in the presence of molecular  $\text{O}_2$  (497, 610). These have been complemented by similar complexes utilizing ruthenium ( $\text{Ru}^{\text{II}}$ ) (348, 366, 580) or iridium ( $\text{Ir}^{\text{III}}$ ) (108), all of which can be conjugated to various macromolecular carriers or polymers to improve solubility or phosphorescence yield. A complete description of  $\text{O}_2$ -sensitive lumiphores can be found elsewhere (115). In principle, complexes are excitable in the UV range (350–410 nm) and emit in the far red (630–700 nm) region, allowing excellent resolution in biological media, with decay lifetimes in the microsecond range. Typically, measurements are taken using time-resolved phosphorescence, whereby the probe is excited, and the  $\text{O}_2$ -sensitive decay in resultant emission intensity is resolved over time (see **FIGURE 2C**). First-generation

phosphorescent complexes were hydrophilic, and hence, measurements were confined to the vasculature (535, 583), but subsequent variations have generated hydrophobic equivalents that can penetrate the cell membrane, such as Oxyphor G4 (136) or MitoXpress Intra (151). The addition of other chemical moieties to the basic metal/porphyrin structure has also alleviated issues with nonspecific protein binding that altered the spectral properties of first-generation compounds in vivo (115). With these, simultaneous measurements of blood and tissue  $\text{PO}_2$  have been reported (9) as well as intracellular  $\text{PO}_2$  within monolayers in culture (75, 151, 615).  $\text{Ru}^{\text{II}}$  complexes have largely been utilized in the OxyLite probe, where they are immobilized in a sensor tip ( $\sim 200\ \mu\text{m}$  in diameter) and excited via a fiber-optic cable, functioning in an analogous manner to a traditional electrode.

## D. Magnetic, Paramagnetic, and Electron Spin Resonance

Positron emission tomography (PET), magnetic resonance imaging (MRI), and electron spin resonance (ESR) techniques have been developed to image regions of hypoxia in vivo, as reviewed elsewhere (60). Imaging using PET employs traditional biochemical markers of tissue hypoxia, such as the imidazole compounds (see below), containing the radionucleotide  $^{18}\text{F}$  as a short-lived source of protons. These compounds accumulate within regions of hypoxia and have been useful in imaging tumor  $\text{PO}_2$  in animal models and in the clinical setting (356). More recently,  $^{64}\text{Cu}$ -containing bishiosemicarbozones have been targeted as potentially useful markers of hypoxia, with  $^{64}\text{Cu}$ -diacetyl-bis-*N*(4)-methylthiosemicarbazone ( $^{64}\text{Cu}$ /ATSM) showing high selectivity for regions of relative hypoxia in the ischemic Langendorff heart (169) and atherosclerotic lesions in rodents (426) as well as tumors in humans (602). An example of  $^{64}\text{Cu}$ /ATSM accumulation in the myocardial ischemic core is provided in **FIGURE 2D**. MRI oximetry emerged in the late 1980s following the discovery that rates of relaxation to perfluorocarbon (PFC) compounds were linearly related to  $\text{PO}_2$  (572). When combined with traditional  $^1\text{H}$  MRI anatomical imaging, MRI oximetry can provide useful spatial resolution in both animals and humans (680). In the lungs,  $\text{PO}_2$  distribution can also be monitored by MRI using inhaled hyperpolarized  $^3\text{He}$ , the decay of which is increased in the presence of  $\text{O}_2$  (127) (see **FIGURE 7**). In addition to using exogenous probes, deoxyhemoglobin is a paramagnetic species itself, and its relative proportion to oxyhemoglobin can be visualized as a disturbance in the transverse relaxation time ( $T_2^*$ ) of the surrounding protons in water. This led to the development of blood-oxygen level-dependent MRI imaging (BOLD-MRI) (436, 577), which uses standard MRI protocols to monitor changes in Hb saturation and is widely used clinically. One major advantage of BOLD-MRI over PFC-MRI and PET is that it does not require the introduction of an exogenous probe, mitigating

fears over chemical or radioactive toxicity. Unfortunately, BOLD-MRI is not capable of determining absolute fluid  $P_{O_2}$  and hence cannot be used to monitor tissue  $P_{O_2}$ . Molecular  $O_2$  is weakly paramagnetic itself and can be detected as a small but definitive increase in the longitudinal relaxation time ( $T_1$ ) of the surrounding protons, first identified using NMR (590) and later confirmed using MRI (267, 432, 656). Notably, changes in  $T_1$  rates occur under conditions in which very limited increases in Hb saturation (and therefore  $T_2^*$  rates) were detected (656). Although this technique has been used to determine absolute increases in  $O_2$  content (ml/L blood) following hyperoxic inspiration, it has had limited application to determine absolute physiological tissue  $O_2$  concentration. Varying  $T_1$  times were reported in the liver, kidney, and muscle of rabbits, which, when combined with simultaneous measurements of  $T_2^*$  rates, may be indicative of tissue  $P_{O_2}$  (432, 656).

Much like PET and PFC-MRI, ESR oximetry relies on the interaction between a probe and molecular  $O_2$ . The most commonly used probes to measure  $P_{O_2}$  using ESR are lithium-based cyanines and India ink (8), which are biocompatible particulate probes and have been used to report tissue  $P_{O_2}$  in liver (275), heart (487), lungs (487), digestive tract (228), and bone (360). The presence of  $O_2$  in close proximity to the ESR probe causes a broadening of the probe spectrum, measurable in the line width, which is directly proportional to  $P_{O_2}$ . Hence, unlike PET and MRI, ESR permits the direct quantification of tissue  $P_{O_2}$  and can be used for long periods of time because of the inert and stable nature of the spin probes (8). Unfortunately, the complex and costly equipment required to detect spin resonance limits the application of ESR to specialized facilities.

## E. Immunohistochemical Methods

The techniques discussed so far have been developed to monitor relative or absolute tissue  $P_{O_2}$ . Complimentary to these has been the immunohistochemical identification of hypoxic areas using exogenous dyes like pimonidazole or EF5 (357, 474) or antibodies raised against known hypoxia-inducible target proteins such as hypoxic-induced factor (HIF) or CA9, which rely on the cellular response to lowered  $O_2$  levels rather than the absolute  $P_{O_2}$ . Pimonidazole and EF5 are 2-nitroimidazole derivatives containing a  $NO_2$  group attached to an imidazole ring, which undergoes rapid reduction to produce a highly reactive intermediate species that will react with any macromolecule in the vicinity. At a  $P_{O_2}$  more than  $\sim 1.5$  kPa  $O_2$ , this reduction is prevented, and thus 2-nitroimidazole staining is selective for regions of severe hypoxia. When sections of hypoxic tissue are costained with pimonidazole and a hypoxia-inducible protein such as HIF-1 $\alpha$  or CA9, distinct and mildly overlapping regions are observed (see **FIGURE 2E**), suggesting that the two probes are marking areas of differing severity of hypoxia (253, 545). Although the nature of pimonidazole  $O_2$  sensitivity

has been considered reasonably binary (staining is either present or absent), gradients in intensity corresponding to measurable gradients in  $P_{O_2}$  have been reported across the intestinal wall (294). This tissue is reported to be severely hypoxic (see sect. VIF2), and hence, it is possible that differences in staining intensity may be resolved within the reported range ( $P_{O_2}$  0–1.5 kPa). A disadvantage in the use of 2-nitroimidazole compounds to identify hypoxic tissue is that staining requires live cells; thus, the dye must be injected before samples being collected. This limits its use in retrospectively identifying hypoxic areas in tissue specimens already collected or in patient samples. A caveat to the use of immunostaining members of the HIF pathway as a marker of tissue hypoxia is the well-described potential of HIF-1 $\alpha$  to be stabilized under oxygenated conditions, most notably during inflammation because of cross-talk with NF $\kappa$ B and direct effects of ROS (44, 607). Hence, results obtained using HIF-based immunostaining should always be confirmed with an alternative method.

## III. OXYGEN DELIVERY IN VIVO

A basic understanding of the delivery of  $O_2$  from the atmosphere to the cytosol is fundamental for interpreting specific tissue  $O_2$  distribution. Moreover, insights into  $O_2$  transport in vivo provide a useful perspective for some of the challenges associated with oxygenation of cell monolayers in vitro. A point worth clarifying before any detailed further discussion is the difference between the terms saturation, concentration, and content as commonly used throughout physiology and partial pressure used universally. In mammals,  $O_2$  is transported in two forms: bound to Hb and dissolved in blood. Saturation refers to the percentage of total number of Hb bindings sites saturated with  $O_2$  (4 mol of  $O_2$  bind to 1 mol of Hb), noting that Hb saturation occurs in continuum until all molecules are saturated. This unit does not strictly measure the concentration of  $O_2$  present (although this can be inferred) but is a good measurement of total blood  $O_2$  content. Although convention is to express components of a chemical reaction as a concentration (in moles per liter, for example),  $O_2$  should be reported as partial pressure (in mmHg, Torr, or kPa, **FIGURE 5A**) in physiology, noting the final dissolved gaseous concentration in a liquid is proportional to its partial pressure within the corresponding gas phase [Henry's Law (235), taking into account changes in temperature and solubility; sect. IVB]. This is because the chemical potential of physiological gases is determined by their partial pressure, and as such, they will diffuse down pressure, not concentration, gradients. Content refers to the total amount of  $O_2$ , in ml/100 ml, that blood can carry, combining that bound to Hb with that dissolved in plasma according to the following equation:

$$cO_2 = ([O_2]_{\max} \times [Hb] \times SO_2 \times 0.01) + (H \times P_{O_2}) \quad (1)$$

in which the maximal  $O_2$ -carrying capacity of blood ( $[O_2]_{\max}$ ) is 1.31–1.36 ml  $O_2$ /g Hb, otherwise known as

Hüfner's constant (110, 194), and  $H$  is the Henry's Law constant for  $O_2$  (0.023 ml/kPa/100 ml of blood). Human blood contains, on average, 14–15 g Hb per 100 ml (194, 604), and therefore the  $O_2$  content ( $cO_2$ ) of fully  $O_2$ -saturated ( $SO_2 \sim 100\%$ ) arterial blood =  $(1.34 \times 15 \times 100 \times 0.01) + (0.023 \times 13) = 20.4$  ml/100 ml blood. Note that  $O_2$  content is also expressed in units of concentration (ml/100 ml), but differs from the traditional use of  $O_2$  concentration, which typically refers to only dissolved  $O_2$  in solution.

With these three terms defined, the disparity between  $O_2$  delivery in vivo and in vitro becomes readily apparent. In the absence of Hb in vitro,  $O_2$  delivery to the cell monolayer is defined largely by the  $PO_2$  of the culture medium directly adjacent, and therefore, the total available  $O_2$  is considerably lower (e.g.,  $cO_2 = 0.48$  ml/100 ml medium under standard atmospheric conditions). The issue of  $O_2$  delivery in vitro will be discussed in more detail in sect. IV. As cells cannot access  $O_2$  bound to Hb, total  $O_2$  content is not a particularly useful unit to use when comparing in vivo and in vitro  $O_2$  conditions at the cellular level. Ideally,  $[O_2]$  should be defined in units of partial pressure (mmHg or kPa) in compliance with Henry's Law (235). However, the majority of biologists prefer to express gas concentrations in vitro as a percentage of atmospheric composition (i.e., cultured in a standard 37°C, 5%  $CO_2$  incubator). As  $O_2$  expressed as a percentage of  $\approx$ kPa at sea level (see FIGURE 5A), we have standardized the expression of  $[O_2]$  in kPa units in this review.

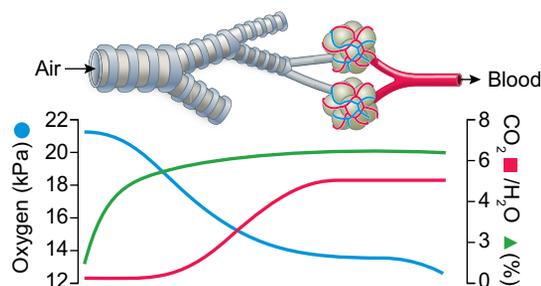
## A. From Air to Blood

Even before entering the circulation, humidification of incoming air within the trachea reduces  $PO_2$ , and the introduction of  $CO_2$  ( $\sim 5$  kPa) within the alveoli reduces this further (FIGURE 3). Hence, the gradient between atmosphere and alveoli can be described according to the following equations:

$$P_{O_2(\text{trachea})} = (P_{\text{atm}} - P_{H_2O}) \times F_{iO_2} \quad (2)$$

$$P_{O_2(\text{alveoli})} = P_{O_2(\text{trachea})} - (P_{CO_2}/RQ) \quad (3)$$

in which atmospheric pressure ( $P_{\text{atm}}$ ) is 101.325 kPa at sea level, normal water vapor partial pressure ( $P_{H_2O}$ ) is  $\sim 6.2$  kPa, and the fraction of  $O_2$  in inspired air ( $F_{iO_2}$ ) is 0.209. Thus,  $P_{O_2(\text{trachea})}$  is normally  $\sim 19.9$  kPa. As this inspired air mixes with expired air containing  $CO_2$  ( $P_{CO_2} \sim 5$  kPa) when respiring with mixed carbohydrate/fat fuel (RQ, respiratory quotient 0.8), the  $PO_2$  is reduced further to  $\sim 13.3$  kPa. A proportion of venous (deoxygenated) blood from the microvasculature supplying the larger airway and lung adventitia drains into the pulmonary vein rather than the bronchial vein (19, 76). Because of this nuance in lung perfusion, known as pulmonary venous admixture or shunt, a small gradient exists between the alveoli and arterial  $PO_2$  (usually



**FIGURE 3.** Oxygen gradients in the respiratory system. Concentrations, in kPa, of  $O_2$  (●, left axis),  $CO_2$  (■, right axis), and  $H_2O$  (▲, right axis) from dry atmosphere to the pulmonary venous circulation. Increases in  $P_{H_2O}$  and  $P_{CO_2}$  in the respiratory tract reduce  $PO_2$  proportionally, and venous admixture within the pulmonary vein reduces  $PO_2$  further.

$< 1.3$  kPa in healthy adults), spoiling an otherwise remarkably efficient exchange. Taken together, the passage of  $O_2$  from air to the blood results in a gradient of  $\sim 9$  kPa, the largest such gradient in mammalian physiology.

## B. From Blood to Cytosol

### 1. Longitudinal gradients within the vasculature

The subject of intravascular  $O_2$  gradients has been reviewed elegantly by Tsai et al. (2003), and as such, it will only be described briefly in this review. Duling and Berne (1970) were the first to demonstrate experimentally a significant loss of oxygen from the arteriolar circulation. They and many others subsequently established that 1) there is a significant decrease in  $O_2$  between the systemic arterial circulation and arteriolar vessels (43, 123, 124, 263, 325, 459), which is proportional to luminal diameter (124, 500) and inversely proportional to red blood cell velocity/blood flow (295, 584); 2) the difference between terminal arteriolar and postcapillary venular  $O_2$  is minimal (325, 534), as is the gradient between capillary and tissue  $O_2$  (43, 325); 3) the next largest tissue compartment outside the lungs in which a significant  $O_2$  gradient is observed is the vascular wall of arterioles (99, 124, 428, 507, 532, 591), which is proportional to the thickness of the arteriolar wall (124); and 4) a postcapillary diffusional shunt occurs in most microvascular beds, in which a portion of  $O_2$  from saturated arterioles diffuses into venules running parallel (131, 534). Furthermore, measurements of  $O_2$  saturation in red blood cells by absorption at 555 nm (460, 461) confirm that Hb saturation falls proportionally with dissolved  $O_2$  (457). Based on these observations, the arteriolar network appears to play more of a role in the delivery of  $O_2$  to the tissue than previously considered (500), and there may even be a role for postcapillary venules in homogenizing tissue  $PO_2$  (328). This was first noted following the observation that the re-

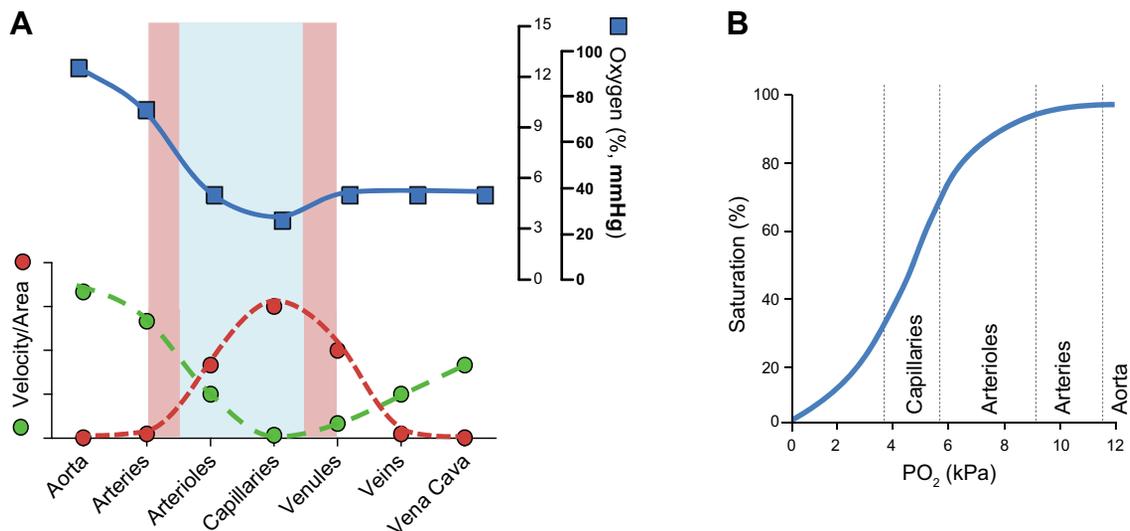
relationship between venular diameter and luminal  $\text{PO}_2$  was opposite to that described for arteriolar vessels. In other words, blood  $\text{PO}_2$  increases between postcapillary and collecting venules (43, 131, 295, 325, 532, 534, 622). However, it must be noted that blood entering the arteriolar network has a  $\text{PO}_2$  above the steepest part of the  $\text{O}_2$  dissociation curve of Hb (see **FIGURE 4B**), and therefore, it is hard to reconcile how so much  $\text{O}_2$  is transferred to the surrounding tissues from these vessels unless only the transfer of dissolved  $\text{O}_2$  is being measured. Moreover, one must also weigh up the influence of the magnitude of the vascular wall  $\text{PO}_2$  gradient (the argument in favor of arteriolar  $\text{O}_2$  delivery) against the raw number of vessels (capillaries vastly outnumber arterioles) when concluding the relative contribution of each type of vessel to tissue  $\text{O}_2$  delivery.

## 2. Radial gradients across and within the vascular wall

The evidence for longitudinal  $\text{O}_2$  gradients within the vasculature is complimented by the finding of significant radial, or transmural, gradients across the vascular wall. Radial gradients have been reported in the rabbit aortic wall (99, 428, 508), cat pial vessels (124), dog carotid arteries (507), dog femoral arteries (410), rat mesenteric arterioles (591), and rat cortical microvessels (622). Elegant work by Ninikoski et al. (428) and Santilli et al. (507, 508) using electrode penetration of the vascular wall demonstrated the existence of a substantial drop in  $\text{O}_2$  between the lumen and a very thin tissue layer directly adjacent, attributed by the authors to the endothelium, although the magnitude of this drop has been questioned subsequently (see sect. VIB1). Nevertheless, a mismatch between intimal and luminal  $\text{PO}_2$

would suggest inefficient transfer of  $\text{O}_2$  from blood to cell. A physical barrier at the tissue level seems highly unlikely because a high  $\text{O}_2$  diffusion resistance of the vascular wall would result in higher downstream  $\text{PO}_2$  than observed (591), and  $\text{O}_2$  is freely soluble in the plasma membrane (562).

The transfer of  $\text{O}_2$  between the lumen and the endothelial cell initially involves the dissociation of  $\text{O}_2$  from Hb. Considering the well-characterized  $\text{O}_2$  dissociation curve for Hb (**FIGURE 4B**), it is clear that arterial blood exists at a sufficiently high  $\text{PO}_2$  to prevent substantial  $\text{O}_2$  dissociation from Hb, as intended in such conduit vessels. Although this relationship can vary with changes in local pH/ $\text{CO}_2$  (the Bohr Shift), it is unlikely that such changes would lead to large dissociations at such a high blood  $\text{PO}_2$  (see **FIGURE 4B**). Moreover, measurements of luminal  $\text{PO}_2$ , as referenced above, reflect dissolved  $\text{PO}_2$  rather than that stored in Hb (total  $\text{O}_2$  content). Thus, the large drop in  $\text{PO}_2$  between lumen and endothelial cell cannot be explained by limited dissociation from Hb. The relative contribution of vascular wall/tissue  $\text{O}_2$  consumption to this large decline is not fully agreed upon, as reviewed elegantly elsewhere (456, 594, 603). There is general disagreement as to whether the vascular wall can consume enough  $\text{O}_2$  to account for the large radial gradient detected, with large differences between cultured cells, tissue segments, and in vivo measurements clouding any consensus [summarized elegantly by Vadapalli and colleagues (603)]. Differences in experimental technique and interpretation can certainly account for some of this variation (see sect. VIB1 for a more detailed discussion), leading to the conclusion that many reported measurements of vascular wall  $\text{O}_2$  consumption may be overes-



**FIGURE 4.** Oxygen gradients in the vascular system. *A*: The relationship between  $\text{PO}_2$  (right axis), area and velocity throughout the vasculature. Highlighted are the generally perceived vessels in which gaseous (red) and nutrient (blue) exchange takes place. Velocity and area are arbitrarily defined in this review, and average  $\text{PO}_2$  is adapted from Tsai et al. (594). *B*: A standard oxyhemoglobin saturation curve, with the average  $\text{PO}_2$  values within relevant blood vessels annotated.

estimated (456, 603). It therefore seems unlikely that this alone is sufficient to drive the large radial gradients alone. Recent evidence indicates that the major barrier to the transfer of  $O_2$  from the lumen to tissue may in fact be the plasma phase of blood. This was first proposed by Hellums (231), who hypothesized that plasma (in which  $O_2$  is poorly soluble) represents a significant barrier between the red blood cell and endothelium. In this model, dissolved  $O_2$  fluctuates as a function of hematocrit, with so-called erythrocyte-associated transients increasing  $PO_2$  near red blood cells and gradients extending in between. Such theories were corroborated by others (148, 405) and later demonstrated experimentally (22, 184, 328). In large vessels with wall thickness large enough to prevent efficient oxygenation of the vascular cells by diffusion alone,  $O_2$  is supplied via the vasa vasorum as opposed to directly from the lumen (58, 230, 410), as discussed in detail in sect. VIB1.

### 3. From vessel to cytosol

The largest  $O_2$  gradient in the vascular network is across the arteriolar wall, implicating these vessels as primary sites for  $O_2$  delivery. However, the smaller overall area of arteriolar networks compared with capillaries dictates that large heterogeneity should therefore exist in tissue  $PO_2$ , with large gradients extending between arteriolar vessels.  $O_2$  transport between the capillary and tissue was first addressed by Krogh (316), in his now seminal description of the cylinder model. These relatively simple models tend to oversimplify, because microvascular networks are rarely uniformly distributed (except perhaps in skeletal muscle), but rather display a more disorganized network. Moreover, Krogh's model assumed that longitudinal gradients occur along the length of capillaries, which we now know is not necessarily the case. The presence of both longitudinal and radial gradients in the vasculature, and diffusional transfer of  $O_2$  between neighboring arterioles, capillaries, and venules, results in a reasonably narrow Gaussian tissue  $PO_2$  distribution (593). The lack of substantial intratissue  $PO_2$  heterogeneity is of physiological significance, because an implication of Krogh's model of tissue  $O_2$  distribution is that tissue close to the venular end of the microvascular network would be at a distinct disadvantage in terms of  $PO_2$ . Of course, this viewpoint is still oversimplified as neither tissue perfusion (i.e., the number of microvascular vessels per  $cm^3$  tissue), nor is cellular  $O_2$  demand generally homogeneous, and thus, tissue  $PO_2$  gradients can still form, especially in larger organs and under uncontrolled tumor growth (as will be discussed in sect. VI).  $PO_2$  distribution in different organs/tissues will be discussed in later sections.

## IV. UNDERSTANDING OXYGENATION IN VITRO

A reoccurring theme throughout this review will be the complex nature of cellular oxygenation in vitro. The com-

bined effects of a static layer of medium above an  $O_2$ -consuming monolayer of cells, and poor solubility of  $O_2$  leads to the formation of a gradient between the atmosphere and intracellular environment (10, 75, 420). In some cases, this gradient can be substantial enough to significantly reduce intracellular  $PO_2$  below ambient, used herein analogously to headspace to refer to the gas phase immediately adjacent to the medium. Thus, intracellular oxygenation, and not ambient  $PO_2$ , is the key parameter to consider when designing research under low  $O_2$  environments. This section will address some of the nuances associated with achieving the desired intracellular  $O_2$  level in vitro to recapitulate levels in vivo.

### A. What Is the $PO_2$ in Room Air?

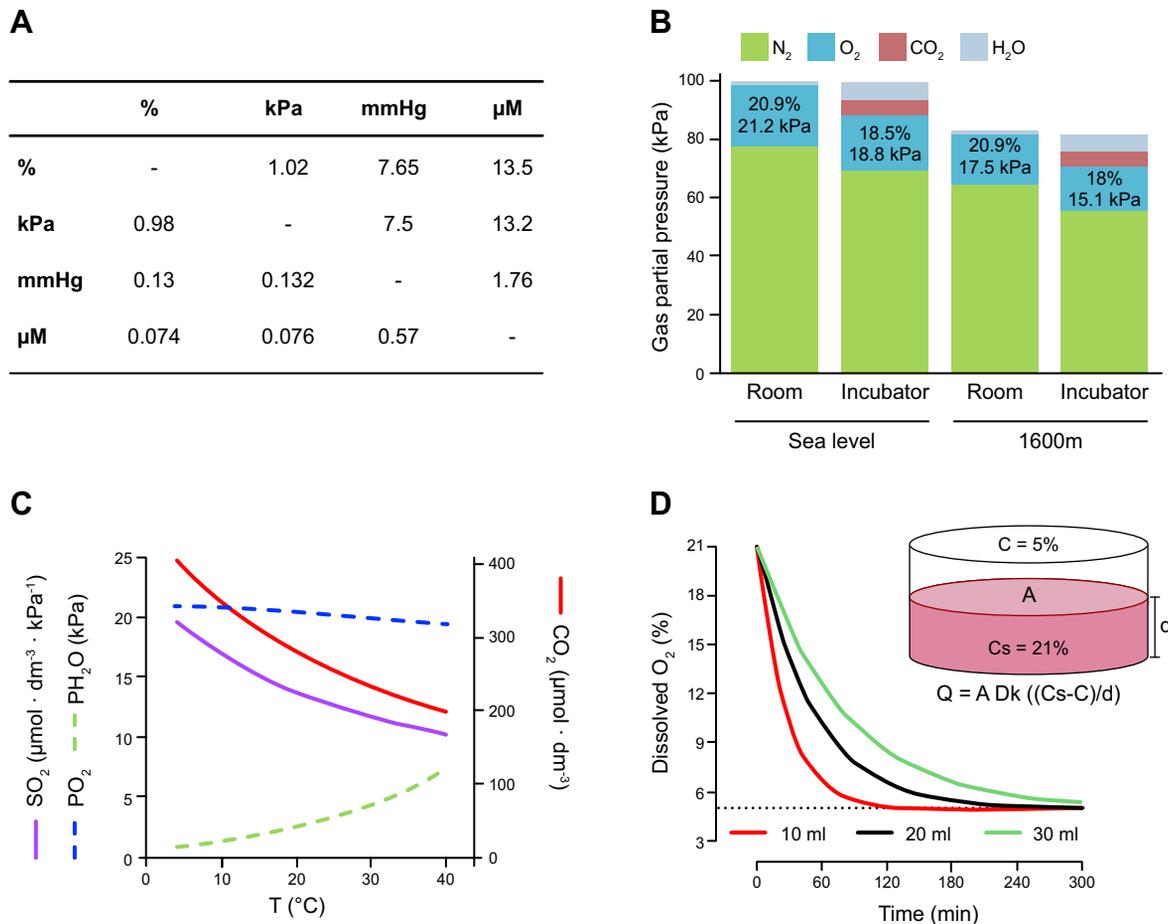
The often-quoted 20.9 kPa refers strictly to standard dry atmospheric air (see **FIGURE 5B**). However, most cell culture is conducted within a controlled atmosphere of 95% air: 5%  $CO_2$ . Moreover, incubators are normally run at 75% humidity (compared with ~50% at room air) to prevent excessive evaporation of medium. Considering this, the actual  $PO_2$  within a standard cell culture incubator is ~18.5 kPa (at sea level; **FIGURE 5**) (377, 420). This value is even lower at high altitude, as the water vapor and  $CO_2$  components are a constant ~47/35 mmHg even under reduced atmospheric pressure. Most atmosphere-regulated cell culture chambers used to perform research under  $O_2$  conditions different from atmospheric alter the  $PO_2$  at the expense of nitrogen, thereby maintaining atmospheric pressure. Moreover, many are engineered to run at slightly higher atmospheric pressure at sea level (101.33–101.78 kPa) to obviate fluctuations in  $PO_2$  due to changes in altitude.

### B. Achieving the Appropriate Dissolved $O_2$ Level In Vitro

Modulating the gaseous atmosphere with respect to  $O_2$  is straightforward, yet cells do not exist in contact with  $O_2$  in the gas phase, with the possible exception of lung epithelial cells (see sect. VIA). The evolution of red cells as an intricate and highly efficient  $O_2$  transporter bears testament to the poor solubility of this gas in solution. In contrast to  $CO_2$ , which reaches equilibrium in solution within minutes,  $O_2$  dissolves too slowly to be overlooked in experimental protocols.

#### 1. Factors affecting $O_2$ solubility

Efforts to determine  $O_2$  solubility are spearheaded by oceanography and hydrometallurgy communities, with  $O_2$  in solution used for numerous industrial processes. Initially defined by Henry's Law (235) (see sect. IIIA), the solubility of a gas in pure water is related to the temperature of water and the gaseous pressure. Such relationships have been confirmed more recently, both experimentally and computa-



**FIGURE 5.** Parameters of atmospheric  $\text{O}_2$  levels within the cell culture environment. *A*: An approximate  $\text{O}_2$  unit conversion table with the multiplication factor required to convert current unit (row) into desired unit (column). *B*: The atmospheric composition at sea level, at 1,600 m above sea level, and within a standard culture incubator (5%  $\text{CO}_2$ , 75% humidity). *C*: The  $\text{P}_{\text{H}_2\text{O}}$  and  $\text{P}_{\text{O}_2}$  in pure water are plotted across a range of temperatures, and the concentration ( $c_{\text{O}_2}$ ) and solubility ( $S$ ) of  $\text{O}_2$  calculated based on the equations of Benson and Krause (32), as summarized by Forstner and Gnaiger (159). *D*: An application of Fick's second law of diffusion to describe the time required for culture medium to equilibrate following exposure to an atmosphere of different  $\text{O}_2$  content. A, liquid surface area; C, new concentration;  $C_s$ , saturating concentration; D, diffusivity of  $\text{O}_2$  in liquid; d, liquid depth; k, solubility of  $\text{O}_2$  in liquid; Q, rate of diffusion.

tionally [see Battino (1981) (25) and Ming and Zhenhao (2010) (399) for a review], and are illustrated in **FIGURE 5C**. The relationship between temperature, pressure, and  $\text{O}_2$  solubility is further defined by the Bunsen adsorption coefficient ( $\alpha$ , measured in  $\text{dm}^3 \cdot \text{dm}^{-3} \cdot \text{kPa}^{-1}$ ). From  $\alpha$ , the solubility of  $\text{O}_2$  ( $\text{S}_{\text{O}_2}$ ) is defined here in  $\mu\text{mol} \cdot \text{dm}^{-3} \cdot \text{kPa}^{-1}$  by:

$$\text{S}_{\text{O}_2} = \alpha / (\text{molar volume} \times 101.325)$$

$$[\text{O}_2 \text{ molar volume} = 22.393] \quad (4)$$

$$\text{S}_{\text{O}_2} = \alpha / 2269.9$$

This initial equation was refined further by Benson and Krause (32, 33) in their proposal of units of standard concentration ( $c^*$ ), defined as the concentration of dissolved  $\text{O}_2$  per volume of solution. As such,  $c_{\text{O}_2}^*$  in pure water under standard atmospheric conditions is defined as:

$$c_{\text{O}_2}^* = \text{S}_{\text{O}_2} \times (\text{P}_{\text{atm}} - \text{P}_{\text{H}_2\text{O}}) \times \text{FO}_2 \quad (5)$$

Temperature also strongly impacts the  $\text{P}_{\text{H}_2\text{O}}$  of a given atmosphere, with higher temperature increasing evaporation and thus increasing  $\text{P}_{\text{H}_2\text{O}}$  at the expense of  $\text{O}_2$ . The salinity of a solution also impacts  $\text{O}_2$  solubility, as demonstrated in pioneering work from Sechenov (524) and tabulated for convenience elsewhere (399). With relevance to physiology, the vast majority of experimental work is conducted in solutions of a reasonably similar salinity, and thus, this factor can be assumed constant. As shown in **FIGURE 5C**, the solubility of  $\text{O}_2$  in pure water at  $37^\circ\text{C}$  is  $\sim 77\%$  than at  $20^\circ\text{C}$ , resulting in  $\sim 30\%$  less  $\text{O}_2$  in solution. This merits consideration when comparing experimental data derived at room temperature with that at  $37^\circ\text{C}$ . Moreover, with relevance to sect. IVB2, the equilibration of culture medium from room air to physiological  $\text{O}_2$  levels is significantly more time efficient when the solutions are cooled to  $4^\circ\text{C}$ .

**Table 1.** Permeability of commonly used plastic culture surfaces

Surface	$D$ ( $10^{-5}$ cm <sup>2</sup> s <sup>-1</sup> )	$k$ ( $10^{-9}$ mol cm <sup>-3</sup> mmHg <sup>-1</sup> )	Reference
Medium	3.3	1.2	(371, 389)
	2	1.2	(671)
	2.8	1.3	(112, 466)
Polystyrene	0.01	8.6	(466)
PDMS	2.2	12.2	(466)
Teflon	0.03	5.1	(311)

$D$ , O<sub>2</sub> diffusivity;  $k$ , O<sub>2</sub> solubility coefficient; PDMS, polydimethylsiloxane; Teflon, polytetrafluoroethylene.

## 2. Equilibration in solution

Mass diffusion was first described by Fick in 1855 in a seminal piece of work from which we now derive Fick's laws of diffusion (153). In the absence of cells, O<sub>2</sub> equilibration between atmosphere and medium follows Fick's second law and can therefore be estimated using a one-dimension, single-compartment diffusion model. This is described by the equation  $Q = AK[(C_s - C)/d]$  (458), in which  $Q$  is the rate of O<sub>2</sub> diffusion ( $\mu\text{M min}^{-1}$ ),  $A$  is the surface area (cm<sup>2</sup>),  $K$  is Krogh's constant (derived from the diffusivity and solubility of O<sub>2</sub>),  $C_s$  and  $C$  are the saturating and desired Po<sub>2</sub> (kPa), respectively, and  $d$  is the depth of the medium (cm). To frame this scenario in the context of in vitro cell culture, imagine a 90-mm petri dish filled with 20 ml of medium and placed within a sealed chamber at a Po<sub>2</sub> of 5 kPa. Using Fick's laws, we can estimate that this medium will take ~2 h to equilibrate to 5 kPa, as shown in **FIGURE 5D**, in agreement with experimentally derived values (10, 420). This rate can be increased by dividing the 20 ml into two 90-mm petri dishes, thereby doubling the effective surface area for diffusion. Dissolved O<sub>2</sub> levels achieved in culture medium are a critical and often underestimated factor in conducting experiments under low O<sub>2</sub> conditions aimed at recapitulating O<sub>2</sub> levels in vivo. Thus, addition of poorly equilibrated, overly oxygenated medium to cells preadapted to low O<sub>2</sub> conditions may generate a reaction akin to the reoxygenation phenomena observed during stroke and myocardial infarction.

## 3. Accounting for plastic leaching

The equations described above assume that the only path by which O<sub>2</sub> equilibrates in solution is through the gas/liquid interface. Although by far the most important source, plastic is not completely impermeable to O<sub>2</sub>, and hence, O<sub>2</sub> can diffuse through the sides and bottom of culture dishes to varying degrees. This is largely deemed negligible by most researchers based on the extremely low diffusivity and solubility coefficients of standard polystyrene cultureware (see **TABLE 1**). The effect of substrate O<sub>2</sub> permeability on pericellular Po<sub>2</sub>, specifically comparing impermeable polystyrene with permeably substrates such as silicone rubber or

Teflon membranes, has been demonstrated mathematically (274, 466) and experimentally (659, 690). Notably, Powers et al. (466) incorporated substrate permeability into the most widely adopted mathematical model to determine pericellular Po<sub>2</sub> (671), accounting for the surface area in contact with cells and substrate O<sub>2</sub> diffusivity and solubility. This was intentionally left out in **TABLE 2** for greater clarity, but essentially involves an additional  $\alpha$  value for the substrate. When monolayer O<sub>2</sub> consumption substantially outweighs O<sub>2</sub> diffusion capacity, using a gas-permeable culture substrate can be an effective way to minimize unintentionally hypoxic conditions. On a separate note, plasticware left at room air (Po<sub>2</sub> 20 kPa) will accumulate a significant amount of O<sub>2</sub>, and this will eventually leach out when placed in an environment of lower Po<sub>2</sub>, thus acting as a O<sub>2</sub> source (558). When plastic equilibrated to 20 kPa was placed within an anoxic water solution, dissolved Po<sub>2</sub> reached ~12 kPa after 60 h (558). Although specific rates of leaching will depend on the plastic composition and its mass/surface, it is highly advised that when working with cells preadapted to a specific low Po<sub>2</sub>, all plasticware (pipette tips, stripettes, petri dishes, and culture flasks) be pre-equilibrated at the appropriate Po<sub>2</sub> before use. This is of particular importance when working with near anoxic con-

**Table 2.** Equations used to predict pericellular Po<sub>2</sub> in vitro

Equation	Reference
$h = k[(P_s - P)/V]$	(559)
$-DdP/dx = VpP/[k(K_m + P)]$	(671)
Solved: $\theta = 0.5 [1 - \alpha - \beta_M + [(1 + \alpha + \beta_M)^2 - 4\alpha]^{0.5}]$ $P = P_s - (Vp/60D)(760/k)(h/A)$	(389)
$-DdP/dx = -Dk(P_x - P_s)/h$	(371)
$1 - \theta = [F_V + (1 - F_V)(\theta/\beta_V + \theta)](\theta/\beta_M + \theta)\alpha^*$ (Solved)	(466)
$P = [(P - P_s)DA]/Vh$	(596)

$\alpha$ ,  $dVp/DkP_s$ ;  $\beta_M = K_m/P_s$ ;  $\beta_V = K_v/P_s$  (where  $K_v$  is a fitted constant describing  $dV/dP_s$ );  $\theta$ ,  $P/P_s$ ;  $A$ , surface area;  $D$ , O<sub>2</sub> diffusivity in liquid;  $d$ , fluid height;  $F_V$ ,  $V_{\text{max},O}/V_{\text{max},O}$ ;  $k$ , O<sub>2</sub> solubility in liquid;  $K_m$ , Po<sub>2</sub> when O<sub>2</sub> consumption is 0.5max;  $P$ , cell density;  $P$ , pericellular Po<sub>2</sub>;  $P_s$ , Po<sub>2</sub> at gas/liquid interface;  $V$  = O<sub>2</sub> consumption rate ( $V_{\text{max}}$ ).

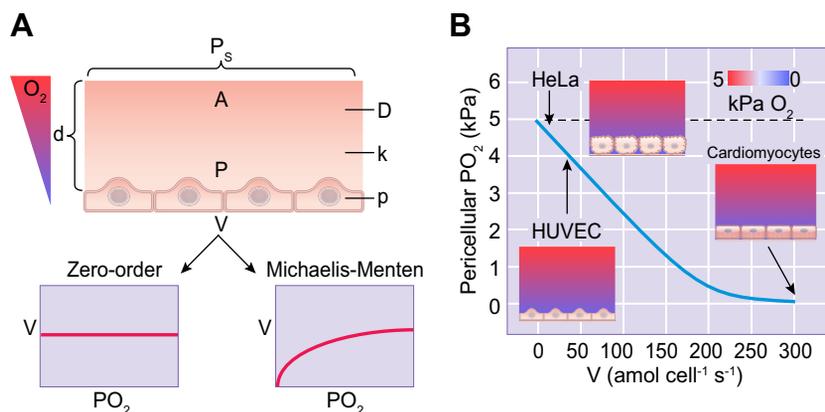
ditions, in which even small amounts of  $O_2$  leaching can severely compromise experiments, and we would always recommend measuring  $PO_2$  in the medium/monolayer under such conditions to be confident a sufficiently low  $PO_2$  is achieved and maintained.

### C. Accommodating $O_2$ Diffusion and Monolayer Consumption

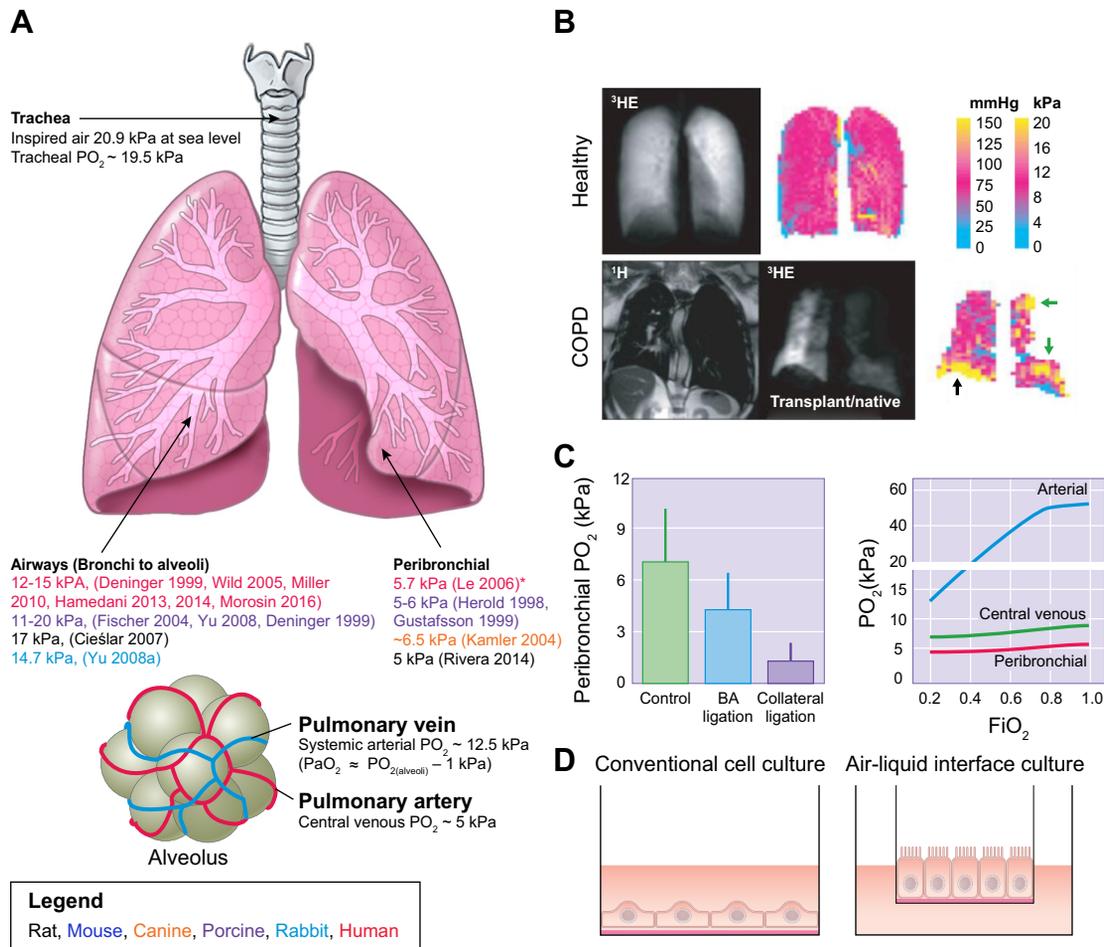
One of the most common, and incorrect, assumptions made during in vitro research is that intracellular  $PO_2$  and ambient  $PO_2$  are synonymous. The consumption of  $O_2$  by cells, coupled to the poor solubility of  $O_2$  in solution, generates a gradient between the headspace and monolayer proportional to the rate of monolayer  $O_2$  consumption (389). Without compensation, cell cultures may inadvertently experience culture-induced hypoxia by consuming  $O_2$  faster than it can diffuse, as discussed in sect. IV-D. Under these conditions, it may become difficult to differentiate the cellular response to physiological and hypoxic  $O_2$  levels, resulting in incorrect interpretations. Compounding this problem has been the lack of technology to accurately monitor intracellular  $O_2$  levels in living cells (see sect. II). In lieu of physical measurements, many have relied on an derivation of Fick's second law to predict pericellular  $PO_2$  in monolayers cultured under static conditions (26, 199, 371, 384, 389, 421, 466, 559, 596, 659, 671). By considering oxygen diffusion within a culture dish as a one-dimensional diffusion/reaction, cell boundary  $O_2$  levels can be predicted and, given that  $O_2$  can freely diffuse across the plasma membrane (562), this approximately equates to generalized intracellular  $O_2$  levels (FIGURE 6A). Although exact equa-

tions differ between studies (summarized in TABLE 2), the common critical variables in determining pericellular  $PO_2$  were always, as expected, ambient  $PO_2$ , cell density, cellular  $O_2$  consumption, and medium height. The most comprehensive equation to date has been put forward by Powers et al. (466), in which the equation by Yarmush and colleagues (671) was adapted to reflect the change in cellular  $O_2$  consumption as a function of ambient  $PO_2$ . Common to a number of such studies was the conclusion that hepatocyte monolayers [rabbit (559), human (671), and HepG2/3B cell lines (389)] are most likely severely hypoxic even when cultured under room air, which has subsequently been demonstrated experimentally (see sect. VIE).

These theoretical observations have been corroborated using electrode and fluorescence-based probes to experimentally determine pericellular  $PO_2$  in monolayer cultures. Increased cell density has been shown to decrease pericellular  $PO_2$  in monolayers of rat hepatocytes (250, 421), human dermal fibroblasts (581), T-47D breast cancer cells (453), and peripheral blood mononuclear cells (PBMC) (63). Notably, comparisons between cell types (389) revealed the importance of considering cell type-specific differences in density at confluence in addition to  $O_2$  consumption rate per cell. Although mesangial cells had similar  $O_2$  consumption rates to Hep3B cells ( $\sim 9$  nmol/min/mg protein), vastly different pericellular  $PO_2$  (14.6 versus  $\sim 0$  kPa at room air) results from differences in monolayer protein content, reflecting morphological differences in cell types (389). The other significant variable, fluid height, has also been confirmed experimentally (77, 371, 389, 421, 581) and is likely the most easily controlled to maintain the appropriate pericellular  $PO_2$ . Using the equation first described by Stevens in



**FIGURE 6.** Predicting pericellular  $PO_2$  in cell monolayers. **A:** Parameters critical in predicting pericellular  $PO_2$  in cultured cells. The value of  $V$  ( $O_2$  consumption rate) can be simplified by considering a zero-order relationship between  $V$  and  $PO_2$ , as described by Yarmush et al. (671) or modeled using Michaelis-Menton kinetics as described by Powers et al. (466). As we know,  $O_2$  consumption is affected by  $O_2$  availability, predictions will have more accuracy if  $V$  is modeled using the latter. **B:** Illustration of the relationship between pericellular  $PO_2$  and cellular  $O_2$  consumption, with commonly used cell types annotated according to published values. Cell types with high  $O_2$  consumption such as cardiomyocytes or hepatocytes can initiate a self-inflicted hypoxia when ambient  $PO_2$  is low.  $A$ , surface area at gas/liquid interface;  $D$ ,  $O_2$  diffusivity in liquid;  $d$ , fluid height;  $k = O_2$  solubility in liquid;  $P$ , cell density;  $P$ , pericellular  $PO_2$ ;  $P_s$ ,  $PO_2$  at gas/liquid interface;  $V$ ,  $O_2$  consumption rate ( $V_{max}$ ).



**FIGURE 7.** Oxygen distribution in the lung. **A:** An illustration depicting the known distribution of  $PO_2$  in the mammalian lung, combining experimentally derived values with theoretical values derived from established physiology. Pulmonary arterial  $PO_2$  ( $PaO_2$ ) is usually slightly lower than alveoli  $PO_2$  as outlined in the equation  $PaO_2 = PO_{2(\text{alveoli})} - 1$  kPa and discussed in Section IIIA. **B:** Whole lung  $PO_2$  mapping using  $^3\text{He}$ -based magnetic resonance imaging (MRI) scanning in healthy volunteers and in patients with chronic obstructive pulmonary disease (COPD). Taken with permission from Miller et al. (396). **C:** Peribronchial  $PO_2$  values determined using microelectrode penetration upon (left) ligation of the bronchial artery (BA) or bronchial collaterals in dog [adapted with permission from Kamler et al. (282)], and (right) increases in forced inspiratory  $PO_2$  ( $FiO_2$ ), [adapted from Herold et al. (236)]. Both examples illustrate the dependence of peribronchial  $PO_2$  on bronchial artery perfusion rather than the bronchi themselves. **D:** Comparison between conventional cell culture, in which the monolayer is completely submerged in medium, and air/liquid interface culture used to maintain differentiated primary epithelial cells. Transwell chambers are used to elevate the monolayer, exposing the apical surface to the atmosphere while maintaining basolateral access to medium through a microporous membrane.

1965 (559), one can calculate the required medium height to achieve the desired pericellular  $PO_2$  as recently reviewed (462). Other methods to control pericellular  $PO_2$  include varying the permeability of the base substrate (466, 659) to bypass the need for  $O_2$  to diffuse through the medium and increasing ambient  $PO_2$  to compensate for monolayer consumption and poor diffusivity (75).

As illustrated in **FIGURE 6B**, cellular  $O_2$  consumption rates vary considerably between cell types: from  $4 \times 10^{-5}$ – $0.02$   $\text{amol } O_2 \text{ cell}^{-1} \text{ s}^{-1}$  in red blood cells (179, 510), to as high as  $200$ – $500$   $\text{amol } O_2 \text{ cell}^{-1} \text{ s}^{-1}$  in cardiomyocytes and hepatocytes (20, 165, 199, 478). These differences between cell types most likely arise from differences in metabolic activity

and mitochondrial content/density. As monolayer  $O_2$  consumption is a major determinant of  $O_2$  diffusion, and ultimately pericellular  $PO_2$ , low consuming cell types are likely to experience much greater intracellular  $PO_2$  than those that consume  $O_2$  more rapidly when placed in the same environment. Sekine and colleagues (521) illustrate this concept by comparing pericellular  $PO_2$  values and oxygen consumption rates in monolayers of human induced pluripotent stem cell cardiomyocytes, rat cardiomyocytes, human aortic smooth muscle cells, and cardiac fibroblasts. Cardiomyocyte monolayers consume significantly more  $O_2$  than the noncardiomyocyte cell types, and this is reflected in a much steeper gradient between ambient and pericellular  $PO_2$  (see **FIGURE 6B**). Similar results were obtained when comparing medium

$\text{PO}_2$  in monolayers of human umbilical vein endothelial cells (HUVEC; low consuming, large size) and human embryonic stem cells (hESC; high consuming, small size) (2). If cellular  $\text{O}_2$  consumption significantly outweighs  $\text{O}_2$  diffusion capacity, a condition of self-inflicted hypoxia may arise at sufficiently low ambient  $\text{PO}_2$  (77, 421) (FIGURE 6B). In reality, because cellular  $\text{O}_2$  consumption decreases with ambient  $\text{PO}_2$  (88, 211, 441, 443), the accuracy of many of the predictions (which assume a constant rate of  $\text{O}_2$  consumption) are limited under extreme hypoxia. It is more likely that under these conditions, intracellular  $\text{O}_2$  levels in high-consuming cell types range around a value more conducive to viability under the control of negative feedback mechanisms orchestrated by HIF (178). In support of this, rat hepatocytes cultured at a  $\text{PO}_2$  of 4 kPa stain strongly with the hypoxic marker Hypoxyprobe (indicating cytosolic  $\text{PO}_2$  below 1 kPa) but retain reasonable viability, suggesting a sufficient supply of  $\text{O}_2$  to maintain function (421).

One technique used extensively to alleviate problems associated with poor oxygenation in vitro has been the use of bioreactor-type culture conditions in which medium is continuously stirred. Under these conditions, cellular oxygenation can occur through convection in addition to diffusion, greatly increasing  $\text{O}_2$  supply (172). Medium agitation also forms a critical component of a successful microbial culture system, in which bacterial or fungal cells are cultured in suspension at very high densities and therefore require additional oxygenation. Such conditions are not generally appropriate for the majority of adherent cell lines without prior immobilization [see bioartificial livers, for an example (579)], although some success has been obtained using roller bottle technology, in which adherent cells are cultured on the side of a cylindrical device placed horizontally on an orbital shaker (175, 462). Furthermore, microfluidic perfusion has received increasing attention in recent years and also solves several problems associated with monolayer oxygenation, especially when constructed using plastic with a high  $\text{O}_2$  permeability coefficient. Many of these techniques can create adequate monolayer oxygenation, even though more effort and expense is required, and thereby provide more accessible means of altering existing culture conditions to improve oxygenation.

## D. Evidence for Compromised Oxygen Delivery In Vitro

As eluded to above, the concept of self-inflicted hypoxia is not restricted to theory. Confluent HepG2 cultures rapidly (within 1 h) deplete medium  $\text{PO}_2$  to  $<0.1$  kPa even at an ambient  $\text{PO}_2$  of  $\sim 20$  kPa. In these studies, an hypoxic status was confirmed by continuous secretion of the HIF target protein erythropoietin (EPO) and an increase in lactate production, indicative of a switch from oxidative phosphorylation to glycolysis (659). Similar observations were made by Metzen et al. (389) and Bhatia et al. (421) in HepG2 and

rat hepatocytes, respectively. Compromised  $\text{O}_2$  delivery in vitro is not confined to hepatocyte cultures, because large culture  $\text{O}_2$  gradients have been reported using a number of different cell types under standard culture conditions and low ambient  $\text{PO}_2$  (see TABLE 3). Traditional micromanipulator-mounted electrode methodologies have largely been superseded by fluorescence- and phosphorescence-based techniques, which can provide a more accurate determination of pericellular  $\text{PO}_2$  in culture dishes. Using immobilized luminescent dyes (see sect. IIC), large culture gradients have been demonstrated in cultures of hESC (2, 320) and Caco-2 intestinal epithelial cells (690). Meanwhile, cell-permeable phosphorescent nanoparticles have been used to monitor intracellular (cytosolic)  $\text{PO}_2$  in mouse embryonic fibroblasts (151), cortical neurons (114), and in HUVEC (75). Hence, intracellular or pericellular  $\text{PO}_2$  provides a more accurate parameter when translating in vitro experiments to an in vivo setting.

## E. Maintaining the Appropriate Environment for the Duration of Culture

Culture of mammalian cells under reduced  $\text{O}_2$  environments has generally been undertaken using three types of equipment: 1) an airtight, gassed chamber placed within a standard  $\text{CO}_2$  incubator, 2) a tri-gas incubator, or 3) a dedicated  $\text{O}_2$ -regulated workstation, with cost and infrastructure requirements increasing accordingly. The former is most widely used because of the relatively low price and ease with which it can be accommodated into existing culture infrastructure, although dedicated chambers generally have limited multiuser space and accessibility. Tri-gas incubators are variations of standard  $\text{CO}_2$ -regulated cell culture incubators in which an additional  $\text{N}_2$  gas input is provided, with which the  $\text{PO}_2$  can be manipulated to a required level. Tri-gas incubators offer increased capacity for multiusers, especially units equipped with independent, modular compartments. However, both these types of equipment suffer from an important disadvantage when used for long-term culture of cells under defined low  $\text{O}_2$  conditions. Cells need to be removed from the chamber or tri-gas incubator to feed, monitor, and perform any required subculture or experimental treatments. Thus, cells are re-exposed to hyperoxic atmospheric levels of  $\text{O}_2$ . Such fluctuations in the resultant pericellular  $\text{PO}_2$  induce a phenotype distinct from that of cells maintained long term under a defined level of  $\text{O}_2$  (289, 437, 640). Indeed, direct comparisons between culture in tri-gas incubators and dedicated  $\text{O}_2$ -regulated workstations demonstrate that repeated re-exposure to atmospheric  $\text{O}_2$  levels during culture is detrimental to human mesenchymal stem cell (MSC) growth (289). Medium and pericellular  $\text{PO}_2$  require hours to re-equilibrate to a required  $\text{PO}_2$  level even when only transiently exposed ( $\sim 5$  min) to atmospheric levels (320, 404, 690). Such technical problems associated with in vitro cell culture mimic reperfusion injury, commonly following restoration of cerebral or myo-

**Table 3.** Pericellular  $P_{O_2}$  levels under standard culture conditions

Cell Type	Method	$P_{O_2}$ (kPa)		Reference
		Ambient*	Pericellular	
Rat hepatocytes	electrode	18	8	(250)
		13	5.8	
		4	1.5	
HepG2/3B	electrode	18	<0.1	(659)
HepG2/3B	electrode	18	<0.1	(389)
			<0.1	
BAEC	electrode	18	10.4	(389)
HUVEC hEPC	Fiber-optic probe	21	19–20	(2)
		5	3.4	
		1	0.7	
HASMC	ESR	21	18.9	(442)
HUVEC	MitoXpress	18.5	~17	(75)
		5	3.5	
hiPSC-CM	electrode	21	10.4	(521)
HASMC			16.4	
HCF			18.6	
HMVEC			17.9	
Rat-CM			14.9	
mESC	Fiber-optic probe	2	2	(404)
hESC	Fiber-optic probe	21	4–5	(2)
iPSC		5	1.5	
		1	0.4	
MEF	MitoXpress	21	8.1	(151)
		10	3.8	
hESC	Fiber-optic probe	21	15	(320)
		5	≤1	
Rat mesangial LLC-PK <sub>1</sub>	electrode	18	14.7	(389)
			<0.1	
Type II alveolar	electrode	18	13.3	(371)
Dermal fibroblasts	electrode	18	12	(581)
		2	0	
T-47D	electrode	21	1–18	(453)
MING (β cells) PANC-1	Pimonidazole HIF-1α	20	–	(511)
		10	–	
		7	+	
		5	++	
		3	++	
0	+++			
Trophoblast	electrode	21	<1	(77)
hESC	Fiber-optic probe	21	15	(320)
		5	≤1	
PMN	Oxodish	21	0–14	(63)
		4	<1	
RAW 264.7	Patch probe	20	~8	(690)
		5	~1.5	

*Continued*

Table 3.—Continued

Cell Type	Method	Po <sub>2</sub> (kPa)		Reference
		Ambient*	Pericellular	
Caco-2	Patch probe	19 1	~4–5 <0.1	(114)
Cortical neurons	MitoXpress	18–20	14–16	(250)

\*Unless clearly defined, ambient Po<sub>2</sub> was determined to be either 21 or 18 kPa based on the inclusion/absence of 5% CO<sub>2</sub> and humidification. BAEC, bovine aortic endothelial cell; ESR, electron spin resonance; hESC, human embryonic stem cell; HASMC, human aortic smooth muscle cell; HCF, human cardiac fibroblast; hEPC, human endothelial progenitor cell; hiPSC-CM, human induced pluripotent stem cell–cardiomyocyte differentiated; HMVEC, human cardiac microvascular endothelial cell; hPSC, human pluripotent stem cell; HUVEC, human umbilical vein endothelial cell; iPSC, induced pluripotent stem cell; MEF, mouse embryonic fibroblast; mESC, mouse embryonic stem cell; PMN, peripheral blood mononuclear cells; Rat-CM, rat cardiomyocytes.

cardial blood after infarction. Re-exposure to atmospheric Po<sub>2</sub> can be avoided completely by using a dedicated O<sub>2</sub>-regulated workstation, where access to cells for subculture and treatment is permitted through gas-tight glove ports and transfer chambers. It is for this reason that we strongly recommend that any work investigating the effects of prolonged culture under well-defined low Po<sub>2</sub> be conducted using a dedicated O<sub>2</sub>-regulated workstation.

## V. CELLULAR OXYGEN SENSING: WHEN IS LOW O<sub>2</sub> HYPOXIC?

Having established the difficulties in accurately predicting and controlling monolayer oxygenation in vitro, a consideration for how cells sense the difference between normoxic and hypoxic Po<sub>2</sub> is now relevant. The question posed relates to the understanding that physiological oxygenation varies by so much in vivo that the use of terminology like hyperoxia, normoxia, and hypoxia should be used contextually rather than absolutely and should always be defined quantitatively for better interpretation. Each cell type has unique responses to a reduction in available O<sub>2</sub>. For example, endothelial cells release vascular endothelium–derived growth factor (VEGF) and nitric oxide (NO) to initiate vasodilation and angiogenesis in an attempt to increase local blood flow, thereby normalizing tissue O<sub>2</sub> distribution (351, 536, 630). A more generalized hypoxic response is orchestrated predominantly by HIFs, with additional contributions from less well-defined pathways. The relevance of these mechanisms in the context of in vitro normoxia remains to be defined fully, because they have evolved to respond to acute reductions in Po<sub>2</sub> within (patho)physiological levels, and not the substantial reductions imposed in the majority of studies in vitro (room air to 1–3 kPa). Thus, the study of cellular phenotypes under low O<sub>2</sub> generally requires culturing cells for a sufficient period to allow adaptation to the new baseline [O<sub>2</sub>]. Several excellent articles have reviewed the general and state-of-the-art literature concerning how cells sense O<sub>2</sub> (476, 516, 522, 575), and as such, only the most well-established cellular O<sub>2</sub> sensors will be covered here. Particular emphasis will be placed on their

relevance under physiological O<sub>2</sub> levels in terms of the Po<sub>2</sub> at which they have been shown to be active. This will be followed by a brief discussion of how the duration of exposure to low O<sub>2</sub> can influence the interpretation of experimental data.

### A. Cellular Oxygen Sensors

#### 1. HIFs

Several excellent reviews have been published on the physiology and biochemistry of HIFs (472, 504, 516, 522), and therefore HIFs will only be briefly discussed. HIFs are evolutionarily conserved transcription factors expressed in all eukaryotic organisms as three  $\alpha$  isoforms (HIF1–3) and a  $\beta$  subunit. The vast majority of research to date has focused on HIF-1, which regulates the acute and reactive phase of the hypoxic response in most cell types (257, 549). Although the  $\beta$  subunit is constitutively expressed and not actively degraded, the  $\alpha$  subunit is posttranslationally modified through O<sub>2</sub>-dependent hydroxylation at prolyl residues [by prolyl hydroxylases (PHD)], which targets the subunit for degradation (35, 134), or at asparagine residues by factor inhibiting HIF-1, which interferes with its binding to transcriptional coactivators (238, 322, 323). Thus, when intracellular O<sub>2</sub> availability decreases, these enzymes are no longer able to hydroxylate HIF $\alpha$  subunits, resulting in the formation of a transcriptionally competent stable  $\alpha/\beta$  dimer. This can then translocate to the nucleus where it binds hypoxia-response elements, initiating the transcription of hypoxia-sensitive genes. Such genes encode proteins such as VEGF (162, 536), EPO (630), and glucose transporter 1 (128), which function collectively to either increase O<sub>2</sub> delivery or reduce cellular O<sub>2</sub> consumption. It was traditionally considered that a large degree of redundancy exists between HIF-1 $\alpha$  and -2 $\alpha$  (549, 667), which itself has fewer selective targets (120, 193, 257, 444, 569, 599, 634). However, recent pangenomic screens (503, 514, 515) have identified a large number of HIF response element (HRE) binding sites with distinct isoform binding affinities, despite an identical core recognition sequence (RCGTG). Such

variance may represent different topographical chromatin binding locations, affinity for HIF- $\beta$  binding partner, and/or the involvement of other transcription factors, most notably AP-1 (321, 503). Comparatively little is known about HIF-3 $\alpha$ , but it is thought to act as a negative regulator of HIF-1 and -2 (219).

The  $K_m$  for O<sub>2</sub> of the reaction catalyzed by PHD ranges between 140 and 250  $\mu$ M (~10–20 kPa) (243, 517), and thus, O<sub>2</sub> may be a rate-limiting substrate under atmospheric O<sub>2</sub> conditions. Despite this, HIFs are not constitutively stabilized in cells at physiologically normoxic levels (on average 5 kPa), otherwise organisms would have no reactive response to further reductions during genuine hypoxia. Persistent stabilization is prevented by HIF-dependent negative feedback mechanisms including specific interactions with microRNA 210 (631) and ROS (254), upregulation of PHD 2 and 3 (36, 106, 178, 372), and the global impact of HIF-induced proteins to increase intracellular O<sub>2</sub> levels. Thus, any reduction in O<sub>2</sub> availability is addressed by transient stabilization of HIF-1 $\alpha$ , and the upregulation of associated regulated proteins, followed by pathway normalization at a new baseline reflecting the altered O<sub>2</sub> levels. A question that remains unsolved in HIF hydroxylation is the concept of range finding; oxygen-dependent regulation of HIF is observed in a variety of tissues existing across a huge variety of O<sub>2</sub> levels (476). The high  $K_m$  of PHD enzymes for O<sub>2</sub> has led many to conclude that absolute O<sub>2</sub> levels are perhaps of secondary importance in the mechanism by which cells sense O<sub>2</sub> and that complimentary signals may further modulate hydroxylase activity. To date, alternative signals include ROS (74, 378), intracellular [Fe<sup>2+</sup>] (306), and competing hydroxylase substrates (91). Inclusion of these additional parameters in the mechanism of HIF O<sub>2</sub> sensing creates an increasingly complex model which may offer insight into the range-finding capabilities of the system (476), a concept critical for defining physiological normoxia.

## 2. Mitochondria and/or superoxide

Given their central role in O<sub>2</sub> homeostasis and intracellular signaling, mitochondria are prime candidates for intracellular O<sub>2</sub> sensors. Mechanisms by which these organelles are thought to transduce changes in O<sub>2</sub> levels revolve around changes in either intracellular redox or energy states (or both) (74, 633). Limitations in O<sub>2</sub> supply would logically lead to reductions in mitochondrial ATP generation, which subsequently activates AMP-dependent protein kinase, a cellular energy sensor (220, 556), although some have argued this occurs because of ROS generation and not changes in ADP/ATP (132). AMP-dependent protein kinase, in turn, targets several transcription factors to repress fatty acid biosynthesis and upregulate proteins involved in glycolysis, resulting in a metabolic shift away from O<sub>2</sub>-consuming oxidative phosphorylation (221). Pharmacological inhibition of the ETC can mimic hypoxic responses

(121, 392), although others report an abolition in O<sub>2</sub> sensing following ETC inhibition (635). One major limitation to the energy state hypothesis of mitochondrial O<sub>2</sub> sensing is that the P50 of cytochrome *c* oxidase for O<sub>2</sub> is ~0.07 kPa (181), and thus, ATP production would not be expected to decrease until cytosolic Po<sub>2</sub> falls very low. However, some have suggested that the affinity of cytochrome *c* oxidase for O<sub>2</sub> is modified substantially by cellular reducing agents [GSH and NAD(P)H], suggesting that O<sub>2</sub> may become rate limiting at much higher levels than previously predicted (633, 653). The generation of superoxide anions by the ETC has formed the basis of intense debate in the context of mitochondrial O<sub>2</sub> sensing, with both decreases and increases in mitochondrial superoxide (O<sub>2</sub><sup>•-</sup>) generation reported to mediate O<sub>2</sub> sensing. On one side, reductions in O<sub>2</sub> availability would logically result in reductions in O<sub>2</sub><sup>•-</sup> production, which in turn, would cause the cytosolic environment to become more reduced, affecting many redox-sensitive pathways (15, 480, 641). Conversely, others have reported a paradoxical increase in superoxide generation in mitochondria during hypoxia (74, 206, 207, 373, 450, 609, 636), resulting from enhanced electron leak within the ETC.

Mitochondria are not the only source of ROS within the cytosol, and indeed, other enzymatic sources have been implicated as O<sub>2</sub> sensors. Because NAD(P)H oxidases (NOX) function to generate ROS with a reported P50 for O<sub>2</sub> of ~1.7 kPa (31), it is tempting to speculate that NOX serve as a key cytosolic O<sub>2</sub> sensors (633). Indeed, mice lacking an essential subunit of the NOX2 isoform (gp91<sup>phox</sup>) exhibit impaired O<sub>2</sub> sensing (168), although this remains controversial (14, 633). Both increases (229, 375) and decreases (100) in NOX-derived ROS generation have been reported during hypoxia.

## 3. Gaseous messengers

A new O<sub>2</sub>-sensing mechanism has emerged in recent years focusing on the interplay between two physiological gaseous messenger molecules, carbon monoxide (CO) and hydrogen sulfide (H<sub>2</sub>S) (468). The effects of CO on hypoxia-induced ventilation have been well known for 50 yr (352), yet the finding that it is produced endogenously highlighted its possible involvement in O<sub>2</sub> sensing. CO is produced by heme oxygenases, of which there are two principle isoforms: inducible (HO-1) and constitutively expressed (HO-2) (369, 542). Importantly, production of CO is O<sub>2</sub> dependent (652) with a P50 of 8.7 kPa (683), placing this potential sensor within the physiological range. CO was found to inhibit the activity of cystathionine- $\gamma$ -lyase, the enzyme responsible for H<sub>2</sub>S synthesis, and hence, H<sub>2</sub>S production is increased when HO-2 becomes substrate limited during hypoxia (683). In archetypical O<sub>2</sub>-sensing cells (e.g., type I cells of the carotid body), it is proposed that H<sub>2</sub>S initiates depolarization through inhibition of Ca<sup>2+</sup>-activated K<sup>+</sup> channels (340) and increasing Ca<sup>2+</sup> influx (56).

Less is known about the role this CO/H<sub>2</sub>S-sensing system functions in nonexcitable, nonspecialized cell types.

## B. Exposure or Adaptation: Does Timing Matter?

With the exception of the HIFs, the above O<sub>2</sub>-sensing mechanisms have been described in the context of whole body physiological reactions to hypoxia, and therefore have an implied negative feedback loop whereby a plethora of actions instigated by the sensing of hypoxia act in conjunction to increase tissue PO<sub>2</sub> to alleviate input stimuli. There is little information on how these mechanisms function in chronically hypoxic environments. The general consensus is that HIF-1 $\alpha$  actions peak after 12–16 h of exposure to low O<sub>2</sub> and then normalize by 24 h to a new set point (62, 178, 249, 630). In contrast, any stabilization of HIF-2 $\alpha$  has been shown to require considerably longer (>72 h) (249, 355). Because these transient responses to reduced O<sub>2</sub> availability are unavoidable during transfer from room air to physiological normoxia, it is critical that experiments aimed at recapitulating physiological conditions enable cells to adapt long term. Importantly, this should include the time required for the expression of any induced protein to also normalize. A global analysis of protein half-life reveals a mean half-life of 46 h (520), and thus, the adaptation time required to circumvent these initial responses to reduced O<sub>2</sub> can be estimated. We have observed that at least 5 days are required for a phenotype to stabilize in human endothelial cells when transferred from room air to a PO<sub>2</sub> of 5 kPa during culture (75, 290), with culture beyond this period inducing no further alterations in cell phenotype (75). To avoid misinterpretation of experimental data, we suggest that cells are cultured for as long as possible (at least 5 days) under physiological normoxic conditions.

## VI. REPLICATING NORMOXIA IN VITRO

Significant efforts have been undertaken to better recapitulate a physiological milieu in vitro, with particular focus on the physical environment in which cells are cultured. For example, numerous studies have characterized the phenotype of endothelial cells exposed to laminar flow (80), or vascular smooth muscle cells (481) and renal mesangial cells (198) exposed to cyclic biaxial stretch, or dermal fibroblasts in three-dimensional (3D) extracellular matrix culture (197). However, few studies have carefully considered the gaseous composition of the culture environment. The following sections provide an overview of current understanding of PO<sub>2</sub> in specific tissues in vivo and summarize the key studies aimed at replicating these conditions in vitro. We focus specifically on investigations in mammalian cells under quasi-physiological PO<sub>2</sub> (not hypoxia) and long-term culture conditions (2–12 kPa, >24 h) to avoid confusing physiological phenotypes with those associated with

relatively rapid adaptive responses to reduced O<sub>2</sub> availability. However, it is worth noting that when reviewing this literature, in most cases, only ambient PO<sub>2</sub> is considered and therefore many observations may not describe the ideal physiologically normoxic phenotype. Furthermore, tissue PO<sub>2</sub> distribution is considerably heterogeneous in both space (regional differences in perfusion or consumption) and time (changes in metabolic activity). The data quoted in this review therefore often represent one observation across a range of potential values and should be interpreted accordingly. All measurements of tissue PO<sub>2</sub> discussed in this review have, to the best of our knowledge, been performed on intact preparations kept in situ to maintain the endogenous blood supply and minimize interference from the atmosphere.

### A. Lungs

In the airways, PO<sub>2</sub> in the gaseous phase can be predicted accurately, and thus, concentrations within the respiratory tract are known with high certainty (see sect. IIIA and **FIGURE 3**). Consistent with the large area occupied by the bronchi, bronchioles, and alveoli, whole-organ PO<sub>2</sub> maps (see **FIGURE 7B**) conducted with MRI scanning using <sup>3</sup>He polarization (3) reveal average PO<sub>2</sub> values of 14.5 (107), 13.4 (649), 13.6 (396), 14 (216), ~12.7 (217), and 13.5 kPa (407) in human subjects, largely reflecting inspired air PO<sub>2</sub>. Whole-lung PO<sub>2</sub> is lower in chronic smokers (216) but does not differ in patients with heart failure, although the alveolar/arterial gradient (see sect. IIIA) is significantly higher in these patients, suggesting a less efficient gaseous transfer (407). These values closely reflect values obtained in experimental animal models, in which mean PO<sub>2</sub> values of 11 (156), 14.7 (682), and 19.6 kPa (107) have been reported in porcine lung, 17.1 kPa in rat lung (85), and 14.7 kPa in rabbit lung (681). Regional heterogeneity in PO<sub>2</sub> measurements throughout the lung was common in all the above studies, consistent with the known variability in lung perfusion and gas exchange. This, coupled with a small image acquisition field of view, can lead to lung PO<sub>2</sub> values skewed by sampling in highly or poorly perfused regions. Encouragingly, lung or alveolar PO<sub>2</sub> values determined by <sup>3</sup>He MRI correlate very well with traditional methods used to determine alveolar PO<sub>2</sub>, in which PO<sub>2</sub> in the expired gas is related to arterial PO<sub>2</sub> and PCO<sub>2</sub> using *Eqns 2/3* (see section IIIA) (217, 407).

The need to transition into the aqueous phase within the airway surface liquid (ASL) for bioavailability make estimates of how a gaseous PO<sub>2</sub> of 13–18 kPa translates into cytosolic PO<sub>2</sub> within airway epithelial cells ambiguous. The average ASL depth in healthy human bronchi is 15–80  $\mu$ m (273) and is therefore unlikely to present a significant barrier to O<sub>2</sub> diffusion. To our knowledge, no measurements of ASL PO<sub>2</sub> in healthy bronchi have been reported, and thus, we are left to interpolate lung epithelial PO<sub>2</sub> based on ASL

depth. Worlitzsch et al. (664) elegantly demonstrated that increased ASL depth (up to 800  $\mu\text{m}$ ) in patients with cystic fibrosis resulted in a mean mucosal  $\text{PO}_2$  of 2.5 mmHg (0.3 kPa). Such hypoxic conditions were associated not only with increased ASL, but also with increased epithelial cell  $\text{O}_2$  consumption and facilitated the early pathogenesis of anaerobic *Pseudomonas aeruginosa* infections (664).

Beyond the epithelia, the lung connective tissue largely consists of fibroblasts whose role it is to maintain the structural integrity of the organ. Intriguingly, adventitial  $\text{PO}_2$  has been reported significantly lower than the average lung  $\text{PO}_2$  (13–14 kPa) as measured by  $^3\text{He}$  inhalation. Using microelectrode penetration, peribronchial  $\text{PO}_2$  values of 5.7 kPa were recorded in patients inspiring  $>50\%$   $\text{FiO}_2$  (326). Similar values have been described in porcine [5.1 kPa (236), 5.8 kPa (205)], canine [ $\sim 6.5$  kPa (282)], and rat [5.1 kPa (487)] experimental models. In the latter study (487), an implantable electron paramagnetic resonance (EPR) resonator was used in conjunction with  $\text{O}_2$ -sensitive EPR probes to monitor deep tissue  $\text{PO}_2$  in real time, confirming measurements using microelectrodes. Anatomically, the site most often sampled by microelectrode penetration lies  $\sim 1$  cm distal to the tracheal bifurcation, near to the peribronchial lymph node. Kamler and colleagues (282) demonstrated that ligation of the aortic stem of the bronchial artery dramatically reduces peribronchial  $\text{PO}_2$  in this region, even when breathing was maintained (FIGURE 7C). This, coupled with the observation that peribronchial  $\text{PO}_2$  does not increase proportionally with  $\text{FiO}_2$  (unlike arterial  $\text{PO}_2$ ) (236), suggests that lung adventitial  $\text{PO}_2$  is critically dependent on blood perfusion from the bronchial artery and does not receive  $\text{O}_2$  supply directly from the airways. How representative this highly sampled region is of nonairway lung tissue as a whole remains to be established, although it has been used as a measure of overall tissue oxygenation following lung transplant and correlates well with improved outcomes (282, 425, 431).

Unlike most other cell types, lung epithelial cells experience a high  $\text{PO}_2$  physiologically and are only separated from gaseous  $\text{O}_2$  by a thin layer of ASL. These conditions have been recapitulated in vitro in the form of air/liquid interface culture, as illustrated in FIGURE 7D. First introduced in the late 1980s by Wu, Kim, and colleagues (6, 7, 645), this technique has been shown to be essential in maintaining primary cultures of tracheal and bronchial epithelial cells in a differentiated state in vitro. Principally, the pseudostratified phenotype observed in vivo can be recapitulated in vitro after  $\sim 7$  days culture at the air/liquid interface (5, 645), with cells typically differentiating into ciliated and granulated mucus-secreting epithelial cells. Other responses to culture at the air/liquid interface include increased  $\text{Na}^+$  transport via short-circuit current (278), restoration of epithelial barrier function (190), and a transcriptional profile more comparative with fresh tracheal/bronchial epithelial

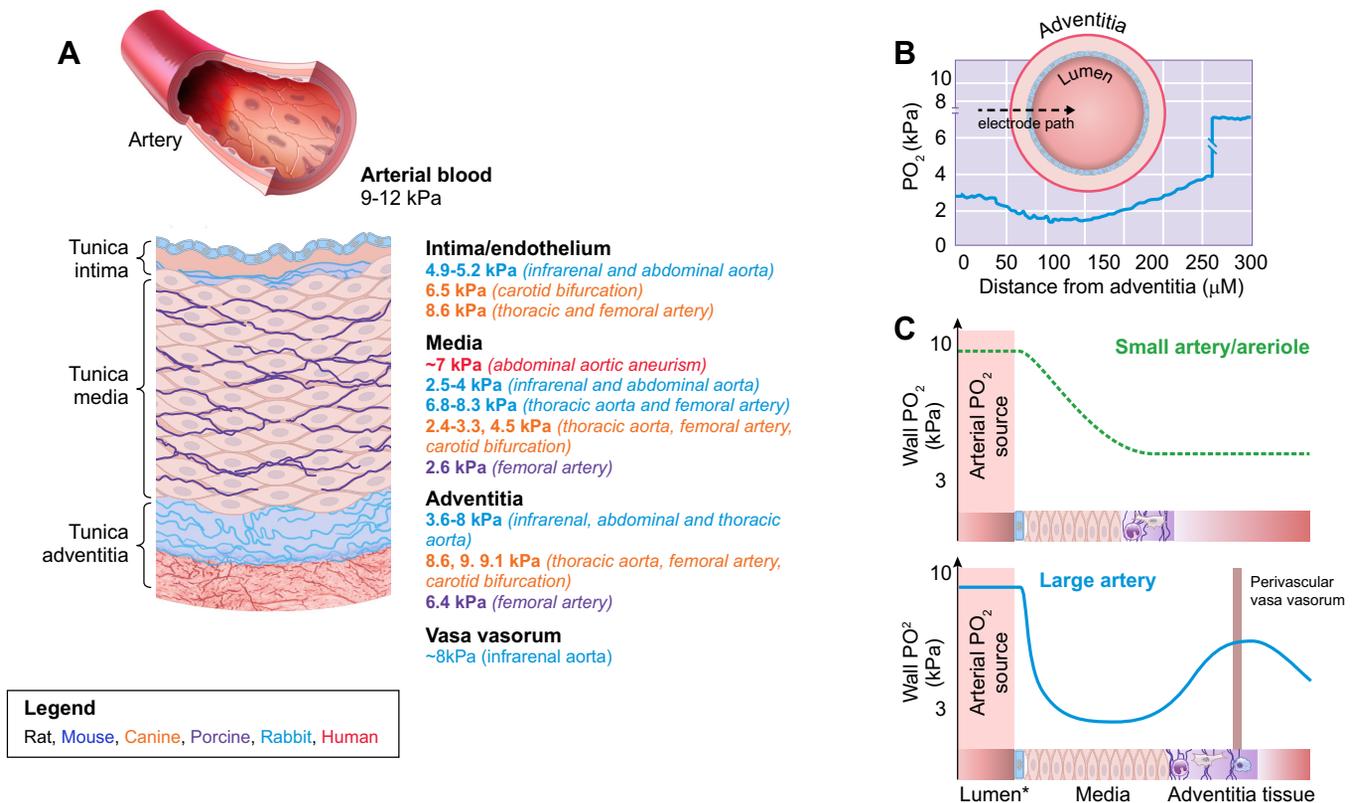
cells in vivo (126, 454), even in response to cigarette smoke inhalation (381). More recently, culture at the air/liquid interface has been used as a tool to differentiate inducible pluripotent stem cells into mature airway epithelial cells (470, 662). This method of culture clearly has profound impact on the phenotype of airway epithelial cells, very accurately recapitulating that observed in vivo. However, we could not identify a publication employing air/liquid interface culture in which the  $\text{PO}_2$  was implicitly defined. When the immortalized epithelial A549 cell line was cultured long term at a  $\text{PO}_2$  of 13 kPa, an increased sensitivity to copper oxide nanoparticles was observed paralleled by a decrease in cellular antioxidant defenses (317). Although pericellular  $\text{PO}_2$  may be lower than 13 kPa in this model, thus poorly representing physiological normoxia, this study provides important insight into the potential of employing culture under physiological normoxia to evaluate environmental toxicity in models of airway damage. Standard incubator conditions ( $\sim 18.5$  kPa, 5 kPa  $\text{CO}_2$ ) reasonably reflect upper tracheal  $\text{PO}_2$ , but bronchiolar  $\text{PO}_2$  can drop as low as 13 kPa. Thus, careful control of ambient  $\text{PO}_2$  during air/liquid interface culture may yield interesting insights into phenotypic differences related to  $\text{PO}_2$  between epithelial cells along the length of the respiratory tract.

## B. The Vasculature

The mechanics of  $\text{O}_2$  distribution in the vasculature have already been covered in section IIIB, and this section aims to further discuss the absolute  $\text{PO}_2$  values measured in the vascular network. In estimating  $\text{PO}_2$  values experienced by different cell types in the vascular wall (endothelial, smooth muscle, and fibroblasts), it is critical to assess the level of  $\text{O}_2$  within the wall tissue itself. An excellent review by Tsai, Johnson, and Intaglietta (594) summarizes the distribution and gradients of  $\text{O}_2$  in the microvasculature, and we have in this review, integrated their summaries and conclusions with recent research findings. Current understanding of the  $\text{PO}_2$  levels in vessels related to specific tissues will be discussed in the context of the relevant tissue.

### 1. The macrovascular wall

Section IIIB2 introduced the concept of radial gradients across the vascular wall, which are particularly prominent in larger arteries such as the aorta and carotid arteries.  $\text{O}_2$  supply to the endothelial layer occurs largely by diffusion from the lumen (containing oxygenated blood  $\text{PO}_2 \sim 12$  kPa), noting that the thickness of the walls of such vessels can severely limit adequate delivery. As such, vessel wall  $\text{PO}_2$  decreases significantly between the luminal and medial layers, as first reported nearly 50 yr ago (410, 428). By advancing a tissue-penetrating Clark-type electrode perpendicular to the vessel wall, as illustrated in FIGURE 8B, a pattern of wall oxygenation in large arterial vessels such as the aorta, femoral, and carotid arteries is clearly evident.



**FIGURE 8.** Oxygen distribution in the arterial wall. **A:** Illustration of known distribution of  $\text{PO}_2$  in the wall of large arteries such as the aorta and carotid and femoral arteries, combining experimentally derived values with theoretical values obtained from established physiology. **B:** Representative trace obtained when a microelectrode is advanced in  $5\text{-}\mu\text{m}$  increments through the wall of the rabbit thoracic aorta. Redrawn with permission from Niinikoski et al. [428]. **C:** Graphical  $\text{PO}_2$  profiles through the walls of small (*top*) and large (*bottom*) arteries, illustrating the effect that the vasa vasorum has on adventitial  $\text{PO}_2$ . \*Endothelium.

Penetrating the intimal layer was associated with a prominent, rapid reduction in  $\text{PO}_2$  in the rabbit infrarenal aorta (237, 330, 428, 509) and abdominal aorta (505, 506, 508), pigeon abdominal aorta (214), and dog carotid artery (507). In such studies,  $\text{PO}_2$  in the intimal layer reached an average of 3–5 kPa, representing a drop of 5–7 kPa from the lumen. Others reported no such sudden drop in similarly sized vessels and preparations (23, 57, 97, 99, 279, 691), instead reporting gradual declines in  $\text{PO}_2$  across the inner third of the wall, reaching a similar nadir within the medial layer. Such discrepancies have been attributed largely to differences in methodology, including 1) the nature of vessel preparation and maintenance, with contrasting  $\text{PO}_2$  profiles observed when the vessel is left in situ (237) versus superfused with physiological solution at a controlled  $\text{PO}_2$  (97) and 2) the method of electrode advancing, with many using vibration-mounting apparatus to minimize tissue distortion. Some (509) have postulated that the resonance created by such devices can interfere with the laminar flow patterns close to the vessel wall, considered critical in forming the aforementioned  $\text{O}_2$  diffusion barrier. In contrast, others (98) have suggested that the sharp decline in  $\text{PO}_2$  at the intimal layer is an artifact resulting from the use of large-diameter electrodes. Whether sharp or gradual, experimental evidence is clear that vessel wall  $\text{PO}_2$  declines propor-

tional to distance from the lumen (in vessels devoid of vasa vasorum, see below).

Aside from this discrepancy, remarkable conformity exists in the reported minimal vessel wall  $\text{PO}_2$ . The nadir within the medial layer shown in **FIGURE 8B-C** occurs at 50%–70% of the wall thickness away from the adventitia ( $\sim 200\ \mu\text{m}$  in a rabbit thoracic aorta) and reaches a  $\text{PO}_2$  of 3–4 kPa (23, 237, 279, 330, 428, 505–509). This value has been shown to correlate negatively with total wall thickness (97, 279), and hence, conditions in which vessel wall hyperplasia occurs can result in significant reductions in medial  $\text{PO}_2$ , as observed in alloxan-induced diabetes (505), atherosclerosis (279), hypertension (99, 506), after insertion of vascular grafts (330, 509) or stents (508), and after balloon de-endothelialization (691). Reduced medial  $\text{PO}_2$  in such conditions has been attributed to an altered bioenergetic profile in resident (and migrating) cells (330) as well as biophysical considerations such as increased wall stress (508) and compression of the vasa vasorum (57, 508). Medial hypoxia has been demonstrated in vivo in rabbits with late-stage atherosclerotic plaques in the aortic arch and thoracic aorta using the biochemical hypoxia marker 7-(4'-(2-nitroimidazol-1-yl)-butyl)-theophylline (41). In this study, plaques  $>400\ \mu\text{m}$  in diameter exhibited hypoxic regions

~200  $\mu\text{m}$  in diameter and 200–300  $\mu\text{m}$  from the endothelial/intimal surface, with an estimated  $\text{PO}_2$  of 0.5 kPa. Using similar probes ( $^{18}\text{F}$ ]EF5 and  $^{64}\text{Cu}$ ]ATSM), hypoxic regions have been visualized within the media of atherosusceptible transgenic mice (427, 537) and rabbits (426). Atherosclerotic plaques occur preferentially in regions of the vasculature that experience oscillatory blood flow, such as the inner curvature of the aortic arch and carotid bifurcation (370), and lower medial  $\text{PO}_2$  has been measured in such regions using microelectrodes (507). It is therefore possible that medial hypoxia precedes and facilitates atherogenesis in such regions rather than occurring subsequent to plaque development and wall thickening.

Limited data are available on  $\text{PO}_2$  profiles in large arteries in humans, as measurements are invasive and difficult to perform in humans. However, Vorp and colleagues (620, 621) performed microelectrode measurements of  $\text{PO}_2$  within the abdominal aortic wall of patients with aneurysms. Although reported measurements were normalized to luminal  $\text{PO}_2$ , interpolation based on an average aortic luminal  $\text{PO}_2$  of ~11 kPa suggests that the aortic aneurysm wall  $\text{PO}_2$  was ~7 kPa in the absence of intraluminal thrombi, falling to ~2.5 kPa when a thick thrombus was evident (620). Although the exact topographical location of the  $\text{PO}_2$  sampling point was not reported, an aortic wall  $\text{PO}_2$  of ~7 kPa is similar to values measured in animal models (279, 505, 506, 508).

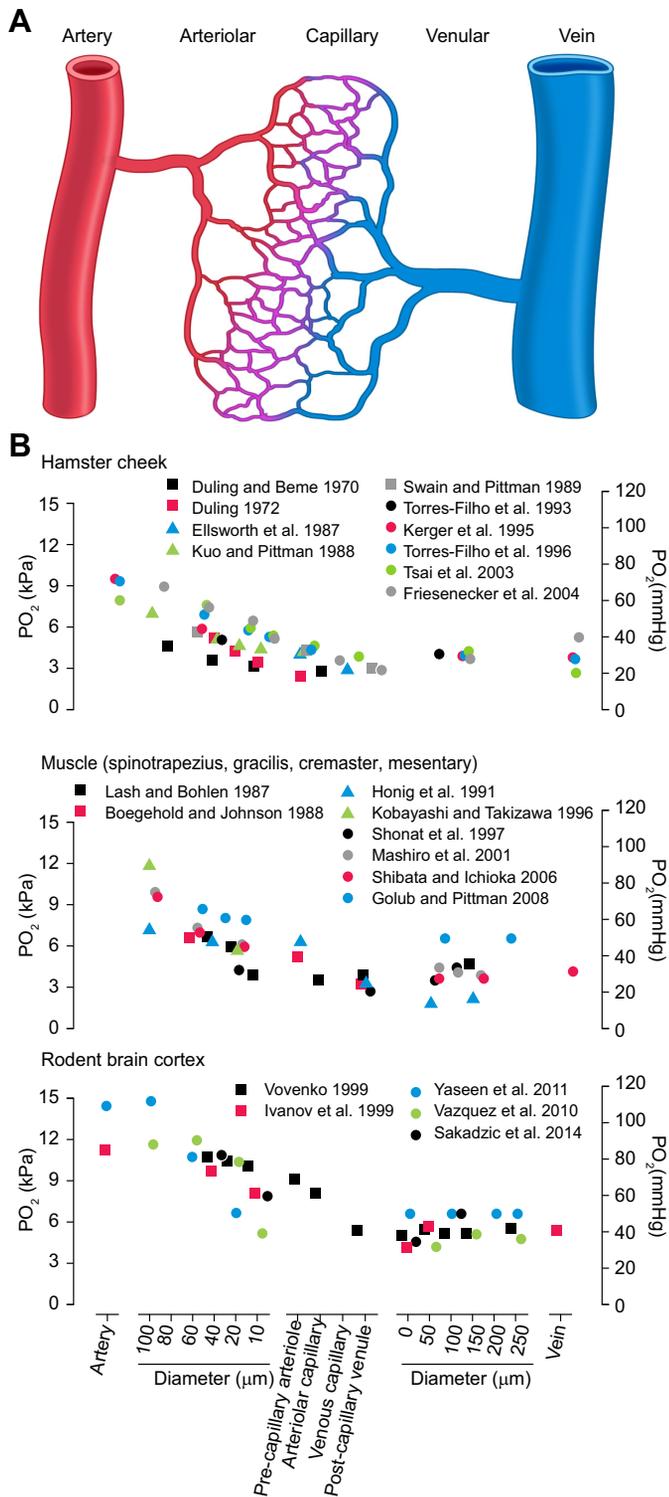
The walls of large blood vessels can be thick enough in diameter to merit their own blood supply, and in arteries, these vessels are termed the vasa vasorum. The extent and nature of such vessels is critically dependent on the wall thickness. Peri-adventitial vasa can exist in moderately sized arteries such as the femoral or carotid, whereas vasa penetrating into the media are thought only to occur beyond a critical threshold diameter (>500  $\mu\text{m}$  or 29 lamellar units, irrespective of species or vessel characteristics) (661). In the context of vessel wall  $\text{PO}_2$  distribution, the presence of vasa vasorum is critical in defining adventitial  $\text{PO}_2$ , as outlined in **FIGURE 8C**. An upward inflection beyond the medial nadir in the  $\text{PO}_2$  profile of a vessel wall is characteristic of a second source of  $\text{O}_2$  diffusion from the outer layers. Arteries confirmed histologically to be devoid of adventitial vasa demonstrate a continuous decline in  $\text{PO}_2$  between the lumen and adventitia (97, 99, 279), and experimental disruption of vasa vasorum patency (surgical or resulting from increased wall stress secondary to increased blood pressure) in those vessels possessing peri-adventitial vasa results in a significant reduction in adventitial  $\text{PO}_2$  (23, 57, 330, 508, 509, 691). Moreover, increases in aortic tissue  $\text{PO}_2$  in response to vasodilatory compounds (adenosine and epinephrine) applied to the adventitia have been attributed to vasa vasorum vasodilation (58). Notably, adventitial and medial neovascularization often occurs in response to vessel injury (413), and Lee et al. (330) showed that

decreased adventitial  $\text{PO}_2$  following insertion of an anastomotic graft can resolve over time in conjunction with the histological appearance of new medial vasa.

## 2. The microvasculature

The vascular network between an artery and vein, encompassing arterioles, capillaries, and venules is the prime region for  $\text{O}_2$  exchange, as evidenced by the significant difference in blood  $\text{PO}_2$  between an artery and vein (~6–7 kPa). This longitudinal gradient was first highlighted in section III B1 and is the focus of previous reviews (456, 594). As such, only an overview of blood  $\text{PO}_2$  within the microvascular network will be included in this review. Microvascular networks are present in all organs, and we provide an overview of blood  $\text{PO}_2$  in an idealized microvascular network comprised of 1) a feeding artery, 2) first-, second-, and third-order arterioles, 3) a capillary bed, 4) first-, second-, and third-order venules, and 5) a collecting vein (**FIGURE 9A**). The majority of studies of microvascular  $\text{PO}_2$  distribution have focused on three experimental preparations: the hamster skinfold/cheek window, rat cremaster/spinotrapezius muscle, and rat pial/cortical microvasculature. Their minimally invasive nature and the ability to monitor intravascular  $\text{PO}_2$  in live animals are major advantages of such models. A summary of studies for each experimental model is provided in **FIGURE 9B**. Blood enters the microvascular network at an average  $\text{PO}_2$  of ~9 kPa and rapidly declines along the arterioles to reach a capillary  $\text{PO}_2$  ~5 kPa. As described by Tsai et al. (594), such a finding suggests that arterioles, and not capillaries, are the major source of  $\text{O}_2$  delivery in most microvascular beds. This may be true for hamster cheek pouch and rat muscle preparations, but reports in rat pial microvessels indicate that intravascular  $\text{PO}_2$  in precapillary arterioles is still ~7–9 kPa, and only falls substantially once it has entered the capillary networks (622). However, recent evidence using two-photon time resolved phosphorescence (500) has refuted such claims, demonstrating that arterioles in the mouse cerebral cortex are responsible for ~50% of  $\text{O}_2$  delivered to the underlying parenchyma. These authors postulated that the expansive capillary network may act as a reserve mechanism for  $\text{O}_2$  delivery during times of increased activity (500).

Unlike large vessels, the presence of radial gradients and their contribution to tissue  $\text{PO}_2$  in arterioles is less well defined. Many studies report differences between intravascular and periarteriolar  $\text{PO}_2$  (260, 531, 585, 591), which appear proportional to the blood  $\text{PO}_2$  and luminal diameter (594). Such differences are in the order of 2.5–3.5 kPa in large (A1) arterioles (531, 591) and ~1.5 kPa in moderately sized (~40- $\mu\text{m}$  diameter) arterioles (260, 531, 585). In contrast, others have observed an arteriolar wall  $\text{O}_2$  gradient of only a few of millimeters mercury [1.4 mmHg/0.2 kPa per micrometer (122, 123); 1.2 mmHg/0.16 kPa per micrometer (527, 623)]. Pittman (456) proposed a possible explanation for this discrepancy, citing misinterpretation of phos-



**FIGURE 9.** Oxygen distribution in the microvasculature. *A*: An idealized microvascular network. *B*: Reported  $PO_2$  values plotted against the vessel diameter in microvascular experimental preparations. Results are separated according to tissue and coded according to the measurement technique employed:  $\square$ , microelectrode penetration;  $\triangle$ , derived from measurements of hemoglobin saturation, in which  $PO_2$  was interpolated based on known species hemoglobin (Hb) dissociation curves; and  $\circ$ , phosphorescence-quenching microscopy. Adapted from Tsai et al. (594).

phorescence quenching data due to  $O_2$  consumption by the probe itself. Attempts to remedy these differences have subsequently been made by adapting the methodology (182, 183, 185). Unusually high vascular wall consumption, the reasoning put forward to explain large radial arteriolar gradients (594), was also refuted by Vadapalli et al. (603). With relevance to estimating physiological normoxia for cells resident within the microvascular wall, we believe that intravascular (blood)  $PO_2$  most appropriately represents this value.

### 3. The human umbilical vein

One of the most well-studied and widely utilized vascular cell type in vitro are HUVEC. However, its unique physiology (fetal, venous tissue carrying oxygenated blood at a low flow rate) means it does not reflect normal artery/vein, macro/microvascular characteristics. Unlike many other tissues in the human body, the umbilical cord can be accessed relatively easily/noninvasively for blood collection and gas analysis, albeit ex vivo. It is therefore fortunate that endothelial cells isolated from these vessels have been used extensively in vascular biology in vitro, allowing for an accurate and well-characterized transition to physiologically normoxic cell culture. A meta-analysis of data extracted from a number of studies reporting umbilical blood  $PO_2$  (102, 109, 298, 313, 347, 376, 465, 486, 576, 605, 675) reveals a mean blood  $PO_2$  of 3.8 and 2.4 kPa within umbilical veins and arteries, respectively. Although collected ex vivo under room air, this has been shown not to increase measured  $O_2$  levels in umbilical blood (382). Interestingly, umbilical vein  $PO_2$  decreases throughout gestation from  $\sim 6$  kPa at 20 wk to  $\sim 4$  kPa at 36 wk (639), and final  $PO_2$  at birth is significantly affected by the method of delivery (spontaneous vaginal versus caesarean) (109, 313) and position of the fetus (breech) (102). The human umbilical vein is a macrovessel of 2–3-mm diameter with an average wall thickness of 430  $\mu m$  and a moderate adventitial layer (344). Although not studied, based on these dimensions, it seems likely that a significant radial gradient would be apparent across the length of the wall (section IIIB2), and thus, physiological normoxia in smooth muscle cells in these vessels may be lower than that measured in the endothelium [ $\sim 3.5$  kPa (75)].

### 4. Endothelial cells

The physiological response to hypoxic tissue  $O_2$  levels is an initial vasodilation followed by the induction of angiogenesis, with both responses increasing  $O_2$  delivery and thereby alleviating the harmful effects of hypoxia (536, 571). Given the primary role of endothelial cells in orchestrating such responses, it is no surprise this cell type has received considerable attention in the context of low  $O_2$  physiology (393, 472, 523), as summarized in **TABLE 4**. We recently described a well-defined model to recapitulate physiological

**Table 4.** *The effects of culture at physiological normoxia on endothelial cell physiology*

Species	Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time (days)	Summary*	Reference
Human	HUVEC	5 (12 shear)	3	<p>↑ Growth (BrdU)</p> <p>↑ Expression of membrane and ECM proteins CD105, CD31, fibronectin, laminin, and type VI collagen.</p> <p>Different morphology after 24 h shear stress (20 dyne/cm<sup>2</sup>) (more spindle-like, elongated).</p> <p>↑ NO and PGI<sub>2</sub> production with shear stress, ↔ with 20% versus 12% O<sub>2</sub></p>	(695)
	EPC	5, 1	3	Dissolved medium O <sub>2</sub> level much lower in ESC, iPSC, and EPC cultures than HUVEC.	(2)
	HUVEC			↑ Traditional hypoxia-sensitive genes (VEGF, Glut1, and EPO).	
	HUVEC	3	up to 25	↑ FGF and VEGF stimulated growth and migration.	(276, 277)
	HUAEC			Putting nonadapted cells in 3% O <sub>2</sub> for 1 day ↑ effects of FGF and VEGF and putting adapted cells in 21% O <sub>2</sub> did not reverse the effect of adaptation of growth. ↓ Cell surface area compared with nonadapted once adhered.	
	HUVEC	5 (5 shear)	3	<p>Microarray analysis showed 41–74 upregulated and 21–86 downregulated genes (all HIF regulated), (HUVEC/HUAEC).</p> <p>↔ Protein/mRNA expression following shear between 5% and 20% O<sub>2</sub>.</p> <p>↓ Apoptosis gene expression (Bcl), no additive effect of 5-FU.</p> <p>↑ Permeability with 5-FU, reversed by resveratrol.</p>	(1)
	HUVEC	5	1, >5	<p>Culture at 5 kPa ambient P<sub>O<sub>2</sub></sub> results in intracellular P<sub>O<sub>2</sub></sub> of ~3.5 kPa in HUVEC monolayers.</p> <p>↓ Induction of antioxidant defense proteins (HO-1 and NQO1) by electrophilic agents.</p> <p>↔ Induction of glutathione-related proteins (GCLC, GCLM, and xCT) but no change in [GSH]<sub>i</sub>.</p> <p>↑ Bach1 protein and siRNA-mediated knockdown rescued HO-1 induction at 5 kPa O<sub>2</sub>.</p> <p>↓ Proliferation</p>	(75)
	HUVEC	5, 1	>5	<p>IC<sub>50</sub> for HIF-1α stabilization is 2.3 kPa O<sub>2</sub> when plotted against intracellular P<sub>O<sub>2</sub></sub>.</p> <p>↑ PP2A-C protein and colocalization with eNOS-mediated rapid dephosphorylation in response to Ca<sup>2+</sup>-dependent stimuli, but not laminar shear stress.</p> <p>PP2A-C protein levels show bell-shaped relationship with ambient P<sub>O<sub>2</sub></sub>, peaking at 5 kPa.</p> <p>NO bioavailability inversely proportional to P<sub>O<sub>2</sub></sub>.</p> <p>Culture at physiological normoxia-induced phenotype distinct from that under hyperoxic (room air) and hypoxic (1 kPa O<sub>2</sub>) conditions.</p>	(290)

*Continued*

Table 4.—Continued

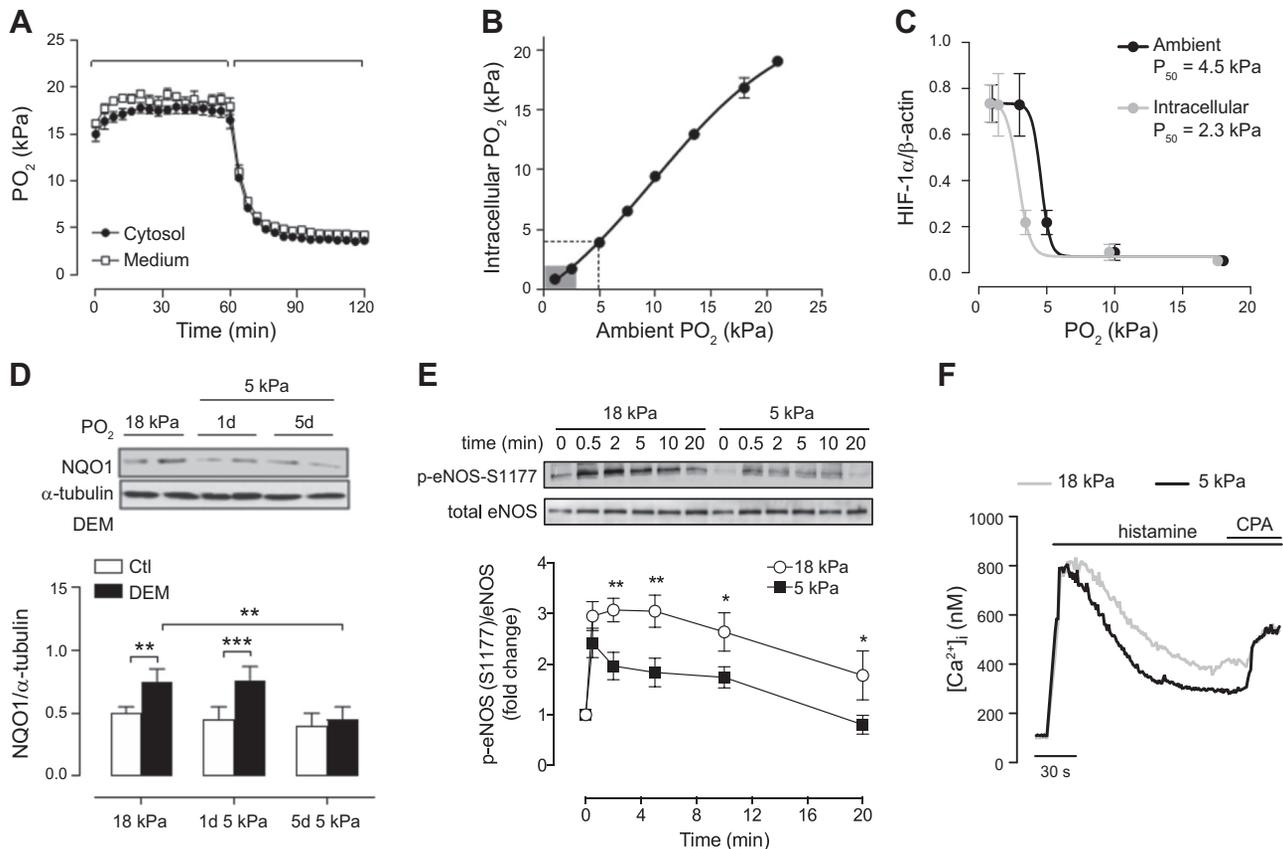
Species	Cell Type	Po <sub>2</sub> (kPa)	Time (days)	Summary*	Reference
	HUVEC	5	>5	↓ Plateau phase [Ca <sup>2+</sup> ] <sub>i</sub> in cells at 5 kPa O <sub>2</sub> , rescued by cotreatment with SERCA-inhibitor CPA. Cells at 5 kPa O <sub>2</sub> more resistant to Ca <sup>2+</sup> overload due to mitochondrial sparing by increased SERCA activity.	(291)
	HPMVEC	5	12	Confluent monolayers contained 30% fewer cells, but formed a tighter barrier as measured by TER.	(547)
	ST1.6R			↑ Cortical actin levels.	
	HDMVEC	5	14	↑ Basal and stimulated growth (PMA and IL-1β). ↑ ECM proteins (type VI collagen).	(697)
Bovine	Corneal EC	6	4	↑ [ <sup>3</sup> H]thymidine incorporation and cell count.	(684)
	BRMVEC	95, 40, 20, 105	4	Endothelial cells more sensitive to effects of oxygen compared with pericytes and fibroblasts from same vessel.	(490)
Rat	Liver sinusoidal EC	5	5	↓ Basal apoptosis (MTT and Annexin V/PI). ↔ Morphology of confluent monolayer or fenestrated characteristics. ↓ Endocytotic capacity during culture significantly less at 5%. ↓ ICAM-1 and IL-6 expression/production (proinflammatory) and ↑ IL-10 production (anti-inflammatory) [only measured after 48 h]. ↑ H <sub>2</sub> O <sub>2</sub> basal production (DCF), treatment with catalase reverses effects on apoptosis. ↔ NO release (Griess reaction).	(377)

BRMVEC, bovine retinal microvascular endothelial cells; CPA, cyclopiazonic acid; DCF, dichlorofluorescein; ECM, extracellular matrix; EPC, endothelial progenitor cell; EPO, erythropoietin; ESC, embryonic stem cell; FGF, fibroblast growth factor; 5-FU, 5-fluorouracil; GCLC, glutamate-cysteine ligase catalytic; GCLCM, glutamate-cysteine ligase catalytic modulatory subunit; Glut1, glucose transporter 1; GSH, glutathione; HDMVEC, human dermal microvascular endothelial cell; HO-1, heme-oxygenase 1; HPMVEC, human pulmonary microvascular endothelial cell; HUAEC, human umbilical artery endothelial cell; HUVEC, human umbilical vein endothelial cell; ICAM-1, intracellular adhesion molecule 1; IL-1β, interleukin-1β; iPSC, inducible pluripotent stem cell; MTT, 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide; NO, nitric oxide; PGI<sub>2</sub>, prostacyclin; PI, propidium; iodide PMA, phorbol 12-myristate 13-acetate; PP2A-C, protein phosphatase 2A catalytic subunit; SERCA, sarco/endoplasmic reticulum Ca<sup>2+</sup>-ATPase; TER, transendothelial resistance; VEGF, vascular endothelial growth factor; xCT, cystine-glutamate antiporter system X; EC, endothelial cells, eNOS, endothelial nitric oxide synthase.

normoxia in cultured human venous and arterial endothelial cells (75, 290, 291). Using a phosphorescent nanoparticle probe to monitor intracellular Po<sub>2</sub> in living cells (**FIGURE 10A**), we established that culture at a Po<sub>2</sub> of 5 kPa was required to compensate for monolayer O<sub>2</sub> consumption and recapitulate a physiologically normoxic intracellular environment of 3.5–4 kPa (measured in umbilical venous blood, see above). To maintain such conditions in different culture apparatus (6-, 24-, or 96-well plates) with various surface area, volume was adjusted to achieve similar surface area: medium-depth ratios. For example, 100 μl in a 96-well plate has roughly the same surface area: medium-depth as 500 μl in a 24-well plate.

The importance of distinguishing between ambient and intracellular Po<sub>2</sub> was further highlighted by the different absolute P<sub>50</sub> (akin to EC<sub>50</sub>/IC<sub>50</sub>) (633) values for HIF-1α sta-

bilization when plotted against each O<sub>2</sub> parameter (**FIGURE 10C**) (290). When ambient Po<sub>2</sub> is used, the resulting P<sub>50</sub> value (4.3 kPa) is not consistent with the known Po<sub>2</sub> distribution in the majority of the microvasculature nor in tissues, where a Po<sub>2</sub> 4–5 kPa would be considered normoxic, and hence, minimal HIF-1α stabilization should be apparent. In contrast, use of intracellular O<sub>2</sub> levels results in a P<sub>50</sub> value of 2.3 kPa, a level more consistent with what one may expect to observe in the hypoxic vasculature in vivo. Under these defined conditions, we have shown that the induction of nuclear factor E2-regulated factor 2-regulated antioxidant gene expression in response to oxidative stress was markedly attenuated in HUVEC (**FIGURE 10D**). Similar findings have been reported in RAW 264.7 macrophages cultured at 5 kPa (208), and in human diploid fibroblasts upon re-exposure to atmospheric Po<sub>2</sub> following long-term culture at 3 kPa (21). Notably, this phenotype was only



**FIGURE 10.** Effects of physiological normoxia on human endothelial cells. Experimental data describing the careful definition of cellular oxygenation *in vitro* and the subsequent characterization of cellular function and phenotype during long-term culture under these conditions. **A:** Intracellular  $\text{PO}_2$  in human umbilical vein endothelial cell (HUVEC) monolayers cultured in 96-well plates (100- $\mu\text{l}$  volume) at a  $\text{PO}_2$  of 18 kPa and then exposed acutely to 5 kPa, measured using MitoXpress Intra in an  $\text{O}_2$ -regulated plate reader. This illustrates that the  $\text{PO}_2$  in the medium is only moderately higher than cytosolic, and both parameters rapidly change upon changes in ambient  $\text{PO}_2$ . **B:** Intracellular  $\text{PO}_2$  in HUVEC monolayers as a function of the ambient  $\text{PO}_2$ , defined by a four-parameter sigmoidal fit. Dashed lines indicate the conditions in which HUVEC were subsequently cultured. **C:** HIF-1 $\alpha$  protein levels in HUVEC were cultured for 5 days at the indicated  $\text{PO}_2$  in an  $\text{O}_2$ -regulated workstation and corrected for the resulting intracellular  $\text{PO}_2$  determined in **B**. Plotting against intracellular  $\text{PO}_2$  results in  $P_{50}$  values more likely to be observed in the vasculature *in vivo*. **D:** Expression of a Nrf2 regulated antioxidant defense protein, NAD(P)H-quinone oxidoreductase 1 (NQO1), in HUVEC cultured at a  $\text{PO}_2$  of 18 or 5 kPa for 1–5 days and then challenged with the electrophile diethyl maleate (DEM; 100  $\mu\text{M}$  for 24 h). These data illustrate the difference between cellular phenotypes when cells are exposed acutely (24 h) or chronically (5 days) to lower  $\text{O}_2$ . **E:** Phosphorylation of endothelial nitric oxide synthase (eNOS) in response to histamine (10  $\mu\text{M}$ , 2 min) stimulation in HUVEC cultured at a  $\text{PO}_2$  of 18 or 5 kPa for 5 days, demonstrating a more rapid decline in phosphorylation over time in cells cultured under physiological normoxia. **F:** Intracellular  $\text{Ca}^{2+}$  mobilization in response to histamine, measured using Fura-2AM. Lower plateau  $[\text{Ca}^{2+}]_i$  at physiological normoxia are reversed by treatment with the sarco/endoplasmic reticulum  $\text{Ca}^{2+}$ -ATPase inhibitor cyclopiazonic acid (CPA). **A**, **B**, and **D** are replotted from Chapple et al. (75); **C** and **E** are taken from Keeley et al. (290); and **F** is taken from Keeley et al. (291).

observed following long-term adaptation (>5 days) to physiological normoxia (75). GSH-based defense systems remained intact, and this alone conferred sufficient protection to maintain cell viability (69). In line with this, basal levels of apoptosis are lower in HUVEC (1) and rat liver sinusoidal endothelial cells (377) cultured at 5 kPa for 3 and 5 days, respectively. We have recently shown that HUVEC cultured at a  $\text{PO}_2$  of 5 kPa exhibited significantly less sensitivity to  $\text{Ca}^{2+}$  overload-induced cell death (291), which we attributed this enhanced sarco/endoplasmic reticulum

$\text{Ca}^{2+}$ -ATPase activity, sparing the mitochondria from  $\text{Ca}^{2+}$  overload (FIGURE 10F).

There are conflicting reports on the effects of physiological  $\text{O}_2$  levels on endothelial cell proliferation *in vitro*. In the context of angiogenesis, the consensus is that a higher proliferative rates occur in endothelial cells cultured under physiological  $\text{O}_2$  levels, and indeed, this has been demonstrated in HUVEC (2, 276, 277, 695) and human dermal microvascular endothelial cells (697). However, we ob-

served a significant reduction in HUVEC proliferation following culture at 5 kPa for more than 5 days (75), in line with the quiescent nature of endothelial cells *in vivo* (133, 244). Moreover, production of extracellular matrix proteins type IV collagen (49, 697), fibronectin, CD105, CD31, and laminin (695) is significantly higher in human dermal microvascular endothelial cells and HUVEC cultured at 5 kPa levels. Differentiating between endothelial cell responses to physiological and hypoxic O<sub>2</sub> levels is especially relevant given their unique and highly regulated response to pathological hypoxia. For example, different HUVEC phenotypes are observed when cultured at a P<sub>O<sub>2</sub></sub> of 3 (277) and 5 kPa (2, 75), largely due to increased stabilization of HIF-1 $\alpha$  under the lower O<sub>2</sub> level. We have recently demonstrated that the synthesis of nitric oxide (NO) is significantly altered when endothelial cells are cultured at 5 kPa (FIGURE 10E) (290). Importantly, these processes were still functional, yet under more strict regulatory control by protein phosphatase 2A. This is in stark contrast to the phenotype observed in hypoxic (1 kPa) cells, in which stimulation of NO synthesis is largely abolished. In many respects, cells cultured at hypoxic O<sub>2</sub> levels more closely resemble those maintained at room air than those cultured at physiological O<sub>2</sub> levels, further highlighting the importance of this distinction.

### 5. Circulating and immune cells

As for endothelial and smooth muscle cells, no single O<sub>2</sub> level can be described as normoxic for circulating cells. This does not preclude the study of circulating cells under physiologically relevant O<sub>2</sub> levels *in vitro*, because even the highest O<sub>2</sub> levels encountered *in vivo* (~13 kPa within the pulmonary circulation) are still much lower than atmospheric. Although circulating cells are exposed to the full dynamic range of blood physiological O<sub>2</sub> (~5–13 kPa) over a relatively short period of time, the majority of blood at any given time resides in the venous and microvascular compartments (~60%–75%) (24, 47), in which P<sub>O<sub>2</sub></sub> averages 5 kPa (594). Moreover, most monocytes reside within the spleen at rest (564), where P<sub>O<sub>2</sub></sub> ranges from 2 to 5 kPa in rodents (48, 61, 67, 266) and swine (573), and 7–8 kPa in rabbits (613, 614). Such variance likely reflects the heterogeneous perfusion of the spleen, with pronounced gradients extending away from the splenic artery in mice (61).

Several studies have investigated the effects of isolation and culture of human PBMC under physiological O<sub>2</sub> (as summarized in TABLE 5). Basal proliferation of human CD4<sup>+</sup>/CD8<sup>+</sup> PBMC (16, 17, 315) and murine CD4<sup>+</sup> T cells (259) was largely unchanged during culture at a P<sub>O<sub>2</sub></sub> of 5 kPa, whereas proliferation stimulated by concanavalin A or CD3/CD28 cross-linking was markedly lower (16, 17). Interestingly, growth stimulated by another lectin, phytohemagglutinin, was unaffected by culture at 5 kPa (16, 17, 315). Another common observation during culture at 5 kPa is enhanced T cell differentiation and activation, with in-

creased early expression of the activated lymphocyte marker CD69 on PBMC (17, 210, 315), activation of PBMC-matured human dendritic cells (171), and murine splenocyte-differentiated T cell CD4:CD8 maturation (61). Indeed, a transcriptional array of human PBMC samples cultured at 5 kPa for 15 days revealed significant upregulation of genes important for lymphocyte biology, whereas expansion at room air highlighted upregulation of gene clusters associated with stress responses, cell death, and repair mechanisms (210). Expansion of human PBMC under atmospheric conditions reduces intracellular GSH levels because of oxidative stress associated with prolonged hyperoxia. This artifact can be reduced by expansion of PBMC expanded at a P<sub>O<sub>2</sub></sub> of 5 kPa (146). Associated with atmospheric culture-induced GSH depletion is the induction of antioxidant and defense proteins such as superoxide dismutase (SOD), catalase, and GSH peroxidase-1 (146), resulting in lower basal cytosolic ROS (146, 315). One potentially significant consequence of the altered human PBMC phenotype at a P<sub>O<sub>2</sub></sub> of 5 kPa was reported by Sahaf and colleagues (499). The HIV transactivator of transcription protein, previously understood to induce apoptosis in *ex vivo* T cell preparations, caused rapid proliferation and primed cells for subsequent infection more rapidly than phytohemagglutinin (499). This novel finding highlights the possibility of drawing misinformed conclusions based on *in vitro* experiments performed under hyperoxic conditions. In summary, culture of PBMC and similar cells under physiological P<sub>O<sub>2</sub></sub> conditions has significant consequences on cell proliferation, redox status, and differentiation capacity. It remains to be investigated whether changes in P<sub>O<sub>2</sub></sub> within the physiological range (2–5 kPa) (e.g., as would occur when monocytes enter the systemic circulation from the spleen), have functional consequences on their physiology.

Human peripheral blood neutrophils undergo rapid (within 24 h) and constitutive apoptosis after isolation and culture under standard culture conditions (P<sub>O<sub>2</sub></sub> 18–20 kPa). This can be reduced significantly by isolation in a low P<sub>O<sub>2</sub></sub> (0–3 kPa) environment (218) and with inhibitors of HIF-1 $\alpha$  hydroxylation (628). Moreover, hyperoxia-induced apoptosis was also reduced in peripheral neutrophils isolated from patients with von Hippel-Lindau syndrome (627), although this was further reduced by hypoxic incubation, suggesting a role for both HIF-1 $\alpha$ -dependent and independent pathways. Despite enhanced survival, neutrophils maintained at a P<sub>O<sub>2</sub></sub> of 3 kPa exhibited defective respiratory burst activity and hence killing ability against *Staphylococcus aureus* infection, seemingly through the limitation of molecular O<sub>2</sub> as a substrate for the generation of ROS (383). This may result from suboptimal O<sub>2</sub> diffusion/supply capacity *in vitro*, as elegantly demonstrated recently (63), rather than true substrate limitation. The effects of low P<sub>O<sub>2</sub></sub> culture on neutrophils has been summarized elsewhere (354, 574) and so will not be discussed in further detail in this review. Although a P<sub>O<sub>2</sub></sub> of 3 kPa may be considered

**Table 5.** *The effects of culture at physiological normoxia on circulating cell physiology*

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time (days)	Summary	Reference
Human	PBMC	5	1–5	<p>↑ Unstimulated and Con A–stimulated proliferation; no effect on PHA stimulation.</p> <p>↑ Early expression of lymphocyte marker CD69.</p> <p>↓ Basal and H<sub>2</sub>O<sub>2</sub>-induced ROS production (DCF).</p> <p>Altered released cytokine profile following stimulation with Con A or LPS.</p>	(315)
	PBMC	5	15	<p>Gene expression array revealed higher expression of genes important for lymphocyte biology, immune function and cell-cycle progression.</p> <p>↓ Expression of genes involved in stress response, cell death, and cellular repair.</p>	(210)
	PBMC	5	5	<p>Proliferation stimulated by antigen CD8/CD28 cross-linking, or Con A, was ↑ at 5%, but no effect on phytohemagglutinin-stimulated proliferation.</p> <p>Unstimulated cell viability unaffected by adaptation to 5%.</p>	(16)
	Negatively enriched T cells	5	3	<p>↓ GSH and GSH:GSSG following culture (versus fresh), less reduction at 5%.</p>	(17)
	PBMC			<p>↓ Proliferation</p> <p>↑ CD8/CD28-stimulated NO and ROS production.</p> <p>↑ Lymphocyte marker CD69.</p>	
	PBMC	5	>6	<p>Tat protein induces apoptosis at 20%, but proliferation at 5% O<sub>2</sub>.</p> <p>Tat can be used to prime cells for HIV infection as well as other methods, only at 5% O<sub>2</sub>.</p>	(499)
	PBMC	5	7	<p>In vitro culture ↑ SOD1–3, CAT, and GPx mRNA. At 5% O<sub>2</sub>, ↓ CAT and GPx mRNA versus room air.</p> <p>↑ GPx activity, no change in CAT or SOD activity.</p> <p>↑ Intracellular GSH, although overall decrease during culture.</p> <p>↓ Superoxide and hydrogen peroxide.</p>	(146)
	PBMC-matured dendritic cells	5	duration of culture	<p>↔ Total cell yield.</p> <p>↓ Endocytosis of dextran/FITC.</p> <p>↑ LPS-induced IL-12 (p70) and T cell activation during coculture.</p>	(171)
Mouse	CD4 <sup>+</sup> T cells	5, 1	36 h	<p>↑ Th17-specific differentiation at 5%; ↓ all subset differentiation at 1%.</p> <p>No effect of 5% on proliferation, 1%.</p> <p>↓</p> <p>Increased mTORC1 activity at 5% O<sub>2</sub>.</p>	(259)
	Primary splenocytes	2.5	6	<p>↑ CD4:CD8, but dramatically higher killing (lytic) potential of CD8<sup>+</sup> cells at 5%, with ↑ density of CD25 surface antigen.</p>	(61)
	Splenocyte-differentiated T cells			<p>↓ Cell death</p>	

Continued

Table 5.—Continued

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time (days)	Summary	Reference
	macrophage line J774	6	24 h	↓ <i>Leishmania amazonensis</i> (intracellular parasite) infection at 5%. ↔ NO or ROS production.	(105)

CAT, catalase; Con A, concanavalin A; DCF, dichlorofluorescein; LPS, lipopolysaccharide; FITC, fluorescein isothiocyanate; GPx, glutathione peroxidase; GSH, glutathione (reduced); GSSG, glutathione (oxidised); HIV, human immunodeficiency virus; IL-12, interleukin-12; mTORC, mammalian target of rapamycin; NO, nitric oxide; PBMC, peripheral blood mononuclear cell; PHA, phytohaemagglutinin; ROS, reactive oxygen species; SOD, superoxide dismutase; Tat, HIV transactivator of transcription.

subphysiological in the general context of this article, one must consider that inflammation can produce localized areas of profound tissue hypoxia (63, 189, 331, 367, 538, 588), and therefore it may be more appropriate to study neutrophil physiology under such conditions, especially if these cells cannot survive at higher P<sub>O</sub><sub>2</sub> for more than a few hours. Active neutrophils consume high amounts of O<sub>2</sub> and can actually create or exacerbate a hypoxic environment in vivo and in vitro (63), which can accelerate the resolution of tissue inflammation.

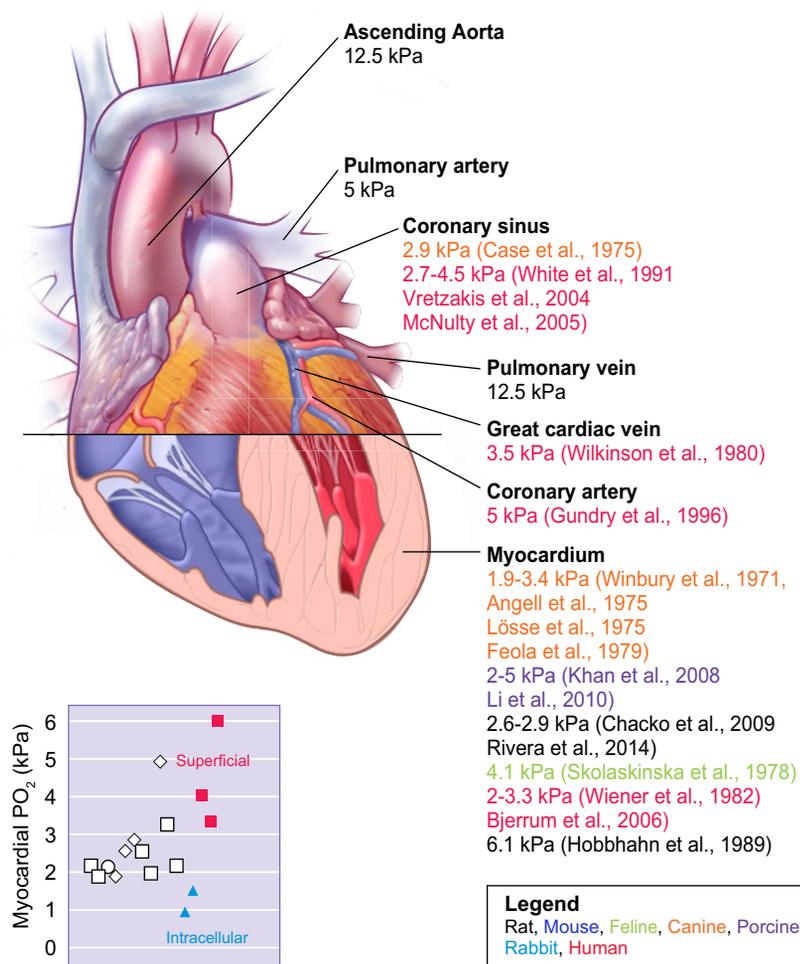
## C. Heart

The heart is second only to the lungs in terms of exposure to O<sub>2</sub>, yet in contrast to the lungs, it is a highly metabolically active tissue with a large O<sub>2</sub> requirement. Although the coronary artery branches directly from the ascending aorta in which blood is at its most oxygenated, measurements of cardioplegic solution P<sub>O</sub><sub>2</sub> sampled from numerous coronary artery branches in patients undergoing revascularization or aortic valve replacement surgery reveal levels of 5 kPa (202). We could not find any measurements of coronary artery P<sub>O</sub><sub>2</sub> in healthy humans or experimental animal models, and thus, whether these measurements reflect normal physiology or are lower as a result of disease remains unclear. Interestingly, P<sub>O</sub><sub>2</sub> values not much lower than these are reported within the coronary sinus in humans [2.7–4.4 kPa (385, 624, 646)], canine [2.9 kPa (69)], and in the great cardiac vein of patients undergoing coronary artery bypass surgery [3.5 kPa (651)]. Using a blood-borne phosphorescent probe, Rumsy and colleagues (496) measured the P<sub>O</sub><sub>2</sub> distribution in the epicardial microvasculature of the porcine heart before and during infarction. An average P<sub>O</sub><sub>2</sub> of 2.2 kPa was recorded in noninfarcted tissue, with a gradient observed toward the ischemic core. The coronary microvasculature penetrates the myocardium superficially, and compression of microvessels during systole means perfusion of the deep myocardial tissue is intermittent. As a result, a gradient of P<sub>O</sub><sub>2</sub> has been observed between the superficial epicardium, the deep myocardium, and individual myocytes, as illustrated in **FIGURE 11**. Such levels range from 4.1 to 6.1 kPa at the epicardial surface (245, 543) to 3.4 kPa in the subepicardium (3-mm depth in the canine heart) (654)

and 2–3 kPa in the myocardial tissue (11, 40, 72, 150, 297, 358, 487, 648, 654). Hence, coronary microvascular P<sub>O</sub><sub>2</sub> [2.2 kPa (496)] closely matches the average adjacent tissue P<sub>O</sub><sub>2</sub>, supporting the concept that a significant portion of O<sub>2</sub> diffusion must occur upstream of the capillary bed.

The increase in O<sub>2</sub> between the endocardium and coronary sinus reflects the increasingly acknowledged arteriolar/venular shunting hypothesis of O<sub>2</sub> distribution (328, 594). Generally, excellent corroboration exists in cardiac P<sub>O</sub><sub>2</sub> measurements using a variety of techniques including the use of implantable EPR probes, which can be used to monitor cardiac P<sub>O</sub><sub>2</sub> with impressive temporal resolution (72, 339, 487) and are stable for at least 112 days in situ (297), although these typically do not offer great spatial resolution. Anatomical complexity in O<sub>2</sub> delivery is compounded by the extremely high O<sub>2</sub> consumption rate of cardiomyocytes (see section IVC), resulting in very low intracellular P<sub>O</sub><sub>2</sub> [1–1.6 kPa (84, 252)], although this low O<sub>2</sub> does not limit aerobic respiration in these cells (84). Myoglobin, present within the cytosol of skeletal and cardiomyocytes, has a greater affinity for O<sub>2</sub> than Hb [P<sub>50</sub> of ~0.3 versus ~3.5 kPa (12)] and is thought to facilitate O<sub>2</sub> delivery to respiring mitochondria (567, 568). It may do this simply by providing a store of O<sub>2</sub> within the cell that can be made available during periods of increased activity or, perhaps, by removing dissolved O<sub>2</sub> from the cytosol, thereby increasing the concentration gradient from the blood to cell in a process of facilitated diffusion (90, 234, 281, 657, 658). Hence, actual O<sub>2</sub> content within a cardiomyocyte in vitro will be higher than the detected dissolved P<sub>O</sub><sub>2</sub>, complicating interpretations of relative monolayer oxygenation.

Stem cells derived from human myocardial biopsies cultured at a P<sub>O</sub><sub>2</sub> of 5 kPa exhibit greater chromosomal stability and fewer karyotypic defects over 1–2 mo of culture than their room air counterparts (343). Moreover, a greater yield was achieved per biopsy, with a higher reparative capacity when subsequently transplanted into a mouse infarcted heart (342). Interestingly, Puente et al. (471) recently demonstrated that the dramatic rise in cardiac tissue P<sub>O</sub><sub>2</sub> in the fetal heart at birth induces growth arrest through oxidative damage. This elegant study may explain the en-



**FIGURE 11.** Oxygen distribution in the adult heart. Illustration depicting the  $\text{PO}_2$  within the heart, summarizing published studies for different species with known values established in physiology. Individual myocardial  $\text{PO}_2$  values are further summarized in the adjacent graph, separated according to technique used:  $\square$ , microelectrode penetration;  $\triangle$ , derived from measurements of myohemoglobin saturation, in which  $\text{PO}_2$  was interpolated based on known species Hb dissociation curves;  $\circ$ , phosphorescence quenching microscopy; and  $\diamond$ , implanted electron paramagnetic resonance (EPR) probes. Values are color-coded to highlight those taken at superficial sites (red) or single-cell intracellular measurements (blue).

hanced proliferative and reparative potential of cardiac stem cells under physiological  $\text{O}_2$  levels, especially when one considers that the true intracellular  $\text{O}_2$  level in these cells may be considerably lower than 5 kPa.

Murine cardiac fibroblasts cultured at a  $\text{PO}_2$  of 3 kPa were also found to proliferate more rapidly, which was attributed to reduced expression of p21 and a less oxidized environment (494). However, because intracellular  $\text{PO}_2$  in these cells are likely to be considerably lower than the ambient (and physiological) 3 kPa, these results more accurately represent a hypoxic phenotype acknowledged by the authors. In line with this, human cardiac fibroblasts cultured under perfused conditions at a  $\text{PO}_2$  of 5 kPa exhibit decreased growth relatively to room air and hypoxic (1 kPa) cultures (600), suggesting hypoxia and hyperoxia, but not physiological normoxia, are potent triggers for fibroblast proliferation in vitro. In this recent study, a clear delineation between the cellular response to normoxia (5 kPa) and hypoxia (1 kPa) is demonstrated, with hypoxia strongly associated with markers of pathological cardiac remodeling (600). However, cells were subjected to altered ambient  $\text{PO}_2$  for only 24 h in this study and hence may not represent truly adapted cells. Rat neonatal cardiomyocytes isolated and

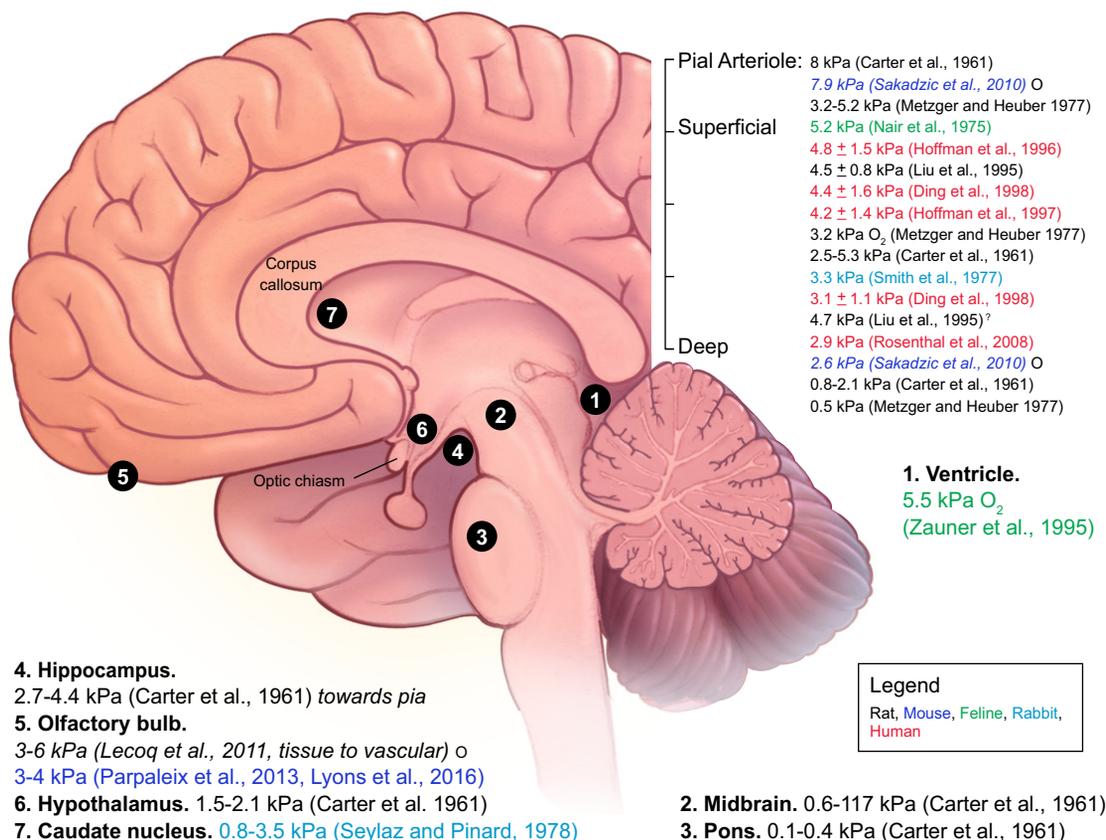
maintained at a  $\text{PO}_2$  of 5 kPa release higher concentrations of adenosine but rapidly release the vasoconstrictive angiotensin II when exposed to higher  $\text{O}_2$  levels (655). Although limited, these studies collectively demonstrate that culture of cardiac-derived cells under physiological  $\text{O}_2$  levels robustly alters their phenotype with significant therapeutic implications.

## D. Brain

The brain receives blood from mainly the common carotid artery and, to a lesser extent, the vertebral artery, both of which branch directly from the ascending aortic arch. In line with microvascular  $\text{O}_2$  distribution outlined above, oxygen levels of  $\sim 8$  kPa have been measured in rat (70, 527) and mouse (501) pial arterioles. Moreover, a  $\text{PO}_2$  of  $\sim 3.5$  kPa in the pial parenchyma (at depth of  $\sim 50 \mu\text{m}$ ) (390, 527) indicates a significant loss of  $\text{O}_2$  across the pial arteriolar wall (527). Similar to other major organs, the cerebral vasculature extends superficially throughout the brain, with fewer vessels penetrating the inner layers of the cortex. Accordingly,  $\text{PO}_2$  within the cortex decrease proportional to the depth: from  $\sim 5$  kPa the superficial cortex (70, 111, 247,

248, 351, 688) to ~3 kPa in the deep white matter (70, 111, 390, 501, 544), as illustrated in **FIGURE 12**. This gradient further extends into the deeper regions associated with central nervous system function (hypothalamus, hippocampus, and midbrain). Surprisingly,  $\text{PO}_2$  levels within these regions have been measured as low as 0.5 kPa [0.5–1 kPa midbrain (70), 0.4 kPa pons (70), 1.5–2 kPa hypothalamus (70), and 0.8–3.5 kPa caudate nucleus (525)]. However, Lyons and colleagues (364) have challenged this concept recently. Using two-photon phosphorescence quenching method (section IIC), they observed no change in intravascular  $\text{PO}_2$  in either arterioles or venules of the somatosensory cortex with increasing depth from the surface (364). These authors proposed that anesthesia and associated stressful handling during the experiment setup may artificially alter brain activity and hence tissue  $\text{PO}_2$  (364). Prior measurements were made using the surgical insertion of a microelectrode, and therefore revisiting brain tissue  $\text{PO}_2$  levels using two-photon light microscopy could provide further insights (501, 502). Indeed, Lecoq and colleagues (328) were able to measure neuronal  $\text{PO}_2$  in the mouse olfactory bulb during odor stimulation, in which average microvascular  $\text{PO}_2$  increased from ~6 kPa to 7.5 kPa, simultaneous with similar increases in red blood cell velocity and intracellular  $\text{Ca}^{2+}$  (328). Nota-

bly, neuropil  $\text{PO}_2$  was substantially lower than the surrounding microvasculature (~3 kPa), yet still increased upon odor stimulation. In subsequent studies, a mean interstitial  $\text{PO}_2$  of 3–4 kPa was found in the murine olfactory bulb and somatosensory cortex (364, 445), consistent with previous studies using implanted ESR probes (125, 350, 439). Changes in brain oxygenation during stimulation or disease have become the focus of increased experimental and clinical studies, the former spurred on by the development of BOLD-MRI (see section IID). Although blood-oxygen level-dependent functional MRI imaging has established clinically that changes in blood saturation correlate with changes in neuronal activity within the predicted area [as reviewed (164)], this technique cannot be used to quantify absolute changes in  $\text{PO}_2$  in the brain. However, several recent studies using microelectrode and phosphorescence-quenching techniques have demonstrated quantitative changes in brain tissue  $\text{PO}_2$  (either in the microvasculature or surrounding neurons) upon sensory stimulation (256, 328, 445, 692). In these studies, stimulation of neuronal activity was associated with a transient reduction in tissue  $\text{PO}_2$ , likely representing localized increases in  $\text{O}_2$  consumption, followed by increases in local blood  $\text{PO}_2$  and flow, confirming similar observations using fMRI.



**FIGURE 12.**  $\text{O}_2$  distribution in the brain. Illustration depicting the reported  $\text{PO}_2$  distribution within the brain, with  $\text{PO}_2$  values concerning microvascular or gray matter arranged according to reported depth of measurement. In some cases, depth was estimated based on the methodological description. Studies marked with a ○ were conducted using two-photon phosphorescence quenching method (PGM).

Neurons isolated from rat striatum (578) and cortex (698), human fetal neurons and the neuronal cell line SH-SY5Y (617), as well as mouse astrocytes (95), have all been studied under physiological normoxia (defined by authors as an ambient  $P_{O_2}$  of 3–5 kPa). A common phenotypic change was observed in all these cell types following normoxic culture, characterized by a hyperpolarized mitochondrial membrane potential, reduced ROS generation and greater survival during prolonged culture. The latter two features may result from enhanced activity of manganese SOD under low  $O_2$  (617). The most significant impact to be uncovered following culture under normoxia is on neuronal mitochondria. In addition to mitochondrial hyperpolarization (578, 698), more dense mitochondrial networks have been observed (578). Moreover, a proteomic screen of SH-SY5Y cells maintained at a  $P_{O_2}$  of 5 kPa revealed significant induction of mitochondrial complex I proteins, most notably NADH:ubiquinone oxidoreductase subunit 3, which was associated with greater sensitivity to the complex I inhibitor rotenone (617).

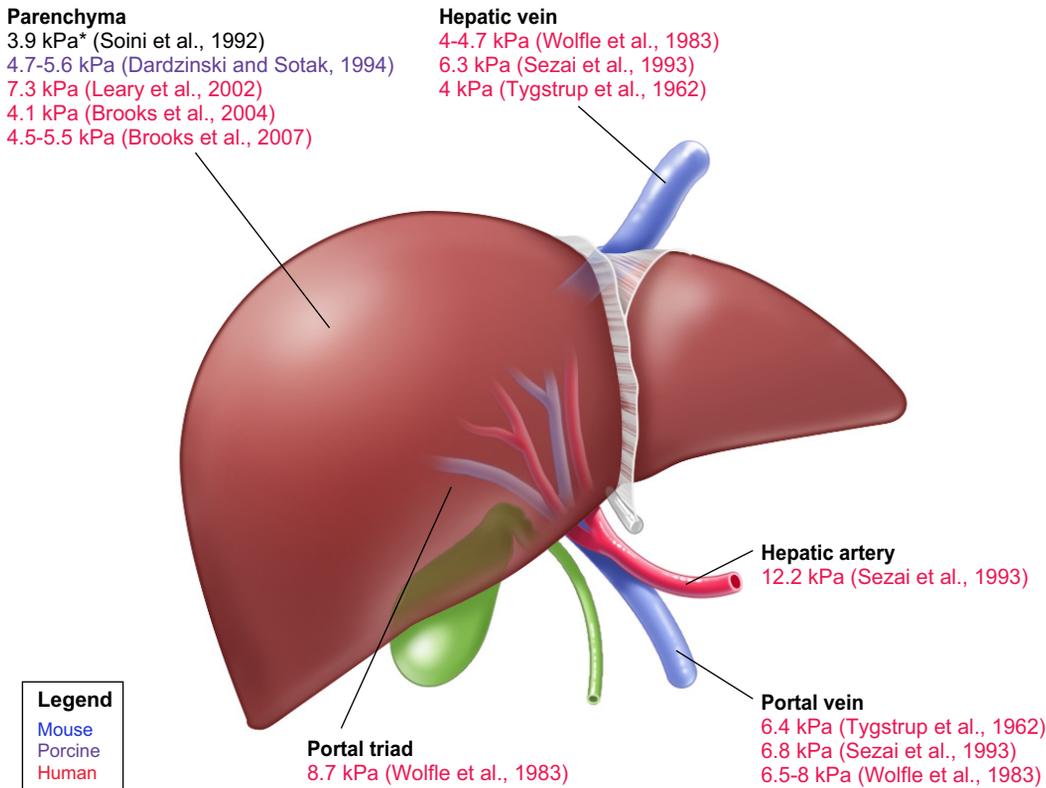
Neuronal stem cells (NSC), otherwise known as neuronal precursor cells, are adult stem cells which differentiate into neurons, astrocytes, and glial within the central nervous system. Neurogenesis generally occurs in regions of the inner brain, such as the hippocampus and dentate gyrus (135), and as such, occurs within a physiological  $P_{O_2}$  range of 0.5–3 kPa (see **FIGURE 12**). NSC from the embryo (554), sciatic nerve (409), cortex (553), midbrain (561), and ganglionic eminence (255, 258) all exhibit higher proliferation, survival, and differentiation potential when cultured at 3 kPa. These effects were associated with enhanced HIF-2 $\alpha$  stabilization and downstream protein expression (258, 554), resulting in an increased transplantation potential following in vitro expansion (553, 554). NSC from whole mouse brain homogenates cultured at 5 kPa also exhibit a higher differentiation potential associated with greater mitochondrial oxidative phosphorylation and reduced production of ROS (563). Although informative, this latter study makes no justification for the level of  $O_2$  used, instead opting for the arbitrary use of 5 kPa as physiological normoxia. Although not necessarily incorrect, the numerous studies listed above suggest that NSC may rarely experience a  $P_{O_2}$  of 5 kPa. Nonetheless, these and other studies have led many to propose a causal relationship between  $O_2$  concentration and stem cell differentiation potential (625), with numerous cell types displaying enhanced differentiation potential under lower  $O_2$  levels. This is corroborated by the anatomical topology of neurogenesis, which occurs predominantly in the brain regions containing lower  $O_2$  (**FIGURE 12**).

## E. Liver

The liver is a highly vascularized and metabolically active tissue and as such is relatively well oxygenated as illustrated

in **FIGURE 13**. Blood entering the hepatic artery is fully saturated and rich in  $O_2$  [human 12.2 kPa (526)]. Processed blood exiting the hepatic vein reportedly has a  $P_{O_2}$  between 4 and 6.5 kPa (526, 598, 660), whereas blood entering through the portal vein is at ~6.5 kPa (526, 598, 660). This dramatic gradient likely reflects the mixing of hepatic arterial blood with venous portal vein blood (at a ratio of 1:3) before entering the hepatic triad, as well as a high metabolic demand of the underlying tissue. Indeed, blood  $P_{O_2}$  within the portal triad is already reduced compared with that of the hepatic artery (8.7 kPa) (660). This level is further reduced within the liver parenchyma, where a  $P_{O_2}$  of between 4 and 7 kPa has been reported (54, 55, 103, 312, 327, 546, 608). Using the oxygen-sensitive EPR probes India ink and lithium phthalocyanine, Jiang et al. (275) were able to measure  $P_{O_2}$  localized to Kupffer cells and whole liver  $P_{O_2}$ , respectively, and demonstrated that Kupffer cells experience a lower  $P_{O_2}$  than the average liver parenchyma (2 versus 3.2 kPa). These values are lower than expected within the liver, possibly reflecting differences in experimental technique. The gradient between the portal triad and vein creates a functional polarization of the underlying hepatocytes, wherein nitrogen metabolism and albumin secretion are proportional to cell surface  $O_2$  level (37). This allows a similar effluent composition under conditions of flow reversal. Clearly, although a significant loss of  $O_2$  occurs during passage through the liver, this organ is still extremely well oxygenated in relation to other similarly active tissues such as the heart or brain (377).

Studies in vitro have provided some explanation for the abnormally high oxygen levels in liver tissue. In contrast to the majority of cell types, hepatocytes isolated from rat livers and maintained under low  $O_2$  (4–10 kPa) for the duration of culture (3–9 days) responded adversely. This included reduced viability (37, 345, 669) and diminished liver-specific gene expression (299, 345) and functions such as nitrogen metabolism and albumin excretion (37, 669). Moreover, several reports have highlighted the enhanced infectivity of liver-associated pathogens such as hepatitis C and *Plasmodium berghei* (during liver-stage malaria) in hepatocytes under low  $O_2$  conditions in vitro (421, 612). Interestingly, acetaminophen toxicity was less pronounced in mouse hepatocytes cultured at a  $P_{O_2}$  of 5 kPa relative to room air (668), although significantly higher basal lactate dehydrogenase release was observed in these cells. Part of this adverse response can be attributed to the very high  $O_2$  consumption rate of primary hepatocytes, which, during static cell culture in vitro, can create an extensive  $O_2$  gradient between air and cytosol (see section IVC) (75, 671). In this context, culture under previously regarded physiological  $P_{O_2}$  (4–10 kPa) may actually expose the cell monolayer to a  $P_{O_2}$  as low as 0.5 kPa (421). In corroboration, exposure to relatively high (but still lower than ambient)  $P_{O_2}$  (13–17 kPa) proved beneficial for cell yield (345, 368) and the response to phenobarbital challenge (299). HepG3 and



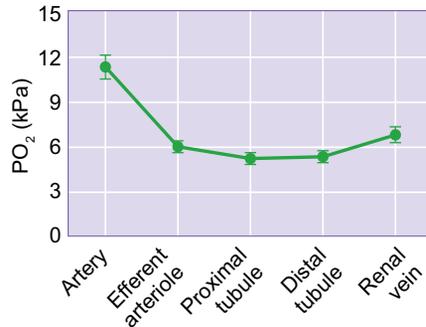
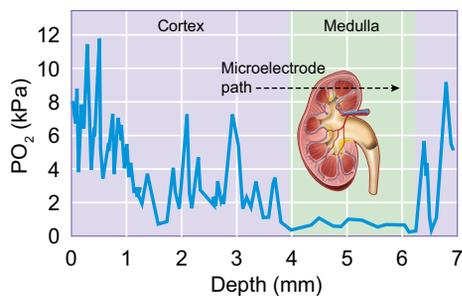
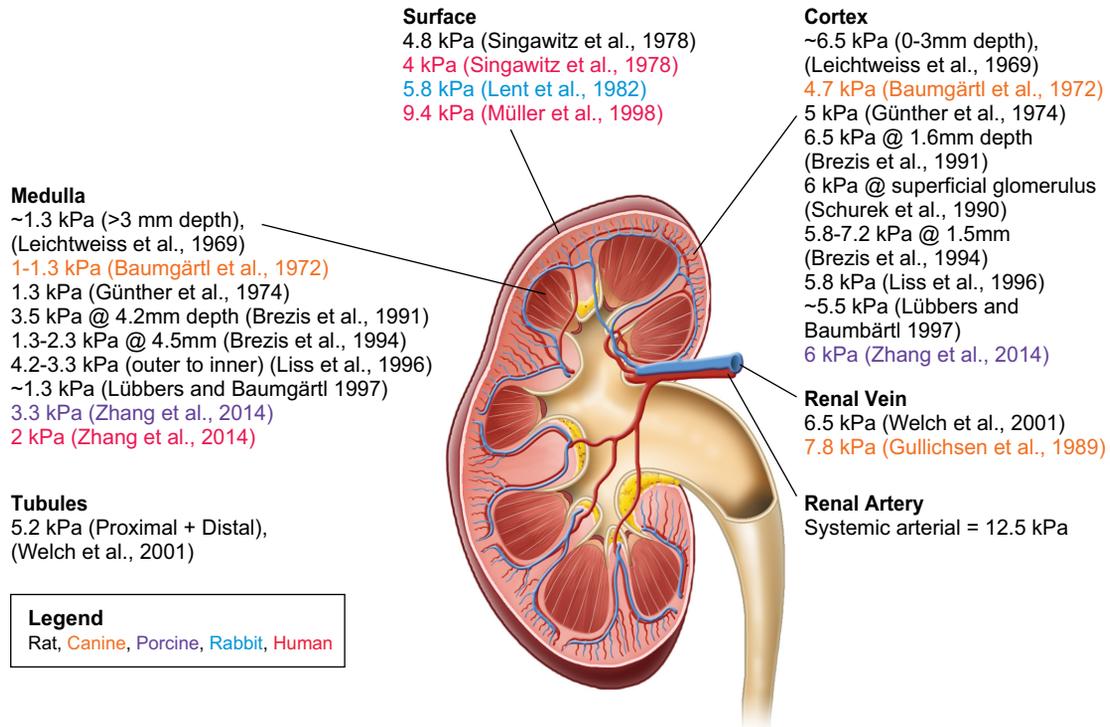
**FIGURE 13.**  $O_2$  distribution in the liver. Illustration of the reported  $PO_2$  distribution in the liver. Note, blood entering the sinusoids is a 3:1 mixture of portal venous and hepatic arterial blood, thus sinusoidal  $O_2$  concentrations can be estimated based on known values for the source vessels ( $PO_2 \sim 8$  kPa).

Hep3B cells cultured at 8 kPa for up to 30 days had higher intracellular, but not mitochondrial, ROS generation with severely reduced intracellular GSH levels (587). Despite this, SOD activity and expression were significantly higher in these cells, and they exhibited greater resistance to oxidative challenge. These studies in hepatocytes emphasize the need to understand monolayer oxygenation more closely. Ambient  $PO_2$  during in vitro culture must be accurately tailored to the cell type to avoid exposing high  $O_2$ -demanding cells to cellular hypoxia (204).

## F. Kidneys

The kidneys comprise only 1% of total body mass, yet filter ~20% of cardiac output (4.2 ml/min/g tissue) and as such are disproportionately perfused compared with the other organs. Indeed, renal cortical blood flow is the highest recorded per gram of tissue within the body (386), and the metabolic requirements are relatively low under normal conditions, yet increase linearly with glomerular filtration rate, renal blood flow, and  $Na^+$  transport (479, 642). Considering such hyperperfusion, renal tissue should be extremely well oxygenated as with other well-perfused organs such as the liver (see above). Counterintuitively, however, renal cortical  $PO_2$  has been measured at 4.7 kPa in the dog (28), 5–7 kPa in the rat (50, 51, 203, 334, 349, 362, 519, 642), 6 kPa in the pig, and 4–9.5 kPa in human (411, 541).

When the measuring electrode is advanced beyond ~3 mm (in the rat kidney), a sharp reduction in tissue  $PO_2$  is observed corresponding to entry into the medulla (see **FIGURE 14**), where  $O_2$  levels are between 1 kPa in the dog (28), 1.3–4.2 kPa in the rat (50, 51, 203, 334, 349, 362, 519, 642), 3.3 kPa in the pig (693), and 2 kPa in human (693). In elegant work by Lübbers and Baumgärtl, a large heterogeneity in cortical  $PO_2$  was observed whereby some regions experienced near-arterial  $PO_2$  values (~11 kPa) (334, 362). Such heterogeneity was not apparent within the medulla, prompting these authors to conclude that the highly vascularized anatomy of the cortex results in the formation of large intrarenal  $PO_2$  gradients. Using ultramicroelectrodes (diameter 3–5  $\mu m$ ), Welch and colleagues achieved measurements of  $PO_2$  in the nephrons of rats (642). In line with previous data, a significant drop in  $PO_2$  was reported between the renal artery and efferent arterioles (10.7–6 kPa), and tubular  $PO_2$  remained around 6 kPa before increasing within the renal vein to 6.7 kPa (see **FIGURE 14**). Kidney  $PO_2$  values determined by Clark electrode penetration were corroborated by recent measurements using BOLD-MRI (395, 451, 693), confirming the validity of both techniques. Notably, measurement of kidney  $PO_2$  using a dual laser Doppler blood flow/ $O_2$  electrode technique consistently demonstrated lower cortical  $PO_2$  values than the corresponding single  $O_2$  electrode [1.3 (434) and 2.1 (463) versus 5.3–6.7 kPa]. This disparity was attributed to the larger diameter



**FIGURE 14.**  $O_2$  distribution in the kidney. Anatomical illustration of known  $PO_2$  values in the kidney, derived from a number of different experimental models, species, and techniques. *Bottom left:* a representative trace obtained from invading an  $O_2$ -sensitive microelectrode into the rat kidney following the illustrated path. Depths corresponding to the cortex and medulla are highlighted. Adapted with permission from Lübbbers and Baumgärtl (362). *Bottom right:*  $PO_2$  values within an individual rat nephron. Adapted with permission from Welch et al. (642).

$O_2$  electrode required in the dual electrode array compared with that used in tissue penetration studies (350–500  $\mu\text{m}$  versus  $<20 \mu\text{m}$ ), potentially resulting in damage to the delicate kidney architecture (434).

The substantial drop in  $PO_2$  between the renal artery and cortical tissue prompted many to postulate the existence of a preglomerular  $O_2$  shunt (28, 334, 338). This was confirmed by Schurek and colleagues, who demonstrated that inspiration of gas at 100 kPa  $PO_2$  led to minimal changes in glomerular  $PO_2$  (5.6–9 kPa) despite a robust increase in systemic  $PO_2$  (12–74.6 kPa) (519). The close anatomical relationship between interlobular arteries and veins, and the absence of surrounding capillaries (141, 422), is thought to be responsible for such a shunt in line with the arteriovenous  $O_2$  transfer theory proposed by Duling and

Berne (123). Indeed, renal vein  $PO_2$  is unusually high compared with systemic venous  $PO_2$  (measured at 6.5 and 7.8 kPa in the rat (642) and dog (201), respectively, versus ~5 kPa), further corroborating renal arteriovenous  $O_2$  transfer. Moreover, although whole kidney  $O_2$  consumption is second only to the heart (10 versus 15 ml/min/g), renal blood flow far exceeds myocardial blood flow (750 versus 250 ml/min), and thus, renal  $O_2$  extraction is only ~10% versus 55% in the heart (452, 479, 485, 687). Taken together, these observations led O'Connor and colleagues to hypothesize that renal tissue is maintained at a low  $PO_2$  level relative to blood flow to prevent overoxygenation and excessive oxidative stress (433). Unfortunately, the side effect of this proposed adaptation is that segments of the papillae within the medulla (in particular the S3 proximal tubule and medullary thick ascending limb) are exquisitely sensi-

tivity to reductions in blood flow and are the first sites damaged during acute renal ischemia (46, 130).

Considering the prominent role of HIF signaling in the kidney (209) and its sensitivity to low oxygen (167, 398), relatively little has been published on the long-term culture of kidney-derived cells under physiological normoxia. This may, in part, be complicated by the significant differences in what may constitute normoxia in this tissue, with medullary  $\text{PO}_2$  values often 4–5 kPa  $\text{O}_2$  lower than corresponding cortical tissue (see above). Much like the gastrointestinal tract (see section VIG), parts of the renal medulla may exist in a state of physiological hypoxia. In intestinal epithelia, cellular phenotypes characterized at a  $\text{PO}_2$  of 1 kPa appear a better reflection of their *in vivo* counterparts than those cultured under room air. However, exposure of renal tubular epithelial cells to hypoxia (1–3 kPa) results in robust HIF downstream target protein (VEGF and EPO) induction (129, 209, 337, 417), phenotypes not observed in their counterparts *in vivo* (491). This discrepancy may reflect the artifactual baseline cellular  $\text{PO}_2$  before hypoxic exposure (room air,  $\text{PO}_2 \sim 18$  kPa), potentially exacerbating the subsequent hypoxic response. It would be interesting to explore whether small reductions in cellular  $\text{PO}_2$  around physiological normoxic values (from 1.5/2 to 1 kPa) can elicit more physiologically relevant responses in these cells. Such experiments may identify additional, more subtle roles for the HIF in renal cells and in doing so, shed further light on the renal cell specificity of von Hippel–Lindau syndrome (29, 419, 503).

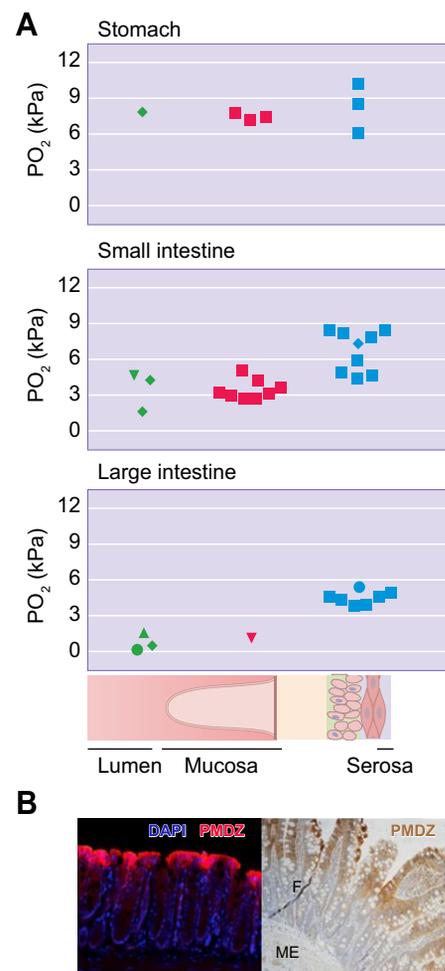
## G. The Digestive System

The discovery of anaerobic bacterium resident within the intestinal lumen led to the concept of physiological hypoxia within the adjacent intestinal tissue (696), with important implications for our understanding of host/microbiome interactions (292). This section aims to review the literature, with an overview of digestive system  $\text{PO}_2$  and discussion of the importance of considering the  $\text{O}_2$  environment during culture of cells derived from the digestive tract *in vitro*. The digestive tract is characterized by an adventitial (serosa) layer, a muscular middle layer, and an epithelial (mucosal) layer. Large arterioles run longitudinally along the serosa and the microvasculature (mesentery), penetrating toward the mucosal layer. Although the digestive tract receives a high proportion of blood flow, only 25% of this perfuses the mucosal and muscular layers at rest (81, 191). Measurements of digestive tract  $\text{PO}_2$  have been divided into luminal, mucosal, and serosal tissue, and the gradient between these values discussed when evident.

### 1. Stomach

The stomach, similar to the lungs and skin, can come into direct contact with atmospheric levels of  $\text{O}_2$ . As a result,

$\text{PO}_2$  measurements at the submucosal aspect of the gastric fundus—using microelectrodes are in the range of 6–10.2 kPa in humans undergoing esophagectomy (94, 264, 265, 529) and 7.6 kPa in experimental canine models (318), with similar values (8.4 kPa) reported in canine serosa (353). Using activated charcoal as an EPR probe (see section IID), He and colleagues (228) determined a luminal  $\text{PO}_2$  of 7.7 kPa at the level of the fundus/pylorus. Because  $\text{PO}_2$  values are roughly equal across the gastric wall (lumen > mucosa > serosa; **FIGURE 15A**), and such a level is not dissimilar from what might be expected in the arteriolar circulation (see section VIB2 and **FIGURE 9**), we might conclude neither the contents of the stomach or the cells of the gastric



**FIGURE 15.**  $\text{O}_2$  distribution in the gastrointestinal tract. **A:** Data from a number of studies (see text for more discussion and references) investigating  $\text{PO}_2$  distribution in the gastrointestinal tract. Values are separated into those taken from the stomach and small and large intestines and further divided according to anatomical/cellular location (lumen, mucosa, or serosa). Symbols are coded according to technique employed:  $\square$ , microelectrode;  $\Delta$ , approximate based on pimonidazole staining;  $\nabla$ , suffusion;  $\circ$ , phosphorescence quenching microscopy; and  $\diamond$ , electron paramagnetic resonance (EPR). **B:** Immunohistochemical images of the colon wall stained with the hypoxia-specific probe pimonidazole. Images are taken using either fluorescence (*left*) or bright-field (*right*) microscopes. Taken with permission from Kelly et al. (294) and Fisher et al. (157), respectively.

wall represent a significant source of O<sub>2</sub> consumption, at least under basal conditions.

## 2. Intestines

As illustrated in **FIGURE 15A**, a longitudinal gradient in luminal PO<sub>2</sub> is observed during passage along the gastrointestinal tract. From a luminal PO<sub>2</sub> of 7.7 kPa in the stomach (228), luminal PO<sub>2</sub> in the small intestine decreases to between 4.2 and 4.6 kPa (312), and decreases even further to 0.4–1.5 kPa in the large intestine (9, 228, 294, 346). Importantly, the techniques used to obtain such data, including EPR and two-photon phosphorescent quenching, are noninvasive and therefore avoid contaminating the bowel environment with atmospheric air and preserve the integrity of the bowel wall. A similar longitudinal gradient is observed in mucosal PO<sub>2</sub> (**FIGURE 15A**); from 6 to 10 kPa in the stomach to values of 3.5 kPa [rat (42)], 5.8 kPa [dog (353)], 2.6–5 kPa [pig (212, 213, 305, 429, 540, 611)], and 4.5–4.8 kPa [humans (529)] in the small intestine and values less than 1 kPa in the colon (9, 294). A similar longitudinal gradient is present, albeit fewer pronounced, at the serosal aspect (**FIGURE 15A**). Small intestine serosal PO<sub>2</sub> is 5.6 kPa [rabbit (163)], 7.2–8.4 kPa [pig (157, 213, 429, 540)], and 8.1 kPa in humans (570). In the large intestine, PO<sub>2</sub> at the serosal layer is reported at 4.6 kPa [rabbit (163)], 3.7–4.5 kPa [pig, corrected for FiO<sub>2</sub> 0.21 (301, 388)], 5.3 kPa [mouse (9)], and 3.9–5.5 kPa [human (412, 529, 530)].

From such data, it is clear that O<sub>2</sub> levels show a general decline along the length of the gastrointestinal tract, being highest in the stomach and lowest in the colon. It is perhaps of more interest to note that the radial gradient across the intestinal wall (lumen to serosa) does not behave proportionally. No detectable difference is observed between the lumen and serosa of the stomach, whereas the lumen of the large intestine is ~5 kPa lower than the serosal layer (**FIGURE 15A**). This radial gradient has been demonstrated directly in the small intestine using the penetrating microelectrode technique (42, 212, 429), by two-photon phosphorescence quenching method (540), and by pimonidazole staining (157), and also in the colon (294) (representative immunohistochemical images from the latter studies are shown in **FIGURE 15B**). Data from the study by Bohlen indicate a difference of as much as 2.3 kPa O<sub>2</sub> between the apex and base of a villus (42), whereas a difference of 4.6–9 kPa is reported between the mucosa and serosa (212, 429, 540). This is corroborated by a gradient in pimonidazole staining along the villus length (157, 294). It was originally proposed that this gradient occurs because of an arteriolar/venular O<sub>2</sub> shunt at the base of the villus, where vessels reside in close proximity to each other (42). However, the finding that this gradient is abolished by antibiotic treatment and is absent in germ-free mice (294) would suggest the O<sub>2</sub> consumption by the gut microbiome is wholly responsible. Upon reflection, this is logical given that the bacterial population increases along the gastrointestinal tract,

whereas there is no evidence to suggest the proposed arteriolar/venular shunt shows similar topographical changes.

The extremely low physiological PO<sub>2</sub> experienced by intestinal epithelium *in vivo* creates an interesting scenario whereby there is probably no real distinction between hypoxia and normoxia, but rather a state of physiological hypoxia exists in the intestinal mucosa (92, 696). Hence, those pathways traditionally important in coordinating a cellular response to pathological hypoxia, such as the HIFs (see section VA1), may have more importance in defining the phenotype of intestinal epithelia *in vivo*. Indeed, a healthy gut epithelium respiring on their preferred substrate butyrate exhibits profound HRE/luciferase activity and HIF-1 $\alpha$  stabilization (63, 294), indicating a persistent activation of the pathway. This constitutive activity was found to be essential for the production of defensins, key endogenous antimicrobial peptides secreted by the intestinal epithelium and accumulated within the mucus layer (293), which itself is regulated by HIF-1 $\alpha$  at a number of levels (170, 359). Moreover, expression of the multidrug-resistance protein 1 (P-glycoprotein) was also found to be dependent on constitutive HIF-1 $\alpha$  activity in the intestine (93). HIF activity is also crucial in maintaining intestinal barrier integrity, with key junctional proteins such as claudin-1 and creatine kinases M and B regulated by HIF-1 and HIF-2, respectively (180, 498). Notably, a key role for constitutive HIF-2 $\alpha$  activity in maintaining iron absorption has also been identified in the mouse duodenum, the epithelium of which also exhibits strong basal pimonidazole staining (379). Hence, the state of physiological hypoxia is important in maintaining host defense, barrier integrity, and iron absorption throughout the gastrointestinal tract.

Importantly, in the context of replicating normoxia *in vitro*, experiments in which intestinal epithelial cell lines (Caco-2 and T84) are exposed to physiological normoxia (PO<sub>2</sub> 1–2 kPa) generally corroborate such observations (see **TABLE 6** for summary). Notably, although few studies have extended the period of normoxic culture beyond 24 h, a number did demonstrate a stable phenotype after up to 4 days of normoxia (93, 566). A point worth discussing is the apparent discrepancy between the effects of low O<sub>2</sub> exposure on transepithelial resistance (TER) *in vitro* and *in vivo*. Exposure of Caco-2 and T84 cells to a PO<sub>2</sub> of 1–2 kPa induces no change or increases in TER *in vitro* (170, 284, 566), a characteristic unique to intestinal epithelial cells (170). In contrast, intestinal permeability is consistently decreased in mice breathing low O<sub>2</sub> (8 kPa) (170, 284, 408, 566). Aside from technical differences, there are two possible explanations for these observations. First, hypoxic exposure does not alter TER *in vitro* relative to room air cultured cells, a condition wholly artificial in the context of physiology. Moreover, if mucosal PO<sub>2</sub> is normally physiologically hypoxic (see above), then a reduction in inspiratory PO<sub>2</sub> (from 20.9 to 8 kPa) may create a genuinely pathologically hypox-

**Table 6.** *The effects of culture at physiological normoxia on intestinal cell physiology*

Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time (h)	Summary	Reference
T84	2.6	0–48	Intestinal epithelial cells maintain barrier resistance under hypoxia, whereas oral epithelia and endothelial cells increase permeability.	(170)
Caco-2 B			<p>↑ ITF mRNA by 4 h, maintained at protein level for 48 h, and is HIF-1 dependent.</p> <p>Anti-ITF antibody attenuates hypoxia-induced ↑ resistance in Caco-2 cells. Addition of ITF to endothelial cells ↑ resistance during hypoxia.</p> <p>ITF is induced in vivo by hypoxia (8% O<sub>2</sub>, 4 h).</p> <p>Hypoxia in vivo associated with increased permeability relative to normoxic controls. Possibly under pathological hypoxia in vivo.</p>	
Caco-2	2.6	0–96	<p>↑ MRD1 mRNA (18 h) and protein (maintained at 96 h, peak at 48 h) in hypoxia, dependent on HIF-1.</p> <p>Increase in protein translated to increased surface expression and function (drug efflux).</p>	(93)
T84	2.6	0–96	<p>↑ CD79 and CD339 mRNA (18 h) and protein (maintained at 96 h, peak at 48 h) in hypoxia, dependent on HIF-1.</p>	(566)
Caco-2			Both proteins are ecto-5'-nucleases responsible for metabolizing 5'-AMP to adenosine, which activates A2B receptors and ↑ barrier integrity.	
T84	2.6	0–48	<p>↑ MUC3 selectively by hypoxia: mRNA (maintained by 24 h) and protein (peaked at 24 h and declined afterwards). Probably HIF-1 mediated.</p>	(359)
ModeK			MUC3 interacts with ITF at the apical surface of epithelial cells.	
T84	2	0–48	Hypoxia ↓ adenosine uptake.	(408)
Caco-2			<p>↓ ENT1 and 2 mRNA and protein during hypoxia, maintained at 48 h and HIF-1-dependent</p> <p>siRNA against ENT2 decreased adenosine uptake, therefore explaining first observation.</p> <p>Hypoxia in vivo associated with increased permeability relative to normoxic controls. Possibly under pathological hypoxia in vivo.</p>	
T84	2	0–48	Time-dependent increased Netrin-1 protein during hypoxia, dependent on HIF-1 activity.	(492)
Caco-2			Endogenous netrin-1 reduces monocyte transepithelial migration via activation of the adenosine A2B receptor on the monocyte. This reduces inflammatory activation and therefore protects the epithelial barrier during inflammation.	
T84	1	0–24	HIF-1 conditional KO reduced expression of DEFB1 in mouse intestine and Caco-2 cells.	(293)
Caco-2			<p>Exposure to hypoxia ↑ HIF-1, although basal levels were observed.</p> <p>No change in DEFB1 protein during hypoxia, despite ↑ HIF and dependence on it.</p> <p>HIF-1 siRNA reduces hBD-1 soluble protein excreted, which would ↑ bacterial load in intestine</p> <p>In human bowel scrapings (epithelial-enriched), expression of DEFB1 mRNA correlated linearly with GLUT1 (HIF target), and hBD-1 staining was most prominent at apical edge of colonic mucosa.</p>	

*Continued*

Table 6.—Continued

Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time (h)	Summary	Reference
Caco-2	1	0–48	Enzymes involved in creatine metabolism regulated specifically by HIF-2 during hypoxia.	(180)
T84			Induction of CKM and CKB maintained at 48 h (protein) and abolished with HIF-2 siRNA CKM and CKB enzymes are localized to the apical surface of polarized epithelium and enriched at the adherens junction. HIF-2-dependent CK induction maintains barrier integrity and protects against inflammation. Inhibition of CK strongly decreases resistance under hypoxic conditions.	
Caco-2	1	0–144	Measurements of medium P <sub>O<sub>2</sub></sub> using optical sensor spots immobilized onto standard 24WPs, gas-permeable 24WP, and Transwell inserts. Medium P <sub>O<sub>2</sub></sub> reached 4 kPa after 6 days postconfluence in standard 24WP, whereas it was only ~15 kPa in gas-permeable plates and in inserts. Despite low O <sub>2</sub> levels, no HIF-1 stabilization was observed under standard conditions in normal plates. Medium volume was 1 ml: very high for 24-well plate, large depth would lead to O <sub>2</sub> depletion.	(690)
Caco-2	1	24	Hypoxic preincubation significantly reduced bacterial internalization. This was dependent on β-1 integrin, the protein levels of which were decreased by hypoxic exposure in correlation with increased HIF-1, although no definitive siRNA experiment was performed. Hypoxia reduces bacterial infection by downregulating β1 integrin.	(689)

CK, creatine kinase; CKB, creatine kinase B; CKM, creatine kinase M; DEFB1, β defensin gene; ENT, equilibrative nucleoside transporter; GLUT1, glucose transporter 1; hBD-1, human β-defensin; HIF, hypoxia-inducible factor; ITF, intestinal trefoil factor; MRD1, multidrug resistance protein 1; MUC, mucin; 24WP, 24-well plate.

ic/near anoxic environment within the mucosal intestinal epithelium. Similar conditions are observed during inflammatory bowel disease and ulcerative colitis (63, 284), conditions associated with increased intestinal permeability. Thus, fundamental differences in the context and degree of hypoxia under these experimental conditions make comparisons difficult to interpret. Second, whole body hypoxia undoubtedly has effects beyond the intestines, and it is therefore difficult to isolate the actions of any paracrine mediators released by other tissues also responding to reduced systemic arterial P<sub>O<sub>2</sub></sub>. Notably, work by Zeitouni and colleagues (689, 690), using O<sub>2</sub>-sensitive chips immobilized on the bottom of standard culture plates, indicates that exposure of Caco-2 cells to an ambient P<sub>O<sub>2</sub></sub> of ~1 kPa results in a near anoxic medium P<sub>O<sub>2</sub></sub> after 6 days (690). However, it should be noted that the authors used 1 mL of medium in a 24-well plate, double the recommended volume for such dishes. Using the example discussed in a previous section (section IVC), these conditions would generate a value for *d* double that commonly used (0.2 mm), facilitating self-inflicted hypoxia in this scenario. Ideally, the correct in vitro

experiment to accompany in vivo hypoxia models would be exposure of intestinal epithelial cells to very low (P<sub>O<sub>2</sub></sub> ~0–0.5 kPa) O<sub>2</sub> from a baseline of 1–3 kPa to more accurately reflect conditions generated in vivo.

### 3. The pancreas

Interest in pancreatic P<sub>O<sub>2</sub></sub> distribution arose largely out of the need to understand the oxygenation of endogenous islets to match this when implanted elsewhere. Using a microelectrode, Harper and colleagues (226) reported a P<sub>O<sub>2</sub></sub> of 3.3 kPa in the acinar/exocrine region of the exteriorized rat pancreas. This was corroborated by more detailed measurements by Carlsson and colleagues (66, 67), who reported a gradient from 4.6 to 2.7 kPa O<sub>2</sub> between the surface and interior of the exocrine pancreas. Kinnala and colleagues used a technique termed suffusion tonometry to monitor whole organ P<sub>O<sub>2</sub></sub> in the porcine pancreas. Briefly, a silicone tube is implanted into the tissue and equilibrated with anoxic saline. After a subsequent period of equilibration with the tissue, fluid is extracted from the tube and P<sub>O<sub>2</sub></sub> deter-

mined using a standard electrode. Using this technique, they reported pancreatic  $P_{O_2}$  values of 5.3 (302) and 5.6 (303), thus reasonably matching reported values using microelectrode techniques. The islets of Langerhans are important anatomical features of the pancreas wherein insulin and glucagon are synthesized and secreted. These tiny collections of cells constitute only 1%–2% of total pancreatic tissue, yet receive 10%–15% of organ blood flow (268). This extensive perfusion is reflected in a  $P_{O_2}$  level considerably higher than the surrounding parenchyma, between 5 and 6 kPa in the rat (66, 67).

The high rates of  $O_2$  consumption in pancreatic  $\beta$  cells has presented a unique problem during their isolation, culture, and implantation. Isolated  $\beta$  cells typically exist in culture as suspended spheroids, and pimonidazole staining illustrates that such conditions produced severe hypoxia (113, 438), which is proportional to medium  $P_{O_2}$  and islet size (310). This also extends to monolayer cultures of the pancreatic cell line MIN6, in which intracellular  $P_{O_2}$  (based on pimonidazole staining) was far below ambient (511). Moreover, exogenously implanted islets rapidly develop hypoxia regardless of their anatomical location (66, 67), reflecting an inability of neovascularization to counteract islet  $O_2$  consumption. Attempts to address this problem have included the use of permeable culture supports such as silicone membranes (18, 304), PFC-based culture dishes (166), or  $O_2$ -leaching materials (96) as well as culture under hyperoxic ambient  $P_{O_2}$  (50 kPa) (309). Using a PFC/polydimethylsiloxane construct, Fraker and colleagues elegantly demonstrated that the combination of high substrate solubility and lower ambient  $P_{O_2}$  (~12.6 kPa) produced the greatest volume of physiologically oxygenated (predicted pericellular  $P_{O_2}$  of ~5.5 kPa)  $\beta$  cells and almost no anoxic cells compared with culture under room air on traditional plasticware (166). This translated into greater  $\beta$  cell viability and function following isolation and a trend toward greater *in vivo* survivability once transplanted.

## H. Bone and Cartilage

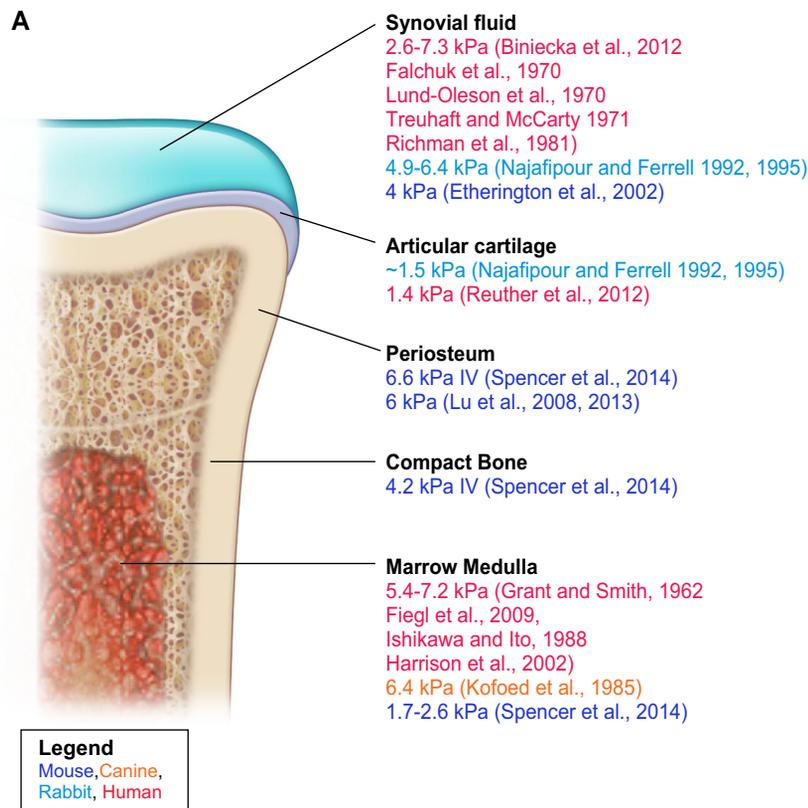
### 1. Bone and bone marrow

Typical bone consists of an outer cortical/compact layer, a spongy/cancellous inner layer, and the medulla containing the bone marrow (FIGURE 16A). The outer mineralized layers are sparsely populated with cells and are effectively avascular, and the only vessels found within this layer are the superficial periosteal arteries and penetrating nutrient arteries perfusing the bone marrow. As such, mineralized bone tissue exists at relatively low  $P_{O_2}$ . In the only known publication measuring bone extravascular  $P_{O_2}$ , Brighton and Heppenstall reported a steep gradient in  $P_{O_2}$  between the diaphyseal and metaphyseal regions (14.5 to 2.6 kPa) of the rabbit proximal tibial epiphyses (52). Because the reported  $P_{O_2}$  in the diaphyseal region is beyond the physio-

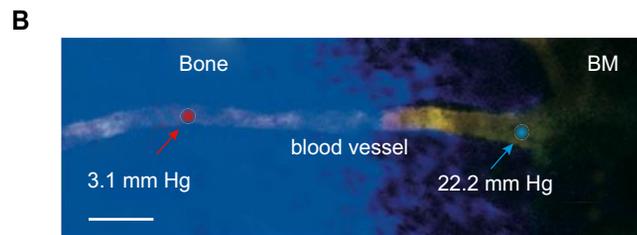
logical arterial range (12–13 kPa), the accuracy of these values necessitates further study. The concept of a steep gradient between regions of mineralized bone has been predicted mathematically (685). More recently, measurement of  $P_{O_2}$  distribution in the mouse tibia was partially accomplished using implantable lithium phthalocyanine crystal EPR probes (see section IID) (360, 361).  $P_{O_2}$  at the periosteum of normal tibia was 6 kPa (360), whereas localized  $P_{O_2}$  within the bone upon fracturing decreased significantly to ~1.5 kPa immediately after injury (361). Subsequent angiogenesis and healing resulted in a robust increase in bone  $P_{O_2}$  (from 1.5 to ~7 kPa), indicating that neovascularization of damaged bone can restore normal  $O_2$  distribution (361). Notably, periosteal  $P_{O_2}$  values reported by Lu and colleagues match closely the intravascular  $P_{O_2}$  values in microvessels of the periosteum [6.6 kPa (552)], suggesting a limited radial gradient in this tissue, which is consistent with the sparsely populated nature of mineralized bone.

The isolation and maintenance of human stem cells under low  $O_2$  has generated promising advances in their clinical application. Although effects of culture under physiological  $O_2$  levels on partially differentiated precursor stem cells have already been discussed under the auspice of their respective tissue origin, bone marrow is a primary source of adult pluripotent stem cells. Furthermore, this tissue is also the source of hemopoietic stem cells, which give rise to all circulating blood cells. As such, a detailed understanding of their physiological environment is of clinical relevance.  $P_{O_2}$  has been determined in human sternum [5.4 kPa (192)] and iliac crest marrow [6.8 (262), 7.2 (227), and 6.1 kPa (154)], canine femoral medulla [6.4 kPa (308)], and mouse femoral marrow [~4 kPa (71)]. These measurements were largely obtained from blood gas analysis following the aspiration of marrow. Recently, detailed *in situ* measurements of marrow  $O_2$  levels in living mice have been obtained using the more advanced two photon light microscopy method (see section VIC) (552), with impressive resolution. Spencer and colleagues (502) reported an intravascular  $P_{O_2}$  gradient between vessels in the periosteum (6.6 kPa), cortical bone (4.2 kPa), and marrow (3 kPa). By comparing intravascular and extravascular  $P_{O_2}$  within the bone marrow, these authors identified a significant radial gradient (~1.5 kPa) in these vessels, which could be abolished by sublethal irradiation or chemotherapy. Indeed, localized bone marrow hypoxia was associated with large clusters of cells within the marrow, indicating that  $O_2$  consumption maintains a low  $P_{O_2}$  environment in the bone marrow.

Although elegant and informative, the study by Spencer and colleagues reports bone marrow  $P_{O_2}$  values considerably lower than values reported by numerous other laboratories (~2 versus ~5 kPa). Tissue trauma associated with bone marrow aspiration or microelectrode penetration may lead to artificially high marrow  $O_2$  level estimations, and hence, the noninvasive measurements by Spencer et al. may be



**FIGURE 16.** Oxygen distribution in bone and cartilage. *A*: Distribution of  $O_2$  within a typical synovial joint. *B*: Representative image highlighting the passage of a microvessel (yellow) from the outer bone (blue) into the marrow (black). Intravascular  $PO_2$  was determined at two different points: within the bone (red arrow and dot) and within the marrow (green arrow and dot). Adapted with permission from Spencer et al. (552). IV, intravascular.



physiologically representative. Species differences are an unlikely explanation, because Ceradini et al. (71) reported a bone marrow  $PO_2$  of ~4 kPa in the mouse femoral marrow. Instead, regional differences in bone  $PO_2$  may provide some clarification, with Spencer et al. opting to study the calvaria (skull cap) in contrast to the femur, sternum, or iliac crest. Similarly,  $PO_2$  distribution in the brain microvasculature differs subtly from other microvascular beds (**FIGURE 9**).

## 2. Cartilage and synovial fluid

Many bones are connected via a synovial joint consisting of a fluid-filled synovial cavity and articular cartilage lining the epiphyses of the bone (**FIGURE 16A**). In addition to providing mechanical support during movement, synovial fluid is also crucial in supplying nutrients, including  $O_2$ , to the articular cartilage, which itself is completely avascular. Chondrocyte physiology is strongly influenced by  $O_2$  tension, during development and in adult life (513), and increases in  $O_2$  consumption are observed during rheumatoid arthritis-associated inflammation (331). For these reasons,

understanding  $PO_2$  distribution within the synovial joint is of great interest. Of the studies reporting synovial  $PO_2$  values, only two investigated synovial fluid  $PO_2$  in healthy tissue. Ferrell and Najafipour (1992) reported a mean  $PO_2$  of 6.4 kPa in the rabbit knee (152). Using microelectrode penetration, these authors also demonstrated a gradient in  $PO_2$  between the superficial synovial membrane and articular cartilage, at which point, mean  $PO_2$  reached ~1.5 kPa, a value corroborated in human septal cartilage more recently (482). Although such  $PO_2$  distribution traces are commonly reported in numerous tissues, the study of a synovial joint under immobile anesthetized conditions may create an artifactual gradient which would not otherwise be present in a mobile joint (152). Indeed, Etherington and colleagues (137) reported a transient increase in knee synovial  $PO_2$  upon mobilization of the joint. A number of studies have reported synovial fluid  $PO_2$  in the human arthritic knee, with values ranging from 2.6 (38), 3.5 (363), 3.7 (143), 4.1 (588), and 5.7 (363) to 7.3 kPa (484). Inflammatory arthritis was also associated with a decline in knee synovial  $PO_2$  in rabbits (416) and mice (137). In general, synovial  $PO_2$  cor-

related negatively with the severity of inflammation (588), with relationships to blood flow (416) and white blood cell count (484) observed. Furthermore, patients with osteoarthritis had significantly higher synovial fluid  $P_{O_2}$  than those with rheumatoid arthritis (363). Hence, it is likely that the inflamed nature of the arthritic joint produces a pathophysiologically hypoxic environment relative to the normal joint, and thus,  $P_{O_2}$  values derived from the study of such joints likely underestimate physiological normoxia.

### 3. Resident bone cells

As described in sections VIG1 and VIG2, the avascular nature of mineralized bone and cartilage creates a physiological milieu containing relatively little  $O_2$  (~1.5 kPa in deep cortical bone and articular cartilage) for resident cells. **TABLE 7** provides an overview of studies conducted to investigate the effects of culture at physiological normoxia on bone cell physiology. Long-term culture (>72 h) of osteoblasts at the lower end of this physiological range ( $P_{O_2}$  2 kPa) is associated with a significant reduction in mineralization ( $Ca^{2+}$  deposition as measured by Alizarin red staining) and alkaline phosphatase activity compared with room air cultures (329, 423, 435, 601, 686). This was reportedly due to a delayed (601) or reduced (423) expression of the osteocyte markers osteocalcin and procollagen lysine dioxygenase and was associated with a reduced ability to synthesize and deposit collagen (435). Indeed, microarray analysis of human osteoblastic cells (SV40-transformed Human Fetal Osteoblastic cells) cultured at 2 kPa for up to 3 wk revealed the greatest impact of low  $O_2$  on the mineralization phase of differentiation (424). However, culture under an ambient  $P_{O_2}$  of 2 kPa would result in a much lower intracellular  $P_{O_2}$ , and hence, this phenotype is likely representative of a reactive, hypoxic cell rather than the physiological norm. This hypothesis is corroborated by the observation that preosteoblastic cell lines (MC3T3-E1 and MLOA5) cultured long term at a  $P_{O_2}$  of 2 kPa exhibit marked HIF-1 $\alpha$  stabilization (686), pimonidazole staining, and HRE luciferase activity (329), indicating a classical hypoxic phenotype. In contrast, paired cultures maintained at a  $P_{O_2}$  of 5 kPa showed no such HIF-1 $\alpha$  activity (329), consistent with our findings in human endothelial cells maintained >5 days under similar conditions (see **FIGURE 10**). Under this more physiologically relevant  $P_{O_2}$  (accommodating for monolayer consumption), MC3T3-E1 cells exhibited earlier and more robust mineralization and alkaline phosphatase activity, which was associated with increased expression of the osteocytic markers osteocalcin, Dmp1, Mepe, and Fgf23 (241). Similar findings were reported in murine calvarial organ cultures maintained under 5 kPa  $O_2$  (241). These findings suggest that higher  $O_2$  levels may stimulate osteocyte maturation and mineral bone formation in vivo, supported by the knowledge that the highest intraosseal  $P_{O_2}$  values (6–7 kPa) recorded are in the periosteal layers of diaphyseal bone (52, 552). Thus, the appropriate

intracellular  $O_2$  level in vitro should be defined based on the differentiation state to be studied.

### 4. Chondrocytes

Grimshaw and Mason (2000) (196) attributed the unusual ability of chondrocytes to withstand severe hypoxia to a very low mitochondrial mass in vivo (53) and low  $O_2$  consumption rates in vivo and in vitro (240). As chondrocytes experience very low  $O_2$  levels in vivo (~1.5 kPa, see **FIGURE 16A**),  $O_2$  conservation may be necessary. There are numerous studies of chondrocytes during culture under normoxic conditions in vitro, as summarized in **TABLE 8**. Such studies have largely focused on culture techniques to reverse the dedifferentiation of primary chondrocytes that occurs following isolation and monolayer culture in vitro. Dedifferentiation is characterized by a switch in collagen production from type II to type I (34), with concomitant downregulation of key chondrocyte markers aggrecan and SOX9. Although very low  $O_2$  (<1.5 kPa) levels exist in deep articular cartilage, new cartilage is formed at the superficial layer adjacent to the synovial fluid where  $P_{O_2}$  values are closer to 5 kPa (see **FIGURE 16A**). When cultured on alginate beads at a  $P_{O_2}$  of 5 kPa for 2–4 wk, the phenomenon of redifferentiation is accelerated and enhanced in human (287, 414, 518), bovine (117, 118, 239, 415), mouse (242), and rabbit (233) chondrocytes. In addition to the expression of *Col2a1*, *Aggrecan*, and *SOX9*, increased deposition of collagen and glycosaminoglycan was frequently observed in alginate 3D bead cultures (518). Furthermore, enlarged matrix area was noted in E14.5 murine forelimbs cultured ex vivo at 5 kPa (242), indicating this effect is not confined to isolated cells.

Culture in 3D alginate beads presents a particular problem concerning  $O_2$  diffusion, and ultimately, intracellular  $P_{O_2}$ . Li et al. (341) addressed this question using a combination of experimentally determined  $O_2$  consumption rates and  $P_{O_2}$  distribution modeling in scaffold-free aggregate cultures seeded at various densities. They reported a critical threshold of ~8 kPa, at which point cells no longer synthesized collagen and preferentially produced proteoglycans. How this relates to previous studies is unclear given that the majority of the studies cited above use cells cultured in pellet or alginate 3D conditions at 5 kPa and report increased collagen deposition relative to room air cultures. Based on the  $P_{O_2}$  profiles published by Li et al., average pellet  $P_{O_2}$  may be closer to 8 kPa when cultured at room air (~18.5 kPa) than under 5 kPa, and therefore, one might expect increased collagen deposition in these pellets. Despite this, gradients in collagen deposition have been observed in alginate beads under 5 kPa, with the highest collagen-associated staining apparent at the periphery (117). Thus, the concept of a critical threshold for collagen deposition may have some merit, but discrepancies in the actual  $P_{O_2}$  value are expected given differences in  $O_2$  diffusion between scaffold-free and alginate cultures.

**Table 7.** *The effects of culture at physiological normoxia on bone cell physiology*

Species	Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time	Comments	Reference
Human	SV-HFO (human osteoblastic cell line)	2	3 wk	↓ Mineralization due to less differentiation and maturation of extracellular matrix components (collagen). ↓ ROS (mitoSOX and DCF) and lower expression of SOD1/2 and CAT.	(423)
		2	3 wk	Microarray of cells cultured at 2 kPa for various phases of differentiation. Impact most prominent during early phase when mineralization begins to occur.	(424)
Mouse	MC3T3-E1 preosteoblast Calvarial organ culture	5	35 d	Earlier and greater Ca <sup>2+</sup> mineralization. ↑ ALP staining and earlier. ↑ Osteocalcin expression initially, but declined by 35 d. ↑ Cx43 expression at cell/cell junctions and whole cell lysates. ↑ Osteocyte markers (Dmp1, Mepe, and Fgf23). ↑ Osteocyte population (cells expressing Dmp1 and Mepe) in organoid cultures.	(241)
	MC3T3-E1 preosteoblast	2,5	72 h	Two kPa strongly associated with HIF stabilization (PMZD staining and HRE luciferase), not observed at 5 kPa. ↑ PGE <sub>2</sub> production and EP1 receptor expression at 2 kPa.	(329)
	MLOA5 (preosteoblast)	2,5	7 d	↓ P <sub>O<sub>2</sub></sub> associated with ↓ ALP activity and mineral deposition.	(686)
	MLOY4 (osteocyte)			No change in viability. ↑ HIF stabilization at 2 kPa preserves cell function under hypoxia.	
Rat	Calvarial osteoblasts	10	7 d	Compared with hyperoxia (90% O <sub>2</sub> ), ↑ proliferation. No change in ALP activity.	(595)
	Primary osteoblasts	0.2–20	18 d	↓ Bone module formation with ↓ P <sub>O<sub>2</sub></sub> . At 2 kPa O <sub>2</sub> , ↓ proliferation, but no change in apoptosis. Delayed osteoblast differentiation markers (osteocalcin and PLOD) and ↓ collagen production.	(601)
Rabbit	Periosteal organ culture	1–90	6 wk	Highest growth and chondrogenesis at 15 kPa. ↓ Collagen synthesis at very high and very low O <sub>2</sub> levels. Culture in a “sealed jar” apparatus.	(435)

ALP, alkaline phosphatase; CAT, catalase; Cx43, connexin 43; DCF, dichlorofluorescein; Dmp1, dentin matrix protein 1; EP1, prostaglandin E receptor 1; Fgf23, fibroblast growth factor 23; HIF, hypoxia-inducible factor; HRE, hypoxia-responsive element; Mepe, matrix extracellular phosphoglycoprotein; PGE<sub>2</sub>, prostaglandin E<sub>2</sub>; PLOD, procollagen lysine, 2-oxoglutarate, 5-dioxygenase; PMZD, pimonidazole; ROS, reactive oxygen species; SOD, superoxide dismutase; SV-HFO, SV40-transformed human fetal osteoblastic cell.

### 5. Marrow-derived stem cells

The concept of a stem cell niche within the bone marrow and its influence on mesenchymal and hematopoietic stem cell (HSC) fate are front and center in our understanding of the physiology of these cells. Elegant imaging-based investigations have demonstrated that HSC preferentially localize to small arterioles within the endosteal marrow (319), and that variations from this niche induce a proliferative

and hypoxic phenotype (319, 430). Given our knowledge that the steepest O<sub>2</sub> gradients outside the lungs exist across the walls of arterioles (section IIIB and **FIGURE 9**), it is likely that steep gradients in P<sub>O<sub>2</sub></sub> also exist in between arterioles within the bone marrow. Such heterogeneity in marrow P<sub>O<sub>2</sub></sub> may be confounded by regional heterogeneity in cell populations, with various degrees of cellular activity and thus O<sub>2</sub> consumption (552). Measurements of marrow P<sub>O<sub>2</sub></sub> range from 1.7 to 7.2 kPa (**FIGURE 16B**), yet no study has directly

**Table 8.** *The effects of culture at physiological normoxia on chondrocyte physiology*

Species	Cell Type	Po <sub>2</sub> (kPa)	Time	Comments	Reference			
Human	Chondrocytes	5	4 wk	↑ Collagen II, aggrecan, and SOX9 mRNA in 3D culture. ↑ Proliferation and GAG synthesis. No change in pH or glucose consumption. Redifferentiated phenotype only achieved when 5 kPa O <sub>2</sub> and 3D culture combined.	(414)			
				Meniscus cells Chondrocytes	5	2 wk	No change in collagen I mRNA. ↑ Collagen II and SOX9 mRNA in meniscus cells, but not chondrocytes.	(4)
							5	3 wk
				5	5 d	No change in aggrecan or Col I mRNA expression or in DNA content, lactate production, or glucose consumption. ↑ VEGF production and mRNA levels at pH 7.4 and 5 kPa O <sub>2</sub> .		
						5	4 wk	No change in growth or DNA content. ↑ CD44 and CD105 expression. ↑ Pellet volume and GAG content. No change in col1/2 mRNA expression, but ↑ aggrecan mRNA.
				20	N/A			Modeling O <sub>2</sub> consumption and Po <sub>2</sub> profiles in 3D alginate chondrocyte cultures. Po <sub>2</sub> < 8 kPa makes chondrocytes favor proteoglycan synthesis over collagen.
Bovine	Chondrocytes	3–60	6 d	↓ DNA content with ↓ Po <sub>2</sub> . ↓ Sulfate incorporation, as indicative of GAG synthesis, with ↓ Po <sub>2</sub> . ↑ Proteoglycan aggregation with ↓ Po <sub>2</sub> .	(86)			
				0.1, 5, 10, 20	7 d	No change in viability or proliferation, which didn't actually occur. No change in aggrecan expression. ↑ Pellet volume peaking at 10 kPa O <sub>2</sub> , indicative of ↑ collagen synthesis. No change in pH until 0.1 kPa. ↓ rRNA yield at 0.1 kPa. Suggested that chondrocytes are particularly robust in withstanding hypoxia relative to other cell types.	(196)	

*Continued*

Table 8.—Continued

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time	Comments	Reference
		5	4 wk	No change in growth, viability, or pH. No change in collagen I mRNA. ↑ Collagen II and aggrecan mRNA. ↑ Matrix collagen and GAG content during 3D culture. Culture at 5 kPa exacerbated redifferentiation during 3D culture. All culture performed on orbital shakers so pericellular P <sub>O</sub> <sub>2</sub> was also ~5 kPa.	(415)
Bovine		5	3 wk	↓ Collagen I mRNA during redifferentiation. ↑ Collagen II and XI and aggrecan mRNA during redifferentiation. ↑ Collagen staining in 3D beads, especially toward the periphery in which P <sub>O</sub> <sub>2</sub> would be highest.	(117)
		5	3 wk	↓ Collagen I and ↑ collagen II/aggrecan mRNA and staining during redifferentiation. ↑ Sulfate and proline incorporation, indicative of GAG and proteoglycan synthesis.	(118)
		2, 5	14 d	↓ Proliferation at both O <sub>2</sub> levels, but no change in protein content. ↑ O <sub>2</sub> consumption during monolayer culture, which was proportional to P <sub>O</sub> <sub>2</sub> . ↑ ROS at 20 kPa. Differences in cellular phenotype between 2 and 5 kPa.	(240)
		2, 5	9 d	↑ Mitochondrial mass during culture, more pronounced at 20 kPa than 2. Associated with ↑ oxidative phosphorylation. ↑ ROS and O <sub>2</sub> consumption at 20 kPa, which could be restored to fresh/2 kPa values, but treatment with NAC. ↑ GAG accumulation in 3D culture at 5 kPa.	(239)
Mouse	C3H10T1/2	5	7 d	↑ BMP-2 induced GAG synthesis with concomitant ↓ ALP activity and alizarin red staining, indicating less osteoblastic differentiation. No change in adipocyte differentiation. No change in proliferation. ↑ Col2a1 mRNA expression and ↓ Col10a1 mRNA expression, mediated by ↑ p-p38 and HDAC4 activity. Enlarged matrix area in forelimbs cultured at 5 kPa O <sub>2</sub> . 5 kPa O <sub>2</sub> promotes chondrogenic differentiation, but not terminally.	(242)
	E14.5 murine forearm limb				

Continued

Table 8.—Continued

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time	Comments	Reference
Rabbit	Chondrocyte	5	3 wk	↑ Proliferation ↑ Collagen II mRNA but no change in aggrecan or collagen I. ↑ Aggregation with more collagen and GAG deposition. Culture at 5 kPa O <sub>2</sub> during the expansion phase more pronounced than during the 3D phase.	(233)

ALP, alkaline phosphatase; BMP-2, bone morphogenic protein 2; ColX, collagen X; 3D, three-dimensional; GAG, glycosaminoglycan; HDAC4, histone deacetylase 4; NAC, *N*-acetyl cysteine; ROS, reactive oxygen species; VEGF, vascular endothelial growth factor.

addressed the concept of localized regions of lower P<sub>O</sub><sub>2</sub>. Moreover, MSC and HSC may originate from the bone marrow, but their sites of action extend throughout the body. Indeed, many have postulated that changes in P<sub>O</sub><sub>2</sub> as cells exit the marrow into the systemic bloodstream serve as a key trigger for terminal differentiation (402). In light of this, defining physiological normoxia for marrow-derived stem cells is difficult. In this review, we will consider 3–5 kPa as normoxia but will discuss select studies in which cells were cultured under 2 kPa for comparative purposes. A full summary of papers meeting these criteria is provided in **TABLE 9**.

Expansion at a P<sub>O</sub><sub>2</sub> of 3–5 kPa has repeatedly demonstrated greater colony formation or proliferation of MSC isolated from human (149, 528, 616) and sheep (700) bone marrow, although conflicting evidence has also been reported (449). A number of studies have identified an enhanced chondrogenic differentiation potential in MSC colonies expanded at 5 kPa (336, 374, 391, 528, 700), as characterized by the expression of *Col2a1* (see above) and quantitative analysis of glycosaminoglycan deposition. One study of human MSC cultured at 5 kPa reported no change in chondrogenic or osteogenic differentiation (449). This could be related to the source of cells used, as the latter study sourced human MSC from a commercial supplier, whereas the majority of studies obtain cells directly from donors. A common observation reported by Pattappa et al. and others (149, 700) is a reduced level of cellular senescence after long-term expansion at 5 kPa. This finding may be related to the increased level of stemness or differentiation potential in these cells and supports the notion of a more physiologically relevant phenotype under physiological P<sub>O</sub><sub>2</sub> in vitro. Fewer studies have focused on HSC (CD44<sup>+</sup>) within the marrow. Reykdal et al. observed less nitrite accumulation in cultures of human CD34<sup>+</sup> HSC isolated and expanded at 5 kPa for 7 days. These authors attributed this to reduced induction of the inducible isoform of nitric oxide synthase, although they did not investigate the contributions of other isoforms. Similar to MSC, HSC proliferate more rapidly under 5 kPa and form larger colonies (483).

## I. Skin

The measurement of transcutaneous P<sub>O</sub><sub>2</sub> using noninvasive techniques has long been used experimentally and clinically as a readout of peripheral perfusion/oxygenation. This procedure involves placing a housed electrode onto the skin surface heated to 41°C–44°C to encourage microvascular vasodilation, thus increasing local blood supply, which creates a local excess of O<sub>2</sub> delivered by the arteriolar circulation (**FIGURE 17A**). Transcutaneous P<sub>O</sub><sub>2</sub> is directly proportional to cutaneous blood flow (647) and is inversely proportional to epidermal thickness (144). Heating the skin from 37°C to 45°C increases blood flow 3- to 4-fold (269); thus, temperature intimately influences the reported P<sub>O</sub><sub>2</sub> value. For example, transcutaneous P<sub>O</sub><sub>2</sub> in the human forearm was recorded as 9.3 kPa at 44°C by Falstie-Jensen et al., yet only 5.1 kPa at 41°C by Spence et al. (550). Although a useful readout of arterial oxygenation clinically, such artifactual conditions result in relatively poor correlation with bone fide measurements of skin P<sub>O</sub><sub>2</sub> (see **FIGURE 17B**). Using penetrating electrodes, P<sub>O</sub><sub>2</sub> has been determined in the human abdominal, forearm, thigh, and fingernail cuticular dermis as well as in rat abdomen. At a generalized subcutaneous level, P<sub>O</sub><sub>2</sub> has been reported to range between 3 (266), 4.1 (626), 5 (551), 5.3 (632), 6.3 (637), and 8 kPa (138). More detailed investigations by Evans and Naylor (140), Baumgärtl et al. (27), and Wang et al. recorded P<sub>O</sub><sub>2</sub> profiles at various dermal depths (see **FIGURE 17C**). Evans and Naylor reported P<sub>O</sub><sub>2</sub> values of 6.1, 6.2 and 7.4 kPa at depths of 1–2, 3, and 5 mm, respectively, and similar profiles are also reported at equivalent depths in other areas of skin (27, 632). Clearly, the skin has two distinct sources of O<sub>2</sub> diffusion, the atmosphere and microvasculature, and a nadir exists in which cells receive little O<sub>2</sub> from either. One apparent pitfall in skin P<sub>O</sub><sub>2</sub> measurements using penetrating electrodes is the potential for overestimated values resulting from damage to the dense microvasculature. Jamieson and Brenk demonstrated that larger electrodes (330-μm versus 60-μm diameter) produced higher average subcutaneous P<sub>O</sub><sub>2</sub> values in the rat abdomen (alongside similar measure-

**Table 9.** *The effects of culture at physiological normoxia on marrow-derived stem cells*

Species	Cell Type	Po <sub>2</sub> (kPa)	Time	Comments	References
Human	MSC	1	1–3 wk	↓ Proliferation	(251)
	MSC in pellet culture	2	14 d	↓ Adipogenic and chondrogenic differentiation. ↑ Sulfated GAG, collagen, and proteoglycan formation, with more homogeneous surface distribution. More chondrogenic.	(374)
	Hemopoietic	5	10 d	↑ CD34 <sup>+</sup> CD38 <sup>-</sup> expansion due to ↑ proliferation, not ↓ apoptosis. ↑ Myeloid-committed cells (CD33 <sup>+</sup> CD14 <sup>+</sup> ) with ↑ colony-forming potential.	(495)
	MSC	5, 2	thawing and duration of culture	↑ Subsequent cell engraftment in irradiated mice. ↓ Colony numbers and cell yield at 5% specifically, but ↓ colony and individual cell size at 2%. ↑ Bone-marrow specific markers (CD44, 73, and 105) at both 5 and 2 kPa. ↓ Cellular senescence at 5% and 2%. ↓ O <sub>2</sub> consumption (microelectrode) and ↑ lactate production, with ↓ proportion of ATP generated by oxidative phosphorylation (azide sensitive).	(449)
	Hemopoietic (CD44 <sup>+</sup> progenitor)	5	>7 d	↑ Chondrogenic differentiation at 5% specifically. ↓ NO production (Griess). ↑ Proliferation and colony formation, with ↑ progenitor cell production and proliferation.	(483)
	Mesenchymal	3	up to 100 d	↑ Colony formation following isolation at 3 kPa ↔ Hypoxia-associated genes, but 2313 differentially expressed genes related mostly to aging (↓) and bone-marrow specific markers (↑). ↓ Senescence over 100 d, with high population doubling times. ↓ AGE accumulation and SA-β-gal <sup>+</sup> cells, markers of senescence,	(149)
	MIAMI	3	15 d	highest proliferation at 3 kPa. ↑ Embryonic and stem genes OCT4, REX-1, and hTERT. ↓ Osteoblast marker genes Runx and OCN. ↓ ALP activity, mineral deposition, and ECM-associated Ca <sup>2+</sup> content. MIAMI cells less differentiation/mature than MSC.	(101)

*Continued*

Table 9.—Continued

Species	Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time	Comments	References
	Marrow nucleated cells	1,5,10	6 d	Largest colonies formed with the highest density of cells at 5 kPa. Similar colonies formed between 1 and 20 kPa.	(616)
Porcine	MSC	5	42 d	Agarose constructs contained increased GAG deposition, particularly within the core. ↑ Col2a1 and ↓ Col1a1 relative to room air	(391)
	MSC	5	expd/dif/both	Expansion at 5% results in larger colony formation and thus higher cell yield. Differentiation at 5%, even when following expansion at 20%, enhances the chondrogenic potential of MSC; more stable pellet/hydrogel with ↑ Ca <sup>2+</sup> content and ↓ collagen X	(528)
Rat	MSC	5	up to 21 d	Enhanced calcium content and mineralization at 5 kPa O <sub>2</sub> suggests cells more likely differentiate in response to stimulation at 5 kPa O <sub>2</sub> .	(336)
Sheep	Mesenchymal	5	up to 14 d	↑ Colony size and number, ↑ proliferation. ↓ Senescence ↑ Chondrogenic differentiation	(700)

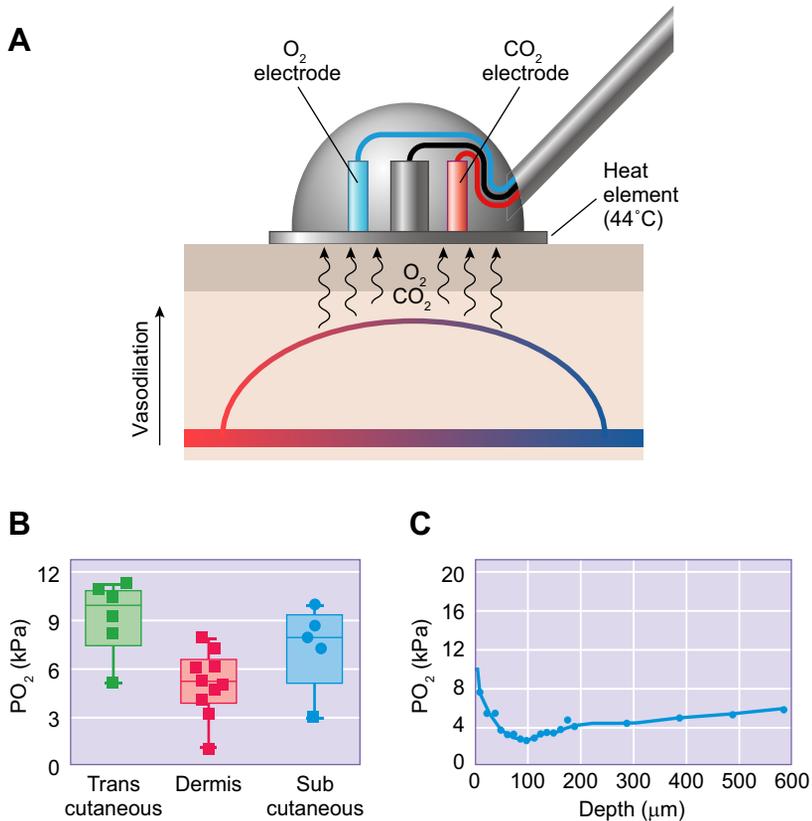
AGE, advanced glycosylation end products; ALP, alkaline phosphatase; ColX, collagen X; ECM, extracellular matrix; GAG, glycosaminoglycan; hTeRT, human telomerase reverse transcriptase; MIAMI, marrow-isolated adult multilineage inducible cells; MSC, mesenchymal stem cell; NO, nitric oxide; OCN, osteocalcin; OCT4, octamer-binding transcription factor 4; Runx; Runt-related transcription factor 1; SA-β-gal, senescence associated β-galactosidase.

ments in liver, kidney, and splenic tissue), with evidence of macroscopic tissue damage.

More recently, significant efforts have been made to develop techniques to noninvasively monitor cutaneous P<sub>O<sub>2</sub></sub> using phosphorescence quenching. Unlike the methods discussed in section IIC, in which a synthetic porphyrin-type dye is administered exogenously as an O<sub>2</sub>-sensitive probe, a technique developed by Mik and colleagues (223) employs 5-aminolevulinic acid, a precursor to the endogenously produced protoporphyrin IX. 5-Aminolevulinic acid cream is administered topically to the skin and results in accumulation of protoporphyrin IX in the mitochondria of epidermal cells within ~3 h (224). Using this technique, a P<sub>O<sub>2</sub></sub> of between 6.3 and 8 kPa was reported in cutaneous mitochondria of the rat abdomen (223, 225, 637), which correlates well with similar measurements using microelectrodes (138, 139). By coinjection of the hydrophilic Oxyphor G4 dye, simultaneous measurement of mitochondrial and microvascular P<sub>O<sub>2</sub></sub> was possible (223). A gradient of ~2.7 kPa between blood and mitochondria was reported in the rat abdominal cutis, which was abolished by topical application of cyanide. Notably, a microvascular P<sub>O<sub>2</sub></sub> of 10 kPa mea-

sured in this study is well within the range of reported transcutaneous P<sub>O<sub>2</sub></sub> values [9.3–11.2 kPa (144, 560, 647)], confirming that transcutaneous measurements accurately reflect microvascular P<sub>O<sub>2</sub></sub>. In a more recent study, mitochondrial P<sub>O<sub>2</sub></sub> was found to be a very sensitive indicator of the limit of hemodilution in pigs (489). However, the average baseline mitochondrial P<sub>O<sub>2</sub></sub> value reported in this study (2.7 kPa) is far lower than that recorded in rats in previous investigations [7.3–8 kPa (223, 225)], a discrepancy that remains unexplained.

Fibroblasts isolated from mouse embryos and tail and human dermis have all been cultured at 3–5 kPa (TABLE 10). Common to many of these independent reports is the observation that cells maintained at low O<sub>2</sub> exhibit markedly less chromosomal instability/breakage (78, 283, 446) and senescence (78, 446). This was particularly apparent in mouse-derived fibroblasts (446), which appear highly sensitive to the damaging effects of atmospheric conditions. Mouse embryonic fibroblasts cultured at 3 kPa had higher and persistent expression of the p53-related proteins p19<sup>ARF</sup> and p16, yet senescence could be rapidly induced by re-exposure to 20 kPa (446). Notably, this sensitivity ap-



**FIGURE 17.** Oxygen distribution in the skin. **A:** Concept of transcutaneous measurement of blood gas concentrations. Heating the skin causes vasodilation and enhances O<sub>2</sub> delivery to the epidermis, where it diffuses toward the measurement electrodes. **B:** Distribution of published PO<sub>2</sub> values in the dermis and subcutaneous tissues as well as transcutaneous measurements. Symbols are coded according to technique used: □, microelectrode; and ○, phosphorescence-quenching microscopy. **C:** An example of a PO<sub>2</sub> profile generating by electrode penetration of the skin. Adapted with permission from Baumgärtl et al. [27].

pears specific to laboratory rodent strains and is not observed in wild animals of the same species (448). This could reflect the longer telomeres observed in laboratory species (232) that are thought to occur in the absence of evolutionary selection for short telomeres in the wild. In human keratinocytes, isolation and culture at 4 kPa O<sub>2</sub> results in enhanced migration rates associated with reduced superoxide generation compared with cells cultured under 20 kPa (493).

Carrera et al. (68) reported increased HIF-1 $\alpha$  activity in primary keratinocyte populations cultured at a PO<sub>2</sub> of 5 kPa for up to 4 days. This was reduced by inhibition of the MAPK cascade and with certain DNA-damaging compounds, such doxorubicin, with minimal effects on proliferation. It is likely that these observations can be attributed to the phenomenon of self-inflicted hypoxia (see section IVD) based on the following observations: 1) HIF-1 $\alpha$  protein levels were still minimal at 5 kPa compared with those observed at 1 kPa. Because monolayer oxygenation decreases with cell density (see section IVC), HIF-1 $\alpha$  protein may only be stabilized at confluency and may therefore only affect proliferation in its latter stages; 2) prominent HIF-1 $\alpha$  protein expression and HRE-luciferase were observed in monolayers of the colon cancerous cell line HCT116 under the same conditions. Oxygen consumption rates are reportedly higher in these cells compared with primary human keratinocytes [25 versus 8 amol/min/cell (147, 619, 638)] and thus would have a lower intracellular PO<sub>2</sub> and hence

higher HIF-1 $\alpha$  activity; and finally, 3) inhibition of HIF-1 $\alpha$  stabilization was observed when cellular activity was reduced by MAPK inhibitors or by DNA damaging agents. A reduction in cellular activity may result in decreased O<sub>2</sub> consumption rates, thereby increasing intracellular PO<sub>2</sub>. As discussed in section IVD, an understanding of O<sub>2</sub> dynamics in monolayer cultures is critical in interpreting experimental data and should be considered when designing a model of in vitro normoxia.

## J. Adipose Tissue

Interest in PO<sub>2</sub> distribution in adipose tissue has increased in the last two decades (246) based on the observations that tissue from obese patients or animals can be hypoxic, although this is not fully accepted (188). In lean mice, PO<sub>2</sub> values have been reported between 6.4 and 7.7 kPa in epididymal fat pads (673, 676) and 5.6 kPa in the perigonadal white adipose tissue (477). Parallel measurements in the *ob/ob* transgenic obese mouse revealed a consistently lower adipose tissue PO<sub>2</sub> (2–4.6 kPa, decreasing with age), with strong histochemical evidence for tissue hypoxia through pimonidazole staining (477, 673, 676). In humans, subcutaneous adipose tissue PO<sub>2</sub> was measured at 7.6 kPa in the arm (280) and 7.3–7.9 kPa in in abdomen (187, 447) of lean patients. In contrast to rodent models of obesity, adipose tissue PO<sub>2</sub> in obese patients has been shown to be both higher (187, 618) and lower (280, 447) compared with

**Table 10.** *The effects of culture at physiological normoxia on skin cell physiology*

Species	Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time (days)	Comments	Reference
Human	82-6 and Bj (HCA2) MEF	3	60 (from isolation)	MEF cultures did not undergo senescence at 3 kPa, but it could be induced by exposure to 20 kPa at early time points. At 3 kPa, MEFs behaved more like human fibroblasts. Changes in expression patterns of p53 regulatory proteins p19 <sup>ARF</sup> and p16 at 3 kPa. ↑ Chromosomal breakage at 20 kPa in MEFs. MEF are particularly sensitive to oxygen metabolism damage, but at 3 kPa are just as robust as human fibroblasts.	(446)
	Keratinocyte	4	From isolation	Comparison between cells from young and old donors. ↑ Migration (scratch) in young, but not old, cells. No change in proliferation. ↓ ROS (DHE) independent of age. Scratching induces ROS production at leading edge, dissipation of which related to migration rate.	(493)
	Dermal Fibroblasts	2	>3	No change in metabolic activity or morphology. ↓ Inhibition of metabolic activity by blue light (450 nm) at 2 kPa, whereas near infra-red light (850 nm) stimulated metabolism only at 2 kPa.	(394)
	HCT116 Keratinocytes	5	4	↑ HIF protein at 5 kPa in HCT116, much less in keratinocytes (barely visible), accompanied by HRE/Luc activity and GLUT1 mRNA increases in HCT116 cells. Inhibition of MAPK cascade with UO126-reduced HIF1 protein, as did treatment with doxorubicin. ↑ Proliferation in HCT116 cells at 5 kPa, barely effected by HIF1 knock out. All observations consistent with self-inflicted hypoxia due to O <sub>2</sub> consumption. Inhibition of MAPK- or DNA-damaging agents would reduce cellular activity (O <sub>2</sub> consumption), thereby increasing pericellular.	(68)
Mouse	Tail fibroblasts MEF	3	7.5	Spontaneous chromosomal breaks at 20 kPa reduced at 3 kPa in cells with compromised chromosome stability (Ku86 <sup>-/-</sup> ). No change in cell proliferation. Some level of spontaneous instability even at 3 kPa, probably due to other sources of ROS.	(78, 283)
Rodent	Fibroblasts	3	30	Fibroblasts from laboratory mouse strains are the only rodent cells to exhibit marked sensitivity to O <sub>2</sub> .	(448)

DHE, dihydroethidium; GLUT1, glucose transporter 1; HRE-Luc, luciferase conjugated hypoxia-responsive element; MAPK, mitogen-activated protein kinase; MEF, mouse embryonic fibroblast; ROS, reactive oxygen species.

matched lean patients. Pasarica and colleagues (447) were able to demonstrate that adipose tissue  $\text{PO}_2$  correlated negatively with percentage fat composition and the expression of the inflammatory marker CD68 while correlating positively with capillary density. Based on these correlative relationships and the known histological characteristics of adipose tissue from obese patients (582), a lower  $\text{PO}_2$  in tissue from obese patients seems logical. The work by Goossens and colleagues (39, 187, 618) reports a higher fasting adipose tissue  $\text{PO}_2$  in obese patients compared with matched lean ( $\sim 9$  versus  $\sim 6$  kPa) subjects (187) and that weight loss in obese patients is associated with a significant reduction in mean adipose  $\text{PO}_2$  (6.8 to 5.5 kPa) (618). It was demonstrated that increasing and decreasing adipose tissue blood flow (using isoprenaline and angiotensin II infusion, respectively) leads to corresponding changes in tissue  $\text{PO}_2$ , corroborating claims by Pasarica et al. (447) concerning the relationship between adipose tissue  $\text{PO}_2$  and perfusion/vascularization. As adipose tissue blood flow is reduced in obese patients (187), one would expect a lower  $\text{PO}_2$ . These discrepancies could be due to either differences in technique used to monitor  $\text{PO}_2$ , with Goossens and colleagues using a custom-designed microdialysis technique as opposed to the more commonly used electrode/fiberoptic probe or physiological state in which measurements were made [fasting (187) versus normal (280, 447)].

As discussed and reviewed in by Trayhurn (586), a large body of work exists examining the effects of hypoxia ( $\text{PO}_2$  of 1–2 kPa) on adipocyte function in vitro to better understand the pathophysiology of obesity. However, as highlighted by Trayhurn, culture at 20 kPa followed by a dramatic drop to 1–2 kPa has limited physiological significance, as neither the starting  $\text{PO}_2$  nor hypoxic value are physiological for adipocytes. It is far more likely that adipocytes experience a  $\text{PO}_2$  of around 6–7 kPa in vivo, and to date, two studies have attempted to address this issue. The first by Wood and colleagues (663) exposed primary human adipocytes to  $\text{PO}_2$  values of 1, 3, 5, 10, 15, and 20 kPa for 24 h and measured expression and release of the key adipokines leptin and adiponectin as well as IL-6 and VEGF. A strong negative correlation was observed between leptin, VEGF, and IL-6 mRNA expression, and  $\text{PO}_2$ , whereas the opposite was observed for adiponectin and glucose uptake (663). Notably, the steepest part of the  $\text{O}_2$  concentration response curve was between 3 and 10 kPa, the physiological/pathophysiological range of  $\text{PO}_2$  in adipose tissue (see above). However, adipocytes were only exposed to different  $\text{PO}_2$  environments for 24 h, which may induce a response more representative of a response to low  $\text{O}_2$  and less indicative of their physiology in vivo. This problem was addressed in a subsequent study in which Famulla and colleagues (145) cultured adipocytes at 5 and 10 kPa for 14 days before measuring key adipocyte functions. Corroborating observations by Wood et al. (663), leptin expression and secretion were decreased at lower  $\text{O}_2$  and associated

with increased triglyceride content and glycerol release. Interestingly, peak responses were observed at a  $\text{PO}_2$  of 10 kPa (145), conditions in which intracellular  $\text{PO}_2$  is likely to be  $\sim 7$  kPa based on known  $\text{O}_2$  consumption rates of cultured adipocytes (694).

In addition to adipocytes and vascular cells, adipose tissue also contains a population of multipotent stem cells known as stromal cells (177). A number of studies have investigated the effects of long-term culture of these adipose-derived multipotent stem cells at low  $\text{O}_2$  levels, as summarized in **TABLE 11**. Similar to other types of stem cells (see section VI, *H5* and *K3*), culture at either 2 (606) or 5 (464, 512, 533) kPa for the duration of culture/differentiation resulted in increased adipogenic (512, 606) and/or osteogenic/chondrogenic (464, 606) differentiation in vitro. Notably, enhanced differentiation potential in vitro did not translate into increased chondrogenesis when explanted in vivo (464). Although informative, the rationale behind culturing adipose derived stem cells at 2–5 kPa is unclear in light of the known distribution of  $\text{PO}_2$  in such tissue in vivo (mean tissue  $\text{PO}_2 \sim 7$  kPa). It is possible that populations of stem cells exist in localized regions of lower  $\text{PO}_2$  within the tissue, although no evidence for this has been put forward to date. It seems more likely that 2 or 5 kPa  $\text{O}_2$  was chosen as a “best guess” based on similar publications in cells of different origin. Although the matter may appear trivial, the work of Wood et al. (663) discussed above illustrates a steep relationship between ambient  $\text{PO}_2$  and adipocyte function between 3 and 10 kPa, and thus, selecting the most appropriate ambient  $\text{PO}_2$  at which to culture such cells is absolutely critical.

## K. Uterus and Embryo

### 1. Uterus and oviduct

The uterus is a highly dynamic organ that experiences gross changes in physiology and function throughout the menstrual cycle, with surges in hormone secretion closely linked to contractile function and blood flow. In seminal work during the late 1960s, Mitchell and Yochim described periodic fluctuations in luminal (intrauterine)  $\text{PO}_2$  that were rhythmic from hour to hour (401), and also changed dramatically according to stage of the menstrual cycle (400). During estrous, intrauterine  $\text{PO}_2$  has been reported at between 3 (677) and 3.4 kPa (288, 400, 401) in the rat, 2.7 kPa in the guinea pig (174), 4.9 kPa in hamster (155), 5.7 kPa in rabbit, 1.7 kPa in rhesus monkeys (155), and between 2 (674) and 2.4–2.5 kPa in humans (440, 488). In experimental rodent models, intrauterine  $\text{PO}_2$  peaked during the diestrous-1 period (288) and was strongly associated with similar increases in blood flow (174, 400). Such changes were not observed in primates (155). Upon conception, intrauterine  $\text{PO}_2$  rises dramatically in rats (677) and

**Table 11.** *The effects of culture at physiological normoxia on adipose tissue–resident cells*

Species	Cell Type	P <sub>O<sub>2</sub></sub> (kPa)	Time (days)	Comments	Reference
Human	Adipocytes	15, 10, 5, 3, 1	1	Leptin, VEGF, and IL-6 mRNA and secretion inversely proportional to P <sub>O<sub>2</sub></sub> . Adiponectin mRNA and secretion proportional to P <sub>O<sub>2</sub></sub> . Steepest part of sigmoid curves between 3 and 10 kPa, with 10 kPa often not different from room air. Glucose uptake and GLUT transporter expression increased proportional to P <sub>O<sub>2</sub></sub> and corresponds to increased lactate secretion.	(663)
	Adipocytes	10, 5	14	No change in differentiation (Oil Red O staining), but decreased lipid droplet size proportional to P <sub>O<sub>2</sub></sub> . Increased triglyceride content at 10 kPa. Increased expression and secretion of adiponectin, IL-6, and DPP4, with concomitant decreases in leptin secretion (adipokine secretion). Increased glycerol release and hormone sensitive lipase expression at 10 kPa (lipolysis). Conditioned medium from 10 kPa cells induced the lowest SMC proliferation.	(145)
	Adipose MSC	5	duration of induction	A combination of kinase chemical inhibitors and 5% O <sub>2</sub> is optimal for the induction of iPSCs from adipose-derived stem cells.	(533)
	Adipose MSC	2	duration of culture	↑ Proliferation ↑ Viability ↑ Adipogenic and osteogenic differentiation potential following preadaptation to low O <sub>2</sub> .	(606)
	Adipose MSC	5	21	↓ Fatty acid binding protein 4 expression. ↓ Glycerol-3-phosphate dehydrogenase activity and triglyceride content, markers of adipogenic differentiation. Effects of low O <sub>2</sub> abolished by cytoskeletal inhibitors cytochalasin D and blebbistatin.	(512)
Human, rabbit	Adipose stromal cells	5	21	Culture at 5 kPa increases chondrogenic differentiation of stromal cells in vitro but does not increase subsequent chondrogenesis in vivo.	(464)

DPP4, dipeptidyl peptidase-4; GLUT, glucose transporter; IL-6, interleukin-6; iPSC, inducible pluripotent stem cell; MSC, mesenchymal stem cell; SMC, smooth muscle cell; VEGF, vascular endothelial growth factor.

rabbits (155), simultaneous with increases in progesterin and decreases in estrogen secretion (677). Indeed, ovariectomy to mimic estrogen depletion also caused large increases in intrauterine P<sub>O<sub>2</sub></sub> in rats (from 3.4 to 8.2 kPa), which were reversed by concomitant estrogen treatment (401). Unfortunately, no data exist to our knowledge concerning intrauterine P<sub>O<sub>2</sub></sub> across the menstrual cycle in humans, nor are there direct measurements before and after conception. Endometrial P<sub>O<sub>2</sub></sub> was measured by Rodesch and colleagues (488) in patients undergoing elective termination procedures at 8–10 wk and in those at 12–13 wk. These authors

report an increase from a mean P<sub>O<sub>2</sub></sub> of 5.3 kPa in the early termination to 6.2 kPa at 12–13 wk. Similarly, Jauniaux and colleagues (271) measured P<sub>O<sub>2</sub></sub> in coelomic/amniotic fluid and in the decidual lining in pregnancies between 7 and 10 wk and 11–16 wk. Although intrauterine fluid P<sub>O<sub>2</sub></sub> was similar [2.5 kPa, similar to that reported by Ottosen et al. (440) and Yedwab et al. (674)], P<sub>O<sub>2</sub></sub> in the decidual lining was significantly higher in late pregnancies (8.6 versus 9.8 kPa) (271). Thus, intrauterine P<sub>O<sub>2</sub></sub> is relatively low before pregnancy and during estrous, especially in primates and humans, but rises rapidly within the uterine wall (myome-

trium/decidua) upon conception or during diestrus in line with increases in blood flow.

In the fallopian tubes, a dichotomy exists between mammalian species according to whether ovulation is cyclic or initiated by copulation. In rodent species (noncycling),  $P_{O_2}$  within the fallopian tubes/oviducts remains constant and is relatively high, ranging from 6.8 to 8 kPa in rabbits (155, 380) and 5.6 kPa in hamsters (155). In contrast,  $P_{O_2}$  in the oviduct of rhesus monkeys is incredibly low when ovulation is not occurring (<1 kPa  $O_2$ ) but increases dramatically during ovulation to between 7 and 10 kPa (155, 365). During passage to the uterus, the oocyte receives nutrients and  $O_2$  directly from the fallopian tube lumen, and thus, it is postulated that rodent oviduct  $P_{O_2}$  is maintained at a high level to ensure it can accommodate an oocyte at any point (365).

## 2. *In vitro* fertilization

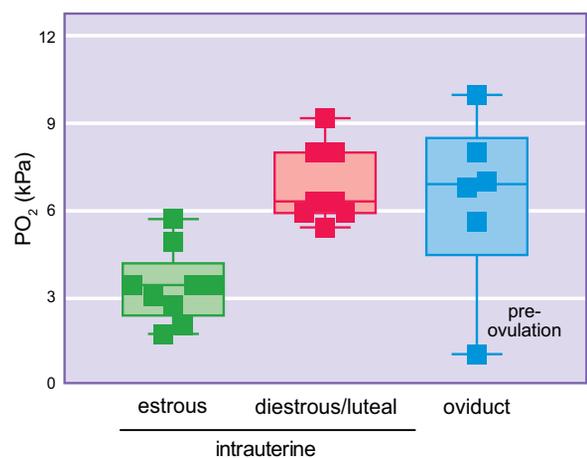
One of the earliest adoptions of *in vitro* culture under physiological normoxia was in the field of *in vitro* fertilization (IVF), in which the first successful culture of a human embryo to the blastocyst stage was achieved only under 5 kPa (557). Since then, working under a reduced ambient  $P_{O_2}$  (usually 5 kPa) has become reasonably common both in research and clinical IVF (45, 186, 285, 314, 418). Given the demand for improved clinical outcomes with IVF procedures, a large number of clinical trials have been performed to investigate whether culturing early-stage embryos at 5 kPa is beneficial. These have been reviewed extensively in several meta-analyses (45, 186, 418), and as such, this topic will not be discussed in detail. In two reviews published in 2011 (45, 186), conflicting conclusions were drawn. Bontekoe and colleagues (45) reported a statistically significant improvement in live birth rate when embryos were cultured at 5–6 kPa  $O_2$ , which equated to an increase in success rate from 30% to between 32% and 43%. In contrast, Gomes-Sobrinho and colleagues (186) were unable to conclude that culture at low  $O_2$  improved outcomes, although they did state that many results seemed promising. Notably, seven studies were retrieved in both reviews based on their respective selection criteria, yet these were not the same seven studies. Differences in selection criteria, with those applied by Bontekoe et al. (45) appearing stricter, are likely to explain the discrepancy in outcomes. In a later review by Nastri and colleagues (418), a small (5%), but significant, improvement was detected in live birth rates when embryos were cultured at 5–6 kPa, corroborating the findings of Bontekoe et al. (45). Common to all reviews was the criticism of study quality, especially related to investigator bias and differences in equipment/technique.

More recently, some have challenged the dogma that 5 kPa represents the ideal physiological  $P_{O_2}$  at which IVF should be conducted (286, 406, 670). This is based on the obser-

vation that  $P_{O_2}$  drops substantially between the oviduct and uterine lining from ~6 to 2–3 kPa (see **FIGURE 18**), and thus, the early blastocyst may experience a decrease in ambient  $P_{O_2}$  during implantation. To model this *in vitro*, embryos have been cultured at room air (670) or 5 kPa (286) until day 3, at which point ambient  $P_{O_2}$  was reduced to 2 kPa and blastocyst yield and quantity assessed at day 5. Cell yield increased 2-fold when embryos were cultured at 2 kPa between days 3 and 5 only when they were previously cultured at 5 kPa (286) with no significant effect detected if the embryo was previously kept at room air (670). In light of the significant effort and expense invested in improving IVF outcomes by utilizing the concept of physiological normoxia, these more intricate efforts to better match physiological conditions are a logical progression.

## 3. *Embryonic stem cells*

Embryonic stem cells (ESC) are pluripotent stem cells derived from the inner cell mass of the early blastocyst, pre-implantation into the uterine wall, and receive nutrients and  $O_2$  from the fallopian tube/uterine fluid. As such, they propagate in an environment containing low  $O_2$ , ranging between 2 and 5 kPa depending on the species (see above). Much like in IVF procedures, the derivation of ESC from the early blastocyst has long been conducted under low  $O_2$  conditions [see (397) and (539) for reviews, and **TABLE 12** for an up-to-date summary]. This has largely been driven by enhanced proliferation or colony/embryonic body formation, consistently observed in both mouse and human ESC expanded at a  $P_{O_2}$  of 2–5 kPa (30, 142, 161, 173, 176, 300, 403, 467, 469, 473, 475, 629). A second advantage is a higher degree of pluripotency and less spontaneous differentiation; whether determined by expression of the OCT4/NANOG/SOX2 triad or downstream targets (643, 678), by



**FIGURE 18.** Oxygen distribution in the oviduct and uterus. Reported values for intrauterine and oviduct  $P_{O_2}$  across mammalian species. Intrauterine values are separated according to menstrual cycle stage. In rhesus monkeys, ovulation is associated with large fluctuations in oviduct  $P_{O_2}$  (365); hence, the preovulation value is labeled appropriately.

SSEA-1 expression (142, 469), or by morphological analysis (161, 469). Interestingly, although maintained in an undifferentiated state, ESC at low  $O_2$  can also more readily differentiate, and to a higher degree, when stimulated. More efficient differentiation into cardiomyocyte (30), vascular (320, 473), pulmonary (173), chondrocyte (307), and, most often, neuronal (300, 403, 404, 666) lineages has been reported. Differentiation into neural precursor cells appears to occur preferentially at very low  $P_{O_2}$  (2–3.5 kPa) under the control of HIF-1/2 (666).

Genomic stability has often been assessed in ESC cultured at low  $O_2$  and compared with those exposed to room air. Forsyth et al. (161) showed that hESC exhibited greater spontaneous chromosomal aberrations after 20 passages at room air compared with those maintained for the equivalent time at 2 kPa, which had very few additional aberrations. Lengner et al. (335) subsequently demonstrated that culture at room air is responsible for the premature and irreversible inactivation of an X chromosome frequently observed during hESC culture, through demethylation of the *XIST* gene promoter region. Similarly, hypermethylation of the *DLK1/DIO3* cluster at room air results in silencing of this gene region which can be prevented by maintenance at physiological  $P_{O_2}$  levels (5 kPa) (TABLE 12).

ESC are known to be highly metabolically active, preferring glycolysis as their source of ATP generation (79). This phenotype appears accentuated when ESC are cultured at low  $O_2$ , with higher rates of glucose consumption and lactate production frequency observed (83, 158, 596). In their most recent paper, Christensen and colleagues (83) propose that increased glycolysis is facilitated by enhanced expression of GLUT3, which correlated positively with OCT4 mRNA expression, thus relating glycolytic activity to pluripotency. ESC are also known to consume a large amount of  $O_2$ , which creates a concern regarding self-inflicted hypoxia during culture (see section IV). It has been demonstrated on a number of occasions that  $O_2$  can be severely limited in monolayer cultures of ESC, especially at low ambient  $P_{O_2}$  (320, 466, 467, 596). Hence, as proposed by Turner et al. (596), confluent cultures kept at a  $P_{O_2}$  of 2 kPa [and even perhaps at 5 kPa (2, 320)] are inevitably encroaching on anoxia. This issue, although acknowledged, is yet to be satisfactorily addressed and thus calls into question the physiological validity of using very low (2–5 kPa) ambient  $P_{O_2}$  in ESC culture, with an intracellular  $P_{O_2}$  ~2–5 kPa being the actual desired outcome. Limited studies have been conducted with ESC cultured at higher (6–10 kPa)  $O_2$  levels, which may counteract  $O_2$  consumption to produce a more physiological intracellular  $P_{O_2}$ . In mouse ESC, similar levels of proliferation and pluripotency (OCT4/NANOG/SOX2 mRNA) (467) and VEGF production (473) were observed between ~4–10 kPa ambient  $P_{O_2}$ . However, human ESC differentiated to a higher degree during colony growth at 10 versus 5 kPa ambient  $P_{O_2}$  (469). Thus, there may well

be physiological consequences to the self-inflicted hypoxia occurring following culture at 2–5 kPa, although this needs further investigation.

#### 4. Placental tissue and trophoblasts

Placental development, and subsequently the health, of the tissue and fetus are closely linked to changes in  $P_{O_2}$  (270, 597, 650). During embryogenesis, rapid proliferation of trophoblastic tissue creates thick villus membranes, which result in reduced diffusion of  $O_2$  from the maternal arterial blood to the surrounding tissue. As such, intervillous  $P_{O_2}$  is reportedly as low as 2–3 kPa in human placenta at 8–10 wk gestation (271, 272, 488), which has been shown to modulate the proliferative and angiogenic trophoblastic phenotype required to establish a patent intervillous circulation (65, 270, 597). Once adequate perfusion is established (>12-wk gestation), a rapid rise in villous/placental tissue  $P_{O_2}$  is observed, reaching 7–8 kPa (271, 272, 488, 548), in which placental tissue  $P_{O_2}$  remains largely stable for the duration of gestation (597).

The issue of oxygenation in vitro has long been considered important in the culture of trophoblasts and placental tissue explants, and a large amount of the literature has already been elegantly reviewed by Tuuli and colleagues (597). Numerous studies have attempted to understand the impact of changes in  $P_{O_2}$  on trophoblast phenotype, largely through comparative studies on cultures maintained at ambient  $P_{O_2}$  values ranging from 20 to <1 kPa. However, measurement of pericellular  $P_{O_2}$  in primary human trophoblast cultures using a microelectrode revealed that cells were experiencing near anoxic ( $P_{O_2}$  of 0.1–0.6 kPa) conditions even when cultured under ambient (20 kPa)  $P_{O_2}$  (77). This gradient was medium-depth-dependent and abolished by methanol fixation of the cells, confirming evidence discussed previously (section IVC). Although not confirmed by others to date, these data clearly call into question the validity of using standard culture conditions to study primary trophoblasts in vitro.

## VII. CONCLUSIONS AND FUTURE PROSPECTS

The concept that oxygen is critical for normal cellular function is unanimously accepted. However, for scientists,  $O_2$  may represent more of a double-edged sword in view of the numerous damaging effects associated with reactive species produced from  $O_2$ . Despite this, traditional methods used extensively in the culture of mammalian cells result in the exposure to undefined, uncontrolled  $O_2$  levels, which are often at either extreme of the quasi-physiological range (i.e., either hyperoxic or hypoxic with respect to the physiological milieu). In this review, we have provided an up-to-date assessment of the current understanding of  $P_{O_2}$  distribution in tissues and organs in vivo and discussed some examples

**Table 12.** *The effects of physiological normoxia on embryonic stem cell physiology*

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time (days)	Comments	Reference
Human	ESC (H1)	5	12–15	hESC differentiation in culture was inversely proportional to P <sub>O</sub> <sub>2</sub> : little differentiation apparent when cultured at 1–4 kPa O <sub>2</sub> . Greater embryonic body formation under low O <sub>2</sub> . Phenomenon is not reversible, exposure to room air after low O <sub>2</sub> does not induce much more differentiation.	(142)
	ESC (H1, RH1 and H9)	2	14	Clonal recovery was 4- to 12-fold higher at 2 kPa, and cells were less differentiated. Switching back to room air reduced colony formation. Less spontaneous chromosomal alterations and perhaps longer telomeres.	(161)
	ESC (H1, RH1 and H9)	2	10 passages	Genetic screen of cells cultured for 10 passages at 2 or 18 kPa O <sub>2</sub> . Between passage 0 and 10, no change in genome at room air, but robust genomic changes at 2 kPa.	(160)
	H1 and H9	4	7 (after multiple passages)	Cultures at 4 kPa displayed less heterogeneity in their transcriptome. No change in the expression of pluripotency after culture at 20 kPa for 7 days, although a number of genes under the OCT4/NANOG/SOX2 triad are expressed much less.	(643)
	CLS1/2	1, 5, 10, 15	Up to 8 wk	Colony formation as inversely proportional to P <sub>O</sub> <sub>2</sub> . After 4 wk, re-exposure to room air rapidly induced proliferation and differentiation, even in cultures kept at 5 kPa for 18 mo. Colonies at 5 kPa O <sub>2</sub> homogeneous and undifferentiated. Inhibition of notch signaling–normalized differentiation.	(469)
	Blastocyst-derived	5	From thawing	Cells thawed at 5 kPa O <sub>2</sub> and then exposed to room air for >3 days. No gross changes in genome after chronic culture at room air. Spontaneous differentiation reduced after exposure to room air. Exposure to room air induces irreversible X chromosome inactivation.	(335)
	H9	5	6–12	At room air, dissolved P <sub>O</sub> <sub>2</sub> ~15 kPa, and near 1 kPa at 5 kPa ambient. Decreased O <sub>2</sub> consumption at 5 kPa. Early vascular markers (CD42, KDR, and CD56) increased at 5 kPa, with morphological evidence for increased endothelial differentiation. When differentiation was split into two parts; culture at 5 kPa was only required for the first 6 days. Culture at 5 kPa increases ROS formation (DCF) and inhibition with DPI abolished this and the increased EC differentiation.	(320)

*Continued*

Table 12.—Continued

Species	Cell Type	P <sub>O</sub> <sub>2</sub> (kPa)	Time (days)	Comments	Reference
	MEL-2 ESC	2	Up to 5	No significant change in proliferation. ↑ Lactate and glucose consumption and ↓ ammonia consumption. ↑ Production of alanine and ↑ consumption of aspartate, asparagine, and glycine. ↓ Consumption of glutamine. Good information on O <sub>2</sub> diffusion and limitations in vitro. Intracellular P <sub>O</sub> <sub>2</sub> most certainly close to 0 kPa at 2 kPa ambient in ESC cultures.	(596)
Human	Shf3 and Hues-7	5	Minimum of 3 passages	No large change in amino acid utilization or production. ↑ Glycine consumption ↓ Serine uptake	(82)
	hESC and hiPSC	2	>5	Genomic screen suggested culture at 2 kPa shifted cells toward neuronal lineages (expression of SOX1, HES5, and FOXP1), specifically toward glial differentiation versus neuronal. Effect was abolished by HIF-2 siRNA and HIF-1α inhibition. HIF regulates MYC, and thus LIN28/let-7, a key neuronal lineage regulator.	(666)
	Blastocyst-derived	5	From derivation/thawing	Imprinted region DLK1-DIO3 frequently silenced during culture because of hypermethylation. When lines were derived and maintained at 5 kPa, gene products from these regions (MEG3 and SNORD114-3) were still highly expressed. Re-exposure to room air caused rapid downregulation of these gene products and methylation of their promoters. Greater genomic stability when cultured and maintained at 5 kPa O <sub>2</sub> .	(665)
	Shf3 and Hues-7	5	Minimum of 3 passages	↑ GLUT3 expression and membrane localization. GLUT3 mRNA positively correlates with OCT4 mRNA. Changes in GLUT3 expression may underlie changes in lactate/glucose consumption.	(83)
Mouse	D3	4	9	mESC cultured at 4 kPa for 9 days and then back to room air for 5 more. Early culture at 4 kPa O <sub>2</sub> increased differentiated cardiomyocyte yield.	(30)
	Stem cell (fresh)	5	28	More outgrowths from blastocysts and increased proliferation with more alkaline phosphatase activity in outgrowths.	(176)
	Stem cell (fresh)	5	From blastocyst isolation	↑ Overall cellular yield. ↓ ROS production (measured using DCF fluorescence). Combination of low O <sub>2</sub> and physiological levels of glucose (100 mg/dl) optimum for yield.	(629)

Continued

Table 12.—Continued

Species	Cell Type	Po <sub>2</sub> (kPa)	Time (days)	Comments	Reference
	CCE and D3 mESC	0, 1, 5, 20 and 40	Up to 25	Mathematical modeling of Po <sub>2</sub> at the cell layer. ↑ Proliferation at 5 kPa versus room air. Very low O <sub>2</sub> levels (<1 kPa), ↓ pluripotency genes (Oct4, Nanog, and Sox2) and at 40 kPa.	(467)
	D3 mESC	3.5	12	Greater degree of differentiation into dopaminergic neuronal precursor cells at low O <sub>2</sub> and with greater yield.	(300)
Mouse	iPSC (MEF)	5	Up to 30	↑ Efficiency of pluripotency induction and ↑ yield. Observed with both viral and nonviral transfection methods. No change in proliferation. ↑ 57.2% ESC-specific genes, ↓ 67.5% fibroblast-specific genes. Demonstrates efficiency in differentiation.	(678)
	R1	1, 2, 4, 8	7	Production and secretion of Flt-1 and VEGF change temporally over 7 days and at low O <sub>2</sub> , driving ESC into either hematopoietic or endothelial lineages at different time points. Colony formation greatest at 2–4 kPa O <sub>2</sub> and lowest at 1 and 20 kPa.	(473)
	E14Tg2a mESC	2	8	Increased viability during 8 days of differentiation. ↑ Neuronal stem cell differentiation.	(404)
	E14Tg2a mESC	2	8	Valuable data on dissolved Po <sub>2</sub> in culture. Highest number and diameter of neural bodies (rosettes) between 4 and 10 kPa O <sub>2</sub> , with the greatest number of viable cells. Greatest number of neuronal precursor cells observed at 4 kPa O <sub>2</sub> . Increases from 2 to 4/6 kPa O <sub>2</sub> associated with ↑ total yield.	(403)
	R1 129/Sv (ESC) MAR B6D2 F1 (ESC)	5	3	↑ Apoptosis ↑ Proliferation	(475)
	E14Tg2A (ESC) iPSwt4F (iPSC)	5	Up to 12	↑ ROS generation (measured using DCF fluorescence). ↓ Cardiomyocyte differentiation ↑ Embryonic body formation ↑ Expression of NKx2.1 and FOXA2, markers of endodermal and early lung epithelial lineages. ↑ Differentiation into early pulmonary lineages following stimulated differentiation.	(173)

DCF, dichlorofluorescein; DLK1-DIO3, delta-like homolog 1-type III iodothyronine deiodinase gene cluster; DPI, diphenyleiodonium; EC, endothelial cell; ESC, embryonic stem cell; Flt-1, vascular endothelial growth factor receptor 1; FOXA4, forkhead box protein A2; FOXG1, forkhead box protein G1; GLUT, glucose transporter; HES5, Hes family BHLH transcription factor 5; hESC, human embryonic stem cell; HIF, hypoxia-inducible factor; hiPSC, human induced pluripotent stem cell; iPSC, inducible pluripotent stem cell; KDR, kinase insert domain receptor/vascular endothelial growth factor receptor 2; MEF, mouse embryonic fibroblast; MYC, v-Myc avian myelocytomatosis viral oncogene homolog; NKx2.1, NK2 Homeobox 1; OCT4, octamer-binding transcription factor 4; ROS, reactive oxygen species; VEGF, vascular endothelium-derived growth factor; mESC, mouse embryonic stem cells.

of in which this knowledge has been implemented to enhance the physiological relevance of cell culture conditions *in vitro*. In collating and critically discussing this information, we hope to provide a reference source for future research aimed at designing novel and physiologically relevant experiments to address ever-more complex scientific questions.

As highlighted throughout this review, accurately recapitulating physiological normoxia *in vitro* is far more complex than simply adjusting the ambient headspace  $PO_2$ . An understanding of the physical conditions in which cells are cultured (i.e., plastic permeability, volume of medium used, and rates of  $O_2$  equilibration in solution) should underpin the choice of the final desired pericellular  $PO_2$  determined using mathematical models and/or experimental data to predict pericellular versus ambient  $PO_2$ . Such careful experimental design informed by our review of the literature should provide researchers with the closest representation of likely tissue  $PO_2$  levels *in vivo*. Differences in experimental conditions and protocols for cell culture, when sufficient detail is reported, and concerns about the definition of physiological normoxia have may limit collective advances for translational research.

Powerful tools are now available to better predict and measure  $PO_2$  in culture, with accumulating studies highlighting their necessity. We thus hope that the contents of this review will help unify experimental approaches used by basic and clinical researchers. In this context, we propose the following guidelines for researchers who wish to culture their cells under defined physiological normoxia *in vitro*:

1. **Define the conditions appropriately.** Oxygen levels should be measured and defined in terms of  $PO_2$  whenever possible. Often reported as room air or 20%  $O_2$ , most cell culture experiments are conducted in incubators in which the ambient  $PO_2$  is closer to 18.5 kPa, and sometimes below.
2. **Start the experiment properly.** Always pre-equilibrate all culture media and solutions for a minimum of 2 h, and considerably longer for large volumes, at the appropriate ambient  $PO_2$  before use on cells. It is advisable to store all culture plasticware at the desired  $PO_2$  to avoid  $O_2$  leaching.
3. **Controlling monolayer oxygenation.** We have highlighted throughout this review that appropriately controlling monolayer oxygenation is a consistent problem. There are several parameters that can be easily altered to maintain control over monolayer oxygenation, listed according to relative ease:
  - i. Use of  $O_2$ -permeable plastic:* this creates a new and much more efficient way in which  $O_2$  can be delivered to the monolayer, alleviating problems due to static medium.
  - ii. Various medium height: surface area:* by minimizing the ratio between medium height and culture

surface area, one reduces the distance for  $O_2$  diffusion and thereby maximizes delivery. Simply reducing the volume of medium can achieve this.

- iii. Various ambient  $PO_2$ :* if medium volume cannot be reduced, one can increase the ambient  $PO_2$  to compensate for monolayer  $O_2$  consumption.
- iv. Continuous perfusion:* to completely alleviate issues associated with  $O_2$  delivery, continuous perfusion of well-oxygenated medium is an elegant way to control intracellular  $O_2$  precisely, even in response to large increases in  $O_2$  consumption.

Results should always be interpreted in the context of pericellular or intracellular  $PO_2$  rather than ambient  $PO_2$ . Mathematical models have proved a useful tool to predict such values, and recent advances in experimental techniques have allowed the direct monitoring of intracellular  $PO_2$ .

4. **Consider a range of  $PO_2$  values.** Oxygenation *in vivo* is heterogeneous in both space and time, and thus, no single value can be described as normoxia for a given cell type. Moreover, the expression and activity of many proteins are not linearly related to the intracellular  $PO_2$ . It is for these reasons that we find it far more informative to conduct preliminary studies under a range of physiological  $O_2$  levels (2–10 kPa, for example), which offer a far more relevant comparison than 21 versus 1 kPa.

Can culture under physiological normoxia improve the translation of cell physiology to animal models and the clinic? There are several excellent studies (342, 499, 553, 578) that have already provided convincing evidence in favor of this hypothesis, and the concept is already implemented clinically in IVF clinics around the world. Despite this, we believe there is still significant scope to demonstrate that culturing cells under their respective physiologically normoxic conditions genuinely recapitulates their native phenotype and improves outcomes of clinical relevance. Moving forward, we believe it is critical for this field of research to avoid isolated phenotypic comparisons between cells at room air and those at normoxia, instead focusing on whether culture under physiological conditions can reveal novel insights into disease pathology or pharmacodynamics and kinetics of existing and novel therapeutics. Moreover, it is perhaps overly simplistic to consider only one normoxic value within a given tissue when there is clearly considerably complexity in tissue oxygenation. Thus, the oxygen-sensitivity of a pathway of interest may be more accurately assessed over a small range of normoxic values, such as that between the renal medulla and cortex (section VIF) or from the inner bone marrow to the associated vasculature (Section VIH). Furthermore, although critically important,  $O_2$  represents just one component of the physiological milieu that is altered during standard culture practice, with other factors such as biomechanics, 3D coculture, and substrate matrix contributing equally to the cellular phenotype. Mov-

ing forward, it is essential to better model all these factors together to truly begin recapitulating the physiological environment in vitro.

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## DISCLOSURES

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